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Polymeric nanoparticles for optical sensing 06

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ARTICLE INFO

ABSTRACT

7 8 9 10 11 13	Article I Receive Receive Accepte Availab	history: Nanotechnology is a powerful tool for use in diagnostic applications. For these purposes a variety of functional 23 nanoparticles containing fluorescent labels, gold and quantum dots at their cores have been produced, with 24 the aim of enhanced sensitivity and multiplexing capabilities. This work will review progress in the application 25 of <i>polymeric</i> nanoparticles in optical diagnostics, both for <i>in vitro</i> and <i>in vivo</i> detection, together with a discussion 26 of their biodistribution and biocompatibility. 27				
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1. Introduction - nanotechnology and optical diagnostics 07

In the past decade, progress in nanotechnology has produced a wide 48 variety of nanoparticles (NPs) useful for diagnostic applications. The use 4950of nanotechnology in diagnostics is attractive because only a small volume of sample is required, allowing a low limit of detection (LOD) 51to be achieved. Often the use of NPs in diagnostic tests makes them 52faster to perform and more sensitive than comparable assays which 53use biomolecules (Jain, 2005). Furthermore, NPs possess unique optical 54 55and magnetic properties depending on their composition. Moreover, according to their intended application, nanoparticles can be engineered 56

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to impart the required properties. The use of NPs in molecular diag- 57 nostics can be termed "nanodiagnostics" and has been successfully 58 employed both in vivo and in vitro assays (Jain, 2007). In recent years, 59 the global market for in vitro diagnostics (IVD) has increased at an 60 incredible rate; from US\$44 billion in 2010 to a predicted US\$60 billion 61 by the end of 2014 (Renub-Research, 2010). The "point-of-care" sector 62 represents the largest part of the IVD global market, followed by immu- 63 nochemistry and molecular diagnostics (RNCOS, 2011). 64

Currently the most important application areas for polymeric NPs in 65 optical diagnostics are biomarker analysis, cancer diagnosis, diagnostic 66 imaging, and immunoassays. The binding of the target biomolecule to 67 NPs is the pivotal step in most nanoparticle-based assays. In order to 68 detect the target analyte, this binding should result in a measurable 69 signal that can be quantified. For this purpose, the most commonly 70

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used labels are enzymes, which can catalyze the formation of colored 7172products that can be detected by a change in color of a solution, or molecules/materials capable of emitting a fluorescent signal. Dyes 73 74 have been popular tools employed in optical diagnostics, allowing the detection of analytes with good sensitivity, either through color 7576changes or by emission of fluorescence. Unfortunately, dyes suffer 77 from photobleaching and often have an asymmetric emission spectrum. 78 Photostability is important in the case of prolonged observation, where 79photobleaching severely impacts on their capability to detect single 80 molecules. Furthermore some dyes, such as fluoresceins and rhodamines, suffer from quenching phenomena when present in solution at 81 high concentration (Demchenko, 2010). Despite the aforementioned 82 drawbacks, organic dyes are widely employed due to their low cost 83 and ease of use. When the dye is embedded in a polymeric matrix how-84 ever, increased photostability is often observed due to the "protective" 85 86 effect of the polymer. Furthermore, covalently coupling the dye to the polymer will also reduce the chance of leakage, which is possible with 87 entrapped dyes, which can still diffuse out of the polymer. NPs can 88 also contain hundreds of dye molecules which will increase the intensity 89 of color or the brightness of emission. Furthermore, the hydrophobic mi-90 91 croenvironment created within polymeric NPs can enhance the guantum 92vield of certain fluorescent reporters (Cui et al., 2013; Hu and Liu, 2010; 93 Shiraishi et al., 2010; Wang et al., 2009). In addition, the presence of reactive functional groups along the polymer backbone allows specific 94 labeling with other molecules as well as allowing the particle surface 95to be modified for specific applications. 96

97 Reporters for optical sensing can be divided into two main catego-98 ries. The first includes reporters used as molecular sensors in systems capable of detecting changes in their surroundings and respond to 99 the presence of specific molecules. The second involves reporters used 100 101 as labels, the aim of which is to give rise to a fluorescent signal which depends only on the presence of the reporter in a particular area of a 102103 diagnostic device, without any variation in the fluorescence properties (Demchenko, 2010). The most important considerations when using 104 labels are how to obtain high brightness and provide protection from 105106 the surrounding environment. The ideal molecular sensor should pos-107 sess high molar absorption coefficient and high quantum yield, it should be photochemically and thermally stable, and give an optical response 108 proportional to the concentration of the target analyte without any 109 interactions with other analytes in the sample. A large Stokes shift is 110 highly desirable for both applications because it allows the fluorescent 111 112 signal to be detected without problems associated with the overlapping of excitation and emission spectra of the dye (Demchenko, 2005). 113

For *in vivo* use, reporters must be non-toxic and their biodistribution 114 should be well-known. Herein, we describe recent advances in the syn-115 thesis and applications of polymeric NPs in optical *in vitro* and *in vivo* 116 diagnostics.

