

Nanomedicine: Nanotechnology, Biology, and Medicine xx (2015) xxx-xxx NANO-01170; No of Pages 6

Nanotechnology, Biology, and Medicine

nanomedjournal.com

Citrem modulates internal nanostructure of glyceryl monooleate dispersions and bypasses complement activation: Towards development of safe tunable intravenous lipid nanocarriers

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Received 29 June 2015; accepted 18 August 2015

11 Abstract

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Lyotropic non-lamellar liquid crystalline (LLC) aqueous nanodispersions hold a great promise in drug solubilization and delivery, but these nanosystems often induce severe hemolysis and complement activation, which limit their applications for safe intravenous administration. Here, we engineer and characterize LLC aqueous nanodispersions from a binary lipid mixture consisting of 2,3-dihydroxypropyl oleate (glyceryl monooleate) and medium-chain triglyceride with tunable internal nanostructures and improved hemocompatibility controlled by citrem as stabilizer. Citrem, in a concentration-dependent manner, modulates the internal nanostructure of LLC dispersions from a biphasic H_2/L_2 feature to a neat L_2 phase, where the latter resembles "thread-like" swollen micelles. Citrem stabilization totally overcomes hemolysis and complement activation, thus realizing the potential of the engineered LLC aqueous nanodispersions for exploitation in intravenous delivery of drugs and contrast agents.

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20 Key words: Citrem; Complement system; Hierarchical materials; Hexosomes; Synchrotron small-angle X-ray scattering (SAXS)

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Competing interests: The authors declare no competing financial interest.

Author contributions: PPW, AY and SMM conceived the idea; IDMA and CN prepared and characterized hexosome preparations by SAXS and cryo-TEM; PPW conducted complement, hemolysis, and size determination experiments; all authors were involved in data analysis and interpretation; PPW and SMM wrote the manuscript.

Financial support by the Danish Council for Independent Research (Technology and Production Sciences), reference 1335-00150b (to AY and SMM) and reference 09-065746/DSF (to SMM) is gratefully acknowledged. PPW is a recipient of a PhD Scholarship Award from the Faculty of Health and Medical Sciences, University of Copenhagen. IDMA is a recipient of a PhD Scholarship Award from the Ministry of Higher Education of Malaysia (MOHE). We also thank Ana Labrador (MAX laboratory, Lund, Sweden), and Klaus Qvortrup (Core Facility for Integrated Microscopy, University of Copenhagen) for their valuable technical assistance on SAXS and cryo-TEM studies, respectively.

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http://dx.doi.org/10.1016/j.nano.2015.08.003 1549-9634/© 2015 Published by Elsevier Inc.

Lyotropic non-lamellar liquid crystalline (LLC) aqueous 22 dispersions of cubosome and hexosome classes exhibit highly 23 ordered and thermodynamically stable internal tunable nano- 24 structures with attributes that make them promising candidates 25 for solubilization of zwitterionic, charged and hydrophobic 26 drugs.^{1,2} However, compatibility of these lipid systems with 27 elements of the human blood remains poor, and therefore in need 28 of optimization.³⁻⁵ For instance, the commonly used phytantriol 29 (PT)-based lipid dispersions induce hemolysis.³ Tri-block 30 copolymers such as Pluronic® F127 as well as PEGylated and 31 polyethoxylated fatty acids are widely used for stabilization of 32 cubosomes and hexosomes, ⁵⁻⁹ but such stabilizers activate the 33 human complement system in both micellar and surface 34 immobilized forms.¹⁰⁻¹² The complement system is the first 35 line of the body's defense against intruders, where its inadvertent 36 activation may contribute to adverse reactions with cardiovas- 37 cular, bronchopulmonary, mucocutaneous, neuropsychosomatic 38 and autonomic manifestations.^{12,13} Indeed, such reactions have 39 been noted in some patients receiving intravenous infusion of 40

Please cite this article as: Wibroe P.P., et al., Citrem modulates internal nanostructure of glyceryl monooleate dispersions and bypasses complement activation: Towards development.... *Nanomedicine: NBM* 2015;xx:1-6, http://dx.doi.org/10.1016/j.nano.2015.08.003

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t1.1 Table 1t1.2 Composition and biophysical characteristics of the LLC aqueous nanodispersions.

	*	* *		*	*							
t1.3	LLC dispersion	GMO:MCT	Lipid content (wt%)	Stabilizer	Stabilizer content (wt%)	Medium ^a	Phase	<i>d</i> (nm)	<i>a</i> (nm)	Mean diameter ^b (nm)	Median diameter ^b (nm)	
t1.4	LD _{F127}	90:10	10	F127	3	Buffer	H ₂	_	5.45	94 ± 8	82	
						Serum	H_2	-	5.52	118 ± 22	101	t1.5
t1.6	LD _{citrem1.5}	85:15	5	Citrem	1.5	Buffer	H_2/L_2	_	5.82	147 ± 10	142	
						Serum	H_2/L_2	_	6.09	_	_	t1.7
t1.8	LD _{citrem3.0}	85:15	5	Citrem	3	Buffer	L_2	5.40	-	119 ± 8	103	
						Serum	L ₂	6.47	_	127 ± 13	120	t1.9

t1.10 GMO: glyceryl monooleate; MCT: medium-chain triglycerides; d: characteristic distance; a: lattice parameter.

t1.11 ^a For incubation conditions see the experimental section.

t1.12 ^b Determined by Nanoparticle Tracking Analysis (NTA).

lipid- and polymer-based nanomedicines, including longcirculating formulations.^{12,13} Here, we describe a simple strategy
in LLC aqueous nanodispersion engineering with tunable
internal nanostructures and improved hemocompatibility. These
engineered nanostructures bypass hemolysis and do not incite
complement, thus realizing their potential for exploitation in
intravenous delivery of drugs and contrast agents.

