



Original Article

Shock attenuation properties at heel strike: Implications for the clinical management of the cavus foot



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ARTICLE INFO

Article history:

Received 15 December 2015

Received in revised form 16 February 2016

Accepted 6 March 2016

Available online 31 March 2016

Keywords:

Heel strike

Acceleration

Shock absorption

Gait

ABSTRACT

Background: This study explored the relationship between foot types and corresponding variations in shock attenuating properties of the heel.

Methods: Thirty matched participants were assigned to 3 groups: pronated, neutral, and supinated. A low-mass accelerometer was mounted to the calcaneus of the right leg of each participant.

Results: Acceleration at heel strike for supinators was significantly higher than that in individuals with pronated and neutrally aligned feet. No significant difference was found in mean and maximum acceleration at heel strike between pronators and neutrals.

Conclusion: Cavus feet undergo significantly higher mean and maximum acceleration forces than neutrally aligned and pronated feet.

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1. Introduction

The impact of the foot with the ground at heel strike generates repetitive impulsive forces which are transmitted throughout the whole body, mostly along the tibia, knees, femur, hip, lower back, and up to the skull. As these forces travel up along the lower extremities, they may be detrimental to the musculoskeletal system. During this process, the lower limbs are responsible for absorbing shock and decreasing impact forces,¹ by the action of the fibro-fatty tissue beneath the calcaneum which is the first line of defense against these acceleration force, since this is the first anatomical region of the foot that normally hits the ground. This is then followed by rapid plantarflexion in the first phase of initial contact, controlled by eccentric deceleration by the ankle dorsiflexors, coupled later on by knee flexion during the initial period of the stance phase. Indeed, literature suggests that walking with reduced knee flexion torque at heel contact results in a reduced heel deceleration.²

There is increasing evidence supporting the link between heel impact forces, once excessive, and the development of a number of pathological conditions, including degenerative joint disease such as osteoarthritis,³ plantar fasciitis, headaches, prosthetic joint loosening, muscle tears, and lower back pain.⁴

There is a surprising paucity of information, however, regarding the repetitive heel impact forces during normal walking, and any relationship that there might be with foot posture. In an investigation of the highest force recorded in the F_z (vertical force) direction during landing, Hargrave et al. (2003) de-emphasized the importance of anatomical foot alignment on impact forces and absorption during a single-leg drop landing, concluding that further investigations are needed to fully elucidate the role of subtalar pronation in force dissipation during dynamic functional activities.⁵

On the other hand, during running, the repetitive loading together with the impact shocks cause microtrauma to underlying tissues, which may cause damage and impair function.⁶

Acceleration at the calcaneus can be quantified by an accelerometer, which is an inexpensive and reliable tool that can measure certain gait parameters, shock attenuation, and body segment accelerations during gait.^{7,8} Notwithstanding the ready availability of these devices, only few studies have investigated calcaneal acceleration in relation to foot types. Ledoux et al. (2001) reported that acceleration of the calcaneus at heel strike was not sensitive for foot type, for neutrally aligned, and pes planus feet; however, the authors did not include pes cavus feet in their study.⁹

A pes cavus, or supinated, foot is assumed to be relatively rigid with reduced shock attenuation abilities while a flat, or pronated, foot is more flexible and able to attenuate the transient forces more efficiently.¹⁰ However, to date, no evidence supports this assumption about the relationship between supinated feet and related reduced shock attenuating properties. Literature has demonstrated

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a lack of congruency regarding the relation between foot structure and lower limb mechanics such as shock attenuation. Despite this general assumption that individuals with a supinated foot type have diminished shock attenuation properties, there is a considerable lack of scientific evidence supporting this theory. This study aimed to explore possible calcaneal acceleration variation during heel strike in the different foot types and consequently this paper outlines the various shock-attenuation characteristics of the main 3 foot types during initial heel strike in healthy adults with controlled cadence.

2. Materials and methods

This study adopted a non-experimental quantitative and comparative design. Thirty healthy participants were recruited via a convenience sampling method, from a university student population following approval by the University Research Ethics Committee. Participants were excluded from the study if they were over 60 years of age, body mass index exceeded 29 kg/m^2 , and if they presented with any orthopedic pathologies, including limb length discrepancy of more than 2 cm and ankle equinus. Neurological disorders, which could potentially prevent normal heel strike during stance phases including peripheral nerve injury, diabetic peripheral neuropathy, and Charcot joint disease, were also excluded.

Prior to commencing data collection, all participants, who signed informed consent, underwent a thorough lower limb examination by an experienced clinician. During this screening process, the feet of each participant were examined for ranges of motion, muscle strength, and quality of the heel fat pad. The subjects were then assigned to three groups of ten participants each, whose foot type according to the Foot Posture Index (FPI-6) determined the group. The FPI is a validated tool which classifies foot posture in a neutral, pronated, or supinated position according to 6 criteria^{11,12} and has been used extensively in various studies where classification of foot type was evaluated.^{13,14}

The three groups were matched for gender, age, and weight. The first group included participants having an FPI-6 value ranging from -1 to -12 (supinated feet), the second group comprised of subjects with values of 0 to $+5$ (neutrally aligned feet) while the subjects in the third group had an FPI-6 value between $+6$ and $+12$ (pronated feet).

A low-mass (12 g) triaxial accelerometer (x-IMU; $33 \times 42 \times 10 \text{ mm}$; 512 Hz; range up to $\pm 8 \text{ g}$) was then adhered to the subjects while standing barefoot in an upright position on even ground. The accelerometer was directly mounted on the posterior aspect of the medial surface of the calcaneus of the right leg of each participant (posterior to and inferior to the medial malleolus) using adhesive taping and reinforced with an elastic strap, in order to preload the accelerometer and to prevent movement of skin¹⁵ (Fig. 1). Before commencing trials, while each subject was standing still in quiet stance, the active axis of the accelerometer was aligned to the long axis of the tibia, so the acceleration due to gravity could be measured. During eventual data calculation, this was then subtracted from the overall calcaneal acceleration value. The participants then walked barefooted on a treadmill at a fixed speed of 3.5 km/h for 5 min. Five sets of 5 stride cycles were collected at random intervals without the participants' knowledge, effectively blinding the participants as they were unaware of the exact moment data was being collected.

Data was collected using x-IMU GUI software (version 13.0.4911.40774; X-IO Technologies Limited, UK) which logged and converted raw data (in g's) which was streamed via a Bluetooth connection from the unit to a nearby laptop. This raw data was then exported to a Microsoft Excel spreadsheet (Fig. 2). For each participant, the average acceleration and maximum acceleration at heel strike of the 5 stride cycles was calculated. Statistical analysis was preceded by the use of Kolmogorov–Smirnov test to check for



Fig. 1. Accelerometer loaded on the leg.

distribution of data. Since the data was found to be normally distributed, the One-Way ANOVA test was subsequently used to compare the average and maximum acceleration at heel strike between pronated, neutral, and supinated feet.

3. Results

Twenty-one female and 9 male participants, with a mean age of 21 years (SD 2.5) and mean weight of 65 kg (SD 10.3), were recruited.

3.1. Mean acceleration at heel strike

The mean acceleration at heel strike for supinated feet (2.127 g) was significantly higher than in pronated (1.344 g) and neutral feet (1.317 g), ($p = 0.002$). The Dunnett T3 post-hoc test revealed comparable average acceleration at heel strike for the pronated and neutrally aligned feet ($p = 0.994$). On the other hand, the mean acceleration at heel strike for supinated feet was significantly higher than the average acceleration for pronated and neutral foot types ($p = 0.039$ and $p = 0.031$ respectively).

3.2. Maximum acceleration at heel strike

The same results were obtained when analyzing maximum acceleration at heel strike. The one-way ANOVA test revealed an average maximum acceleration which was significantly higher in supinated feet (2.709 g) as opposed to pronated (1.733 g) and neutral (1.665 g) foot types ($p = 0.002$).

When values for pronated and neutral feet were analyzed, the maximum acceleration at heel strike was not significantly different ($p = 0.968$). However, when comparing supinated feet to the pronated and neutral feet, a significant difference ($p = 0.040$ and $p = 0.025$ respectively) was found between foot types.

4. Discussion

This study aimed to explore possible calcaneal acceleration variation during heel strike in the different foot types. Results confirm that supinated feet had significantly higher mean and higher maximum acceleration at the calcaneus during heel strike than the neutral and pronated types, i.e. this foot type resulted in reduced shock attenuation. Although this has for long been suspected, the scientific evidence is conspicuously lacking.

The results of this study also revealed no significant difference for the average acceleration and the maximum acceleration at heel strike between pronated and neutral foot types. This supports results of the study by Ledoux and Hillstrom (2001), who also report no differences in subjects with pes planus and neutrally aligned feet.⁹ Despite the fact that supinated feet were not

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