



ORIGINAL ARTICLE / *Vascular imaging*

## Lower extremity CT angiography at 80 kVp using iterative model reconstruction

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### KEYWORDS

Lower extremity;  
Angiography;  
X-ray computed tomography;  
Low tube voltage;  
Iterative model reconstruction;  
Radiation dose

### Abstract

**Purpose:** To evaluate the use of 80 kVp and iterative model reconstruction (IMR) in lower extremity computed tomography angiography (CTA).

**Materials and methods:** Sixty patients were randomly assigned to Group A or Group B (both  $n = 30$ ) to further undergo CTA. Group A received Protocol 1 (P1) with 120 kVp, 180 mAs, and 100 mL of contrast agent with filtered back-projection (FBP). Group B received Protocol 2 (P2) and Protocol 3 (P3) with 80 kVp, 140 mAs and 75 mL of contrast agent with hybrid iterative reconstruction (P2) and IMR (P3). Mean intravascular attenuation (MIA), image noise, contrast-to-noise ratio (CNR), and signal-to-noise ratio (SNR) were compared. Radiologists assessed image quality on a 5-point scale, and radiation was compared between both groups.

**Results:** Group A had 9 men and 21 women (mean age,  $68.2 \pm 9.3$  years [range: 53–85 years]), and Group B had 20 men and 10 women (mean age,  $64.8 \pm 10.4$  years [range: 37–81 years]). The MIA of P2 and P3 were significantly larger than that of P1 ( $P < 0.01$ ). The CNR and SNR of P3 were significantly higher than those of P1 and P2 ( $P < 0.01$ ). The interobserver agreement had Kappa values of 0.78, 0.77, and 0.81 for P1, P2, P3, respectively. The mean CT volume dose index and dose-length product of Group B were lower than those of Group A ( $P < 0.01$ ).

**Conclusion:** Lower extremity CTA using 80 kVp and IMR is useful for lower radiation and contrast agent dose while preserving image quality. IMR can also provide better image quality for small-caliber vessels below the knee than HIR.

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28 Computed tomography angiography (CTA) is widely used  
29 in patients with lower extremity arteriosclerosis obliterans,  
30 thus providing accurate criteria for treatment decision [1,2].  
31 However, lower extremity CTA is associated with high radia-  
32 tion exposure and high doses of contrast agent for patients  
33 due to the necessity of completing an extensive scanning  
34 from the abdomen to the feet. Therefore, new methods are  
35 being studied to reduce the dose of radiation and contrast  
36 agent while obtaining a relatively satisfactory image qual-  
37 ity [3–6]. Among various methods for reducing the radiation  
38 dose, low tube voltage appears as the most effective, while  
39 also permitting a reduction in contrast agent dose due to  
40 generating higher vascular enhancement [7]. However, low  
41 tube voltage also increases the noise due to the reduction  
42 of transmitted radiation, which can potentially affect the  
43 image diagnostic quality [5,8,9].

44 Currently, the filter back-projection (FBP) algorithm is  
45 widely used, which is a very fast and robust reconstruc-  
46 tion technique. However, there is a noticeable increase  
47 in image noise with the decreasing tube voltage [10–12].  
48 Iterative reconstruction (IR) is an alternative image recon-  
49 struction method to FBP that can reduce radiation doses  
50 with similar quality image indexes such as noise compared  
51 to routine-dose FBP [13–18]. Previous reports have shown  
52 that CTA using low tube voltage with hybrid IR (HIR),  
53 which is a raw-data-based iterative method and consists  
54 of a dual-model (noise and anatomical) technique, can  
55 decrease the dose of radiation and contrast agent without  
56 compromising image quality [19–21]. The knowledge-based  
57 iterative model reconstruction (IMR) is a recently developed  
58 image reconstruction algorithm that uses a knowledge-based  
59 approach to optimize a penalty-based cost function while  
60 accurately incorporating the geometry and physical charac-  
61 teristics of a CT scanner [10]. Studies have shown that IMR  
62 can significantly improve both qualitative and quantitative  
63 image quality compared with FBP and HIR [22–25]. However,  
64 the feasibility of IMR with low tube voltage and reduced  
65 contrast agent in lower extremity CTA is still unknown, and  
66 there are also no reports about comparing the image quality  
67 between IMR and HIR in lower extremity CTA with low tube  
68 voltage. Therefore, we hypothesized that lower extremity  
69 CTA using IMR at 80 kVp can provide at least equivalent if not  
70 better qualitative and quantitative image quality compared  
71 to FBP at 120kVp and HIR at 80 kVp.