2. Synthesis of polymeric nanoparticles

118

Polymeric NPs can be made from organic polymers or inorganic 119 materials such as silica. Generally, organic NPs are prepared either by 120 polymerization of monomers or by processing of preformed polymers. 121 In the latter case, the techniques most frequently employed are: solvent 122 evaporation, salting-out, nanoprecipitation, dialysis and supercritical 123 fluid technology (Rao and Geckeler, 2011). Otherwise, polymeric NPs 124 can be produced from monomers by several methods, such as: disper- 125 sion, precipitation and interfacial polymerizations. For diagnostic appli- 126 cations, the most commonly employed techniques are emulsion and 127 living free radical polymerization. The former is carried out in water 128 as the dispersion medium, with or without the addition of surfactant, 129 and allows excellent control to be exerted over the size distribution of 130 the NPs produced, including the production of monodisperse emulsions. 131 Similarly, the living free radical polymerization methods permit excel- 132 lent control over the molecular weight, polydispersity and composition 133 of NPs (Zetterlund et al., 2008). These latter procedures are based on the 134 establishment of dynamic equilibria between a small number of grow- 135 ing radicals and a large majority of the dormant species. Even though 136 this method can have some issues related to the colloidal stability of 137 NPs, living polymerization is an excellent technique for the production 138 of functionalized NPs. Moreover, in contrast to conventional free radical 139 polymerizations, living polymerizations do not undergo exothermic 140 autoacceleration, allowing superior control of parameters such as the 141 polymer chain length and particle size. 142

Silica NPs are generally synthesized either in an emulsion-based 143 technique performed in organic solvents or by the Stöber method. The 144 first process requires large amounts of surfactant, whereas the Stöber 145 method is performed in a mixture of water and ethanol in the absence 146 of surfactants and allows spherical NPs to be obtained in a narrow size 147 distribution. It was recently shown however that the silica layer present 148 on NPs produced by the Stöber method can be inhomogeneous (Wong 149 et al., 2011). In both approaches for the synthesis of NPs, dye can be 150 added to the monomer mixture prior to initiating the polymerization, 151 with the results that it becomes entrapped within the polymeric matrix. 152 Copolymerization with a polymerizable form of the dye can eliminate 153 the leaching of dye from the particle, but generally has a requirement 154

t1.1 Table 1

Q4 Comparison of the most frequently employed methods for the synthesis of NP for biomedical application.

t1.3	Organic nanoparticles					
t1.4	Synthetic method	Particle size/initiator	Advantages	Drawbacks/issues		
t1.5	Mini- and micro-emulsion polymerization	10–200 nm Initiator: persulfate; azoisobutyronitrile	Performed both in water and organics. Good monodispersity	Size control. Surfactant needed to obtain smaller particles		
t1.6	Living radical polymerization	30–300 nm Initiator: alkoxyamines, thioesters, alkyl halides, iniferters	Performed both in water and organics. Ideal for synthesis of functionalized nanoparticles	Residues of initiator and surfactant (if employed). Colloidal stability		
t1.7	Precipitation and dispersion polymerization	200 nm–10 µm Initiator: persulfate; azoisobutyronitrile	With/without surfactant. Moderate-good monodispersity	Size control. Possible irregular shape. Difficult to obtain particles < 200 nm		
t1.8 t1.9	Inorganic nanoparticles					
t1.10	Synthetic method	Particle size/catalysis	Advantages	Drawbacks/issues		
t1.11	Microemulsion polymerization	10–70 nm Basic catalysis	Good monodispersity	Presence of surfactant. Performed in organics		
t1.12	Sol-gel method	50 nm–2 μm Acid/basic catalysis	Good monodispersity	Presence of surfactant		
t1.13	Stöber method	15 nm–2 μm Basic catalysis	Surfactant-free excellent monodispersity	Difficult to obtain particles <50 nm		

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