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Should we be concerned about composite (nano-)dust?

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ABSTRACT

Dental personnel often come into contact with composite dust upon polishing or grinding composites. Contemporary composites typically contain high amounts of (silica) nano-filler, but so far it has never been investigated whether composite dust may be hazardous.

Objectives. The objectives of this study were (1) to characterize composite dust in vitro and (2) to assess the clinical exposure.

Methods. Polymerized blocks of contemporary composites were ground with a diamond bur according to a clinically relevant protocol, and aerosolized dust was collected on 1- μm pore-size filters and gravimetrically quantified. In addition, the dust was characterized by transmission electron microscopy. Respirable dust was quantified with a mass particle counter in a dental operatory.

Results. All composites released respirable dust ($<5\ \mu\text{m}$) in vitro. These observations were corroborated by the clinical measurements; however only short episodes of high concentrations of respirable dust upon polishing composites could be observed. Electron microscopic analysis showed that the size of the dust varied widely with particles larger than $10\ \mu\text{m}$, but submicron and even nano-sized particles could also be observed. The dust particles often consisted of multiple filler particles contained in resin, but single nano-filler particles could also frequently be distinguished.

Significance. This study showed that inhalation of composite dust is better avoided. Therefore, it is recommended to always use water-cooling upon polishing or removing composites, to use good aspiration, to frequently ventilate the dental operatory and to wear masks with high particle-filtration efficiency for small particle sizes.

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1. Introduction

Tooth tissue lost due to trauma or caries is nowadays preferentially replaced with composite. Dental composites typically

contain (photo-)polymerizable resins and inorganic filler particles that are functionalized with a silane coupling agent to attach them to the resin matrix [1]. The size of the filler particles varies widely, but contemporary composites may contain large quantities of sub-micron and even nano-particles.

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Typically, 40-nm-sized pyrogenic silica ('microfill') is very often used [2]. The most recent class of composites is coined 'nano-composites', as they contain larger amounts of amorphous nano-particles (<100 nm) than traditional 'hybrid composites'. Beside pyrogenic silica, they also contain filler produced in a sol-gel process, which are typically composed of mixed oxides, like ZrO_2-SiO_2 , and which can be added to a greater extent without overly increasing the viscosity of the unpolymerized composite.

Like in other fields of industry involving nano-technology [3], some dental researchers and practitioners have expressed concerns that there may be health risks connected to the use of these nano-particles [4]. Dental personnel may inhale aerosolized composite dust while shaping and polishing new composite restorations, and upon removal of old composite restorations [5]. Especially in case of inadequate aspiration and/or lack of assistance, dental professionals (and patients) may be exposed to composite dust. In general, dust smaller than $5\ \mu\text{m}$ and larger than $0.01\ \mu\text{m}$ may be respired and can penetrate deep into the alveolar region of the lungs, beyond the body's natural mechanisms of cilia and mucous clearing [6]. Chronic inhalation of respirable dust (< $5\ \mu\text{m}$) and nano-particles may provoke both local and systemic toxicity [6,7]. Excessive and long-term exposure to respirable dusts can induce pneumoconiosis [8], a chronic lung condition marked by nodular fibrosis. Nano-particles (<100 nm) may also be absorbed in the blood or the lymphatic system resulting in systemic toxicity [9–11].

Two decades ago, Collard et al. showed that respirable crystalline silica could be released upon abrading traditional quartz-containing composites (which are now no longer commonly used) [12]. So far, the potential of contemporary composites to release respirable (nano-)dust has never been explored.

The objective of this study was to assess the potential of contemporary composites including nano-composites to release respirable dust. The null hypothesis to be tested was that no potentially harmful respirable dust is released upon grinding. The potential of dental composites to release respirable dust upon grinding was investigated by measurements in both an in vitro and a clinical setting, and the composite dust was characterized by electron microscopy.

2. Materials and methods

Seven commercial composites (1 hybrid, 1 micro-hybrid, one nano-composite and 4 nano-hybrid composites) were included in this study. Their compositions and classifications (including definitions of the classifications) are given in Table 1.

For each composite, five standardized composite blocks with a size of $15\ \text{mm} \times 13\ \text{mm} \times 3\ \text{mm}$ were prepared in a silicon mold according to a clinically relevant procedure. Each block weighed approximately 1 g, which corresponded to the size of a molar-crown [13]. The composite was