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A ratiometric fluorescent probe based on boron dipyrromethene and rhodamine Förster resonance energy transfer platform for hypochlorous acid and its application in living cells





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HIGHLIGHTS

- A probe based on BODIPY and rhodamine was developed for sensing HOCI.
- The probe could sense HOCl in a ratiometric manner based on the FRET platform in PBS buffer solution.
- The probe can detect HOCl in 15 s accompanied with a fluorescence colour change.
- This probe was successfully used to monitor HOCl in living RAW 264.7 cells.

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G R A P H I C A L A B S T R A C T



ABSTRACT

We have developed a ratiometric fluorescent probe **BRT** based on boron dipyrromethene (BODIPY) and rhodamine-thiohydrazide Förster resonance energy transfer (FRET) platform for sensing hypochlorous acid (HOCl) with high selectivity and sensitivity. The probe can detect HOCl in 15 s with the detection limit of 38 nM. Upon mixing with HOCl the fluorescence colour of probe **BRT** changed from green to orange. Moreover, probe **BRT** was applied to successfully monitor HOCl in living RAW 264.7 cells. © 2016 Elsevier B.V. All rights reserved.

1. Introduction

Hypochlorous acid (HOCl)/hypochlorite (⁻OCl) is known to be one of the reactive oxygen species (ROS) [1], which plays a vital role in many physiological processes. In our daily life, HOCl is used as disinfectant, deodorant, and bleaching agent [2–4]. Biologically, endogenous HOCl is generated from hydrogen peroxide and chloride ion by the enzyme myeloperoxidase (MPO) catalysis in

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activated leukocytes including neutrophils, macrophages and monocytes [5,6]. And it contributes to the human immune defence system, and plays an important role in killing a wide range of bacteria and pathogens in cells [7]. However, much evidence suggests that once the level of endogenous HOCl is higher than normal, that may cause some diseases, such as inflammatory, atherosclerosis, rheumatoid arthritis, respiratory distress, cardiovascular diseases and even cancer [8–15].

In the last decade, scientists have focused on much effort to the development of methods for the recognition of HOCl including chemiluminescence, electroanalysis and potentiometry [16-20]. Fluorescent probes have attracted great attention because of their high selectivity, high sensitivity, low cost, real-time essay and most important of all they can provide not only in vitro detection but also in vivo imaging studies [21-30]. A considerable number of fluorescent probes have been reported for the sensing of HOCl by the modification of common fluorophores such as fluorescein [31–33], coumarin [34,35], cyanine [36], BODIPY [37,38], rhodamine [39,40] and so on [41-47]. However, most of them are intensity-based fluorescent probes and these probes may be affected by the factors such as environment variations, instrumental efficiency and sensor concentrations. In contrast, ratiometric fluorescent probes employing the signal ratios at two wavelengths can alleviate the above problems and provide accurate analysis [48,49].

Inspired by the Förster resonance energy transfer (FRET) mechanism [50], we designed and synthesized a ratiometric fluorescent probe **BRT** for the detection of HOCI. In this new FRET system, BODIPY performed as the donor, rhodamine-thiohydrazide acted as the acceptor. Probe **BRT** can respond to HOCI under acid conditions by the reaction of thiohydrazide with HOCI [51], accompanied with the fluorescence intensity of BODIPY decreases and the fluorescence intensity of rhodamine gradually increases at the typical excitation of BODIPY fluorophore. Therefore, probe **BRT** can sense HOCI in a ratiometric manner by recording the ratios of emissions of the two fluorophores. Further, we found that probe **BRT** can be applied to monitor HOCI with high selectivity, sensitivity and low detection limit (38 nM). More importantly, probe **BRT** has been successfully used in imaging of endogenous HOCI in living cells.

2. Experimental

2.1. Materials and instrumentations

All reagents were purchased from commercial suppliers and used without further purification. TLC was conducted on silica gel 60 F₂₅₄ plates (Merck KGaA). ¹H NMR and ¹³C NMR spectra (400 and 100 MHz) were recorded on a Bruker Avance 400 spectrometer using tetramethylsilane (TMS) as an internal standard with DMSO*d*6 as a solvent. IR spectra were determined with an IR spectrophotometer VERTEX 70 FT-IR (Bruker Optics). UV–vis spectra were recorded on a U-4100 spectrophotometer (Hitachi). Fluorescence measurements were recorded on a Perkin–Elmer LS-55 luminescence spectrophotometer. HRMS spectra were recorded on a Q-TOF6510 spectrograph (Agilent). All pH measurements involved the use of a Model PHS-3C pH meter (Shanghai) at room temperature about 298 K. Deionized water was used throughout the experiment.

2.2. Preparation of ROS and RNS

Various ROS and RNS including NaOCl, H_2O_2 , *t*-BuOOH, •OH, *t*-BuO·, NO, ONOO⁻, $^-O_2$, 1O_2 were prepared according to the following methods. Sodium hypochlorite (NaOCl), H_2O_2 and *tert*-butylhydroperoxide (*t*-BuOOH) were diluted from the commercially available solution to 0.1 M in water. Hydroxyl radical (·OH)

was generated by Fenton reactions by mixing $FeSO_4 \cdot 7H_2O$ with 1 equivalent of H_2O_2 , the concentration of $\cdot OH$ was estimated from the concentration of Fe^{2+} .

Tert-butoxy radical (*t*-BuO·) was prepared according to Fenton reactions by mixing FeSO₄·7H₂O with 1 equivalent of *tert*-butyl-hydroperoxide (*t*-BuOOH), the concentration of *t*-BuO· was estimated from the concentration of Fe²⁺.

Nitric oxide (NO) was generated from potassium nitroprusside dehydrate. Peroxynitrite (ONOO⁻) was prepared according to the reported method [52]. Superoxide ($^{-}O_2$) was generated from KO₂ according to the literature [53]. Singlet oxygen $^{1}O_2$ was generated on mixing of NaOCl with 2 equivalent of H₂O₂ according to the literature [54].

2.3. General procedure for the measurement of absorption and fluorescence spectra

A 1.0×10^{-3} M stock solution of probe **BRT** was prepared in EtOH. Proper amounts of probe **BRT** solution were added directly with a micropipette to 10 mL glass tube, the solutions were diluted to 10 mL with PBS (pH = 5) and EtOH (v/v, 4:6), different amounts of NaOCl were added directly with a micropipette to the above solutions. Then the absorption and fluorescence measurements were run.

2.4. Detection limit calculation and the efficiency of energy transfer (EET)

Detection limit for HOCl was calculated by Eq. (1):

Detection limit =
$$3\sigma/m$$
 (1)

where σ = standard deviation of 10 blank measurements and m = slope obtained from the graph of fluorescence intensity ratio vs concentration of HOCI [55].

The efficiency of energy transfer (EET) was calculated according to Eq. (2):

$$\eta_{\text{EET}} = 1 - \Phi_{\text{F(donor in FRET system)}} / \Phi_{\text{F(donor)}}.$$
(2)

where η_{EET} is the efficiency of energy transfer. $\Phi_{\text{F}(\text{donor in FRET system})}$ is the fluorescence quantum yield of the donor part in FRET system (BODIPY part in compound **BRA** in this work), $\Phi_{\text{F}(\text{donor})}$ is the fluorescence quantum yield of the donor when the FRET system is blocked (BODIPY part in probe **BRT** in this work) [56] and the fluorescence quantum yield was calculated according to the literature [57].

2.5. Cytotoxicity assay

The standard sulforhodamine B (SRB) assay was performed to examine the cytotoxicity of probe **BRT** in RAW264.7 cells. Briefly, RAW264.7 cells were cultured in 96-well culture plates for 12 h, and then incubated with DMEM containing different concentration of probe **BRT** (1, 5, 10 μ M) for 12 h. The cells were fixed with 4% TCA for 1 h at 4 °C, then washed 5 times with deionized water. SRB (50 μ L) was added to each well, and after sufficient reaction with cells, the remaining SRB was removed by washing each well with 1% acetic acid solution, then 100 μ L Tris–HCl was used to dissolve the SRB. Absorbance at 540 nm was measured in a 96-well multi well-plate reader (TECAN).

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