48 Methods

Details for the preparation of lipid dispersions and their characterization by Nanoparticle Tracking Analysis, cryogenic transmission electron microscopy (cryo-TEM), and synchrotron small-angle X-ray scattering (SAXS) were reported before,¹⁴ and presented in the supplementary material. Details for the hemolysis test and complement activation studies were in accordance with our previous studies^{10,15} (Supplementary Material).

56 Results and Discussion

We used a binary lipid mixture consisting of 2,3-dihydroxypropyl 57oleate (glyceryl monooleate, GMO), which is the most investigated 58surfactant-like lipid with a non-lamellar propensity, and medium-59chain triglyceride (MCT) to form LLC aqueous nanodispersions 60 stabilized with citrem¹⁴ (LD_{citrem}), Table 1. Citrem is an anionic citric 61 acid ester of monoglycerides, which has been approved by the United 62 States Food and Drug Administration as an emulsifying agent in food 63 products.¹⁴ For comparison, we prepared GMO/MCT nanodisper-64 sions stabilized with the most commonly used stabilizer Pluronic® 65 F127 (LD_{F127}). The SAXS pattern for LD_{F127} showed three Bragg 66 reflections ((10), (11) and (20)) characteristic for an internal inverted 67 hexagonal (H₂) phase (hexosomes),¹⁶ Figure 1, A, and this finding 68 was supported by cryo-TEM (Figure 1, D). On the contrary, with a 69 dispersion stabilized with 1.5 wt% citrem (LDcitrem1.5) there was an 70 increase in the lattice parameter of the internal H₂ phase from 5.45 71 72to 5.82 nm showing an additional broad peak at $q \sim 1 \text{ nm}^{-1}$ (Figure 1, B). This indicates co-existence of a less ordered internal 73inverted-type microemulsion (internal L₂ phase).¹⁷ However, 74 increasing citrem concentration to 3 wt% (LDcitrem3.0) transformed 75the internal biphasic H_2/L_2 structure to a neat L_2 phase (emulsified 76microemulsions, EMEs). The identification of this phase was based 77

on the detection of a single broad peak at $q = 1.16 \text{ nm}^{-1}$. On the 78 basis of cryo-TEM observations we suggest that the interior 79 nanostructure of EME closely resembles "thread-like" swollen 80 micelles (Figure 1, *D*). Citrem may incorporate into the hydrophobic 81 domain of the internal GMO/MCT nanostructure as well as in the 82 water/GMO interface due to its surface-active property. Accord-83 ingly, the aforementioned transition is most likely regulated by the 84 extent of citrem incorporation into the hydrophobic GMO/MCT 85 domains, thereby modulating the critical packing parameter, and 86 consequently increasing the negative mean curvature.¹⁴ 87

On serum incubation (4 h, 37 °C), the internal H₂ nanostruc- 88 ture of LD_{F127} was retained, but showed a slight increase in the 89 lattice parameter of the H₂ phase (from 5.45 to 5.52 nm) 90 (Figure 1, C, Table 1, Supplementary Figure S1). Both citrem- 91 stabilized nanodispersions also showed swelling of the internal 92 structure on serum incubation, as viewed by an increase in the 93 lattice parameter (a) of the internal H_2 phase and the 94 characteristic distance (d) of the internal L₂ phase (Figure 1, C, 95 Table 1, Supplementary Figure S2). With LD_{citrem3.0}, the 96 increase in d was dramatic (from 5.40 to 6.47 nm, corresponding 97 to 19.8%), whereas with LD_{citrem1.5} the lattice parameter of the 98 internal H₂ phase was increased marginally (from 5.82 to 99 6.09 nm, corresponding to 4.6%). This notable enlargement of 100 the L_2 phase may arise either from interaction of the interior 101 nanostructure of GMO/MCT with serum components and/or 102 trapping of serum proteins in the aqueous core of the "swollen" 103 inverted type micelles (Figure 1, E). Accordingly, the microen- 104 vironmental conditions of the hydrophilic cylindrical nanochan- 105 nels of the H₂ phase limits trapping of large amount of serum 106 components, since only a slight serum-mediated enlargement of 107 the hydrophilic pores is detectable.

Next, we compared membrane disruptive properties of 109 LD_{F127} and $LD_{citrem3.0}$ by examining erythrocyte lysis in fresh 110 human whole blood (WB) (Figure 2). We chose lepirudin as an 111 anticoagulant (a specific thrombin inhibitor), which has no effect 112 on membrane integrity and the complement system.¹⁸ LD_{F127} 113 showed concentration-dependent hemolysis in the WB with a 114 significant membrane damage even at low lipid concentration 115 (0.05 wt%). In the absence of plasma, hemolysis was consider- 116 ably higher, starting at a lipid concentration of 0.01 wt%. In 117 contrast, $LD_{citrem3.0}$ did not induce hemolysis in the WB even at a 118 high lipid concentration (0.20 wt%), but hemolysis could 119 proceed in the absence of plasma (a non-physiological condition) 120

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