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Numerical investigation of ultrasound reflection and backscatter measurements in cancellous bone on various receiving areas

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ABSTRACT

In this study, new ultrasound reflection and backscatter measurements in cancellous bone using a membrane-type hydrophone are proposed. A membrane hydrophone made of a piezoelectric polymer film mounted on an annular frame allows an incident ultrasound wave to pass through its aperture because it has no backing material. Therefore, in measurements using the membrane hydrophone, the receiving area could be located independently from the transmitting area. In addition, the size and shape of the receiving area, which corresponded to those of the electrode deposited on the piezoelectric film, could be arranged in various ways. To investigate the validity of the proposed measurements, before bench-top experiments, the reflected and backscattered waves from cancellous bone were numerically simulated using a finite-difference time-domain method. The reflection and backscatter parameters were measured on various receiving areas, and their correlation coefficients with the structural parameters in the cancellous bone were derived. The simulated results suggested that appropriate receiving areas for the reflection and backscatter measurements could exist and that the proposed measurements could be more effective for evaluating bone properties than conventional measurements.

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1. Introduction

Various ultrasound measurements in bone have been studied to establish accurate and precise quantitative ultrasound (QUS) techniques for clinical assessment of bone quality [1–4]. Among these, ultrasound reflection and backscatter measurements in cancellous bone have been attempted [4–6] because of their easy applicability to skeletal sites where through-transmission measurements are difficult. The reflected and backscattered waves are generally received using only one transducer that acts as both transmitter and receiver in pulse-echo mode. Thus, the sizes, shapes, and locations of the transmitting and receiving areas must be the same; however, independent arrangement of the receiving area is desirable to effectively detect the wave characteristics associated with the bone properties.

In this study, new reflection and backscatter measurements in cancellous bone are proposed in which a membrane-type hydrophone is inserted between the ultrasound transmitter and the bone. The membrane hydrophone is composed of a piezoelectric polymer film and an annular frame without a backing material, which allows an incident ultrasound wave to pass through its aperture [7,8]. The advantage of the technique is that when the membrane hydrophone is used, the receiving area can be easily

changed, which was the advantage in the proposed measurements. It is difficult to verify an ultrasound measurement in bone because an immense number of experiments are required owing to the variability in bone structure. Numerical simulations are helpful as a surrogate for experiments [9,10]. Thus, by using a finite-difference time-domain (FDTD) method [11–14], the reflected and backscattered waves from the cancellous bone were numerically simulated for various receiving areas. The correlations of the reflection and backscatter parameters with the structural parameters of the cancellous bone—specifically the porosity and mean intercept lengths (MILs) [15] of the trabecular elements and pore spaces—were investigated to demonstrate that the dependences of QUS parameters on bone properties can change with the receiving areas.

2. Ultrasound measurements using a membrane hydrophone

2.1. Membrane hydrophone

Piezoelectric polymer films such as poly(vinylidene fluoride) are a suitable piezoelectric material for an ultrasound receiver in water (namely hydrophone) because their acoustic impedances are relatively close to the impedance of water. Hydrophones made of piezoelectric films can be classified into two types: needle-type [16] and membrane-type [7,8]. The former is composed of the piezoelectric film and a cylindrical backing material, and the latter is composed of the film and an annular frame. A schematic of the

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84 construction of the membrane hydrophone is shown in Fig. 1. In
85 the case of the general construction in Fig. 1(a), circular and linear
86 electrodes are deposited on the piezoelectric film. The circular
87 electrodes on either surface overlap, but the linear electrodes are
88 separated. Therefore, an incident ultrasound wave can be received
89 only in the circular area, which corresponds to the receiving area.
90 In a membrane hydrophone, various receiving areas can be easily
91 realized by changing the overlapping area of the electrodes, as in
92 the annular area in Fig. 1(b). Moreover, as shown in Fig. 1, no material
93 exists on the back of the receiving area.

94 2.2. Measurement of reflected and backscattered waves

95 Fig. 2 illustrates the method of measuring the reflected and
96 backscattered ultrasound waves from cancellous bone using the
97 membrane hydrophone. The hydrophone was arranged between
98 the needle-type ultrasound transmitter and the cancellous bone
99 in water. Because the acoustic impedance of the hydrophone's piezo-
100 electric film was close to that of water, the transmitted ultra-
101 sound wave could pass through the film and arrive at the cancellous
102 bone. The reflected and backscattered waves from the
103 bone were received by the membrane hydrophone.

104 If the inner diameter of the annular frame mounting the piezo-
105 electric film is sufficiently larger than the diameter of the ultra-

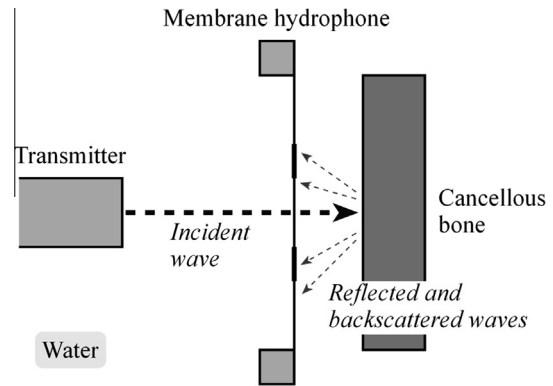


Fig. 2. Method of measuring reflected and backscattered ultrasound waves from cancellous bone using a membrane hydrophone.

106 sound beam, the membrane hydrophone cannot significantly
107 disturb the ultrasound field. The half-width 2θ of the ultrasound
108 beam (wavelength: λ) transmitted from a circular flat surface
109 (diameter: $2a_t$) is approximated as
110

$$2\theta \approx 2 \arcsin \left(0.705 \frac{\lambda}{a_t} \right), \quad (1)$$

113 and the beam diameter $2a_b$ at a distance d from the transmitter is
114 calculated as
115

$$2a_b \approx 2d \tan \theta. \quad (2)$$

118 For example, for $\lambda = 1.48$ mm at a frequency of 1 MHz in water,
119 $2a_t = 10$ mm, and $d = 40$ mm, the calculated $2a_b$ is approximately
120 17.1 mm; thus, an inner diameter of 20 mm is adequate for the
121 annular frame. Practically, a smaller inner diameter is acceptable
122 because a focused transmitter is generally used in QUS apparatuses
123 for bone assessment.

124 3. Numerical simulations of reflection and backscatter
125 measurements

126 3.1. Simulation model

127 Three-dimensional (3D) FDTD simulations of reflection and back-
128 scatter measurements using the membrane hydrophone were per-
129 formed using self-made FDTD software [14]. The simple
130 simulation model was constructed with consideration of *in vitro*
131 experiments, which will be performed for comparison between
132 the experimental and simulated results in the future. A cross-
133 sectional view of the simulation model is shown in Fig. 3. This model
134 had a spatial interval of $57 \mu\text{m}$ and consisted of cancellous bone
135 and water regions, whose dimensions were $5.016 \times 6.84 \times$
136 6.84 mm^3 ($88 \times 120 \times 120$ points) and $7.98 \times 6.84 \times 6.84 \text{ mm}^3$
137 ($140 \times 120 \times 120$ points), respectively. In Fig. 3, the x -direction cor-
138 responds to the direction of ultrasound transmission, and the y -
139 z plane corresponds to the cancellous bone surface.

140 The transmitting area with a rigid backing material had a circular
141 concave shape with a diameter of 5.7 mm (100 points), which
142 was set at the center of the y - z plane at $x = 0$ mm at a distance
143 of 7.98 mm (140 points) from the cancellous bone surface. The fo-
144 cal distance was 10.488 mm (184 points), which corresponded to
145 the focal point 2.508 mm (44 points) inside of the cancellous bone.
146 The transmitted waveform was a single sinusoid at 1.0 MHz multi-
147 plied by a Hanning window (note that the center frequency was
148 shifted to approximately 1.25 MHz owing to the window). Its time
149 interval was 4 ns. At $x = 0, 1.995, 3.99,$ and 5.016 mm (0, 35, 70, and
150 88 points) from the transmitting area [7.98, 5.985, 3.99, and
151 2.964 mm (140, 105, 70, and 52 points) from the cancellous bone

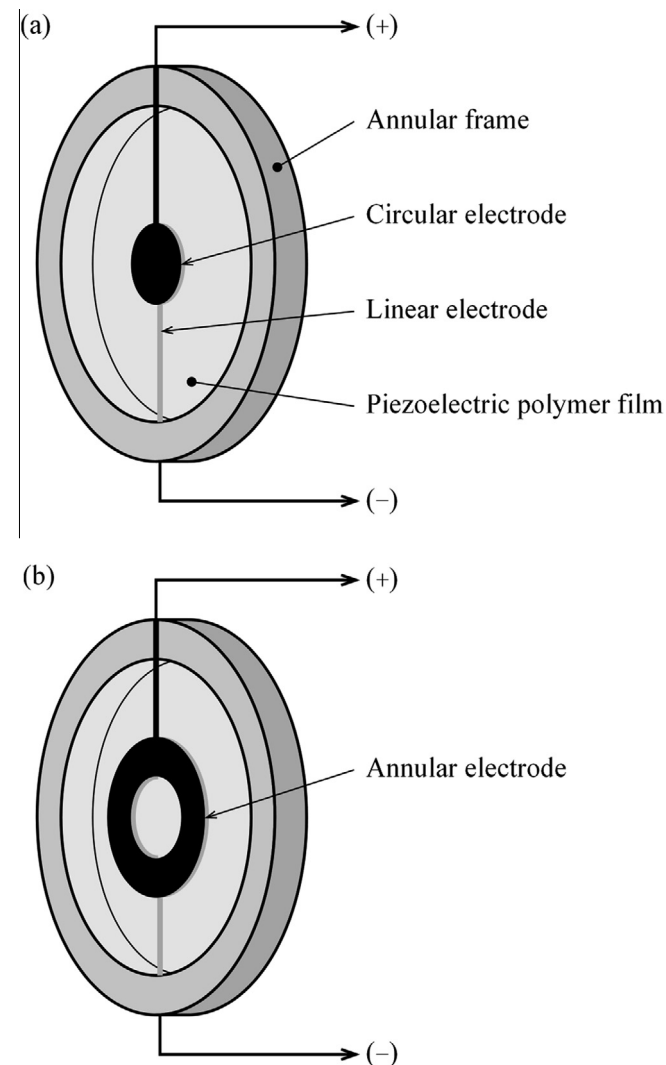


Fig. 1. Schematic construction of membrane hydrophones with (a) circular and (b) annular receiving areas.

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