72 The purpose of this study was to evaluate the feasibility  
73 of using 80 kVp and IMR in lower extremity CTA.

## 74 Material and methods

### 75 Patients

76 Sixty consecutive patients with suspected lower extremity  
77 arteriosclerosis obliterans were enrolled between October  
78 2016 and July 2017. The clinical data collected included age,  
79 gender, body weight, and height. The exclusion criteria were  
80 allergy to iodinated contrast agent, renal insufficiency, and  
81 history of stenting or bypass surgery in lower limb arteries.  
82 Based on a random-number table, all patients were ran-  
83 domly assigned into a control group (Group A,  $n=30$ ) using  
84 120 kVp for CTA and an experimental group (Group B,  $n=30$ )  
85 using 80 kVp. This study was approved by our institutional

review board. Written informed consent was obtained from  
all participating patients.

### CT scanning protocol

86 All CTA examinations were performed using a 256-sections  
87 CT scanner (Brilliance iCT<sup>®</sup>; Philips Healthcare, Cleveland,  
88 OH, USA). Scanning was performed in a craniocaudal direc-  
89 tion from the distal abdominal aorta to the foot. Scanning  
90 parameters included: detector collimation,  $128 \times 0.625$  mm  
91 with dynamic z-focal spot; gantry rotation time, 0.27 s; and  
92 matrix,  $512 \times 512$  pixels. The automatic tube current mod-  
93 ulation (ATCM) (Doseright index<sup>®</sup>; Philips Healthcare) was  
94 used in both groups. Reference tube current-time product  
95 was 180 mAs in Group A and 140 mAs in Group B. A dual-  
96 head power injector (Ulrich REF XD 2051<sup>®</sup>; Ulrich Medical  
97 GmbH, Ulm, Germany) via a 20-gauge intravenous cannula  
98 (inserted into a superficial vein positioned in the right ante-  
99 cubital fossa) was used. Group A, as a control, used 100 mL  
100 of contrast agent (iohexol, Shuangbei 350<sup>®</sup>, Beilu Pharma-  
101 ceutical Co., Ltd. Beijing, China) injected at a flow rate of  
102 4 mL/s followed by infusion of normal saline (40 mL) at the  
103 same flow rate. Group B used 75 mL of the same contrast  
104 agent. The time it takes for the contrast agent to reach the  
105 distal vessel is usually late for lower extremity arterioscle-  
106 rosis obliterans, so the flow rate was decreased to 3 mL/s in  
107 order to maintain continuous intra-arterial contrast agent  
108 during the CT scanning. For both groups, the bolus-tracking  
109 technique was used, and the monitor region was placed at  
110 the lumbar 3 vertebral body level. Scans were initiated 20 s  
111 after attenuation reached 200 Hounsfield units (HU).  
112  
113  
114

### Image reconstruction

115 The CT data of Group A were reconstructed with Protocol 1  
116 (P1) via FBP, whereas those of Group B were reconstructed  
117 with Protocol 2 (P2) via HIR (iDose4<sup>®</sup>, Philips Healthcare,  
118 Cleveland, OH, USA) and Protocol 3 (P3) via IMR. The iDose4<sup>®</sup>  
119 system offers seven levels to control or reduce the amount  
120 of image noise at a given tube output; levels 1–7 provide  
121 noise reduction factors of 0.89–0.45 [19]. Similarly, the pro-  
122 totype provides three levels for IMR, and levels 1–3 provide  
123 60%, 70%, and 80% noise reduction, respectively [26]. In our  
124 study, iDose4<sup>®</sup> at level 4 and IMR at level 1 were applied  
125 to image reconstruction, which are routinely used at our  
126 institute. Images were reconstructed in transverse sections  
127 with a slice thickness of 1.5 mm and increment of 1.0 mm.  
128 Next, all datasets were transferred to a dedicated work-  
129 station (IntelliSpace Portal<sup>®</sup>, Philips Healthcare). Maximum  
130 intensity projections (MIP) and curved planar reformations  
131 (CPR) were performed for each patient.  
132

### Evaluation of objective image quality

133 All experimental measurements were performed by an  
134 experienced radiologist with 10 years of CTA experience.  
135 The intravascular attenuation was measured on the axial  
136 images at the following locations: abdominal aortic bifurca-  
137 tion (AAB), bilateral common iliac arteries (CIA), common  
138 femoral arteries (CFA), middle superficial femoral arteries  
139 (MSFA) and middle popliteal artery (MPA). Within the ves-  
140 sels, the region of interest (ROI) was defined as large as  
141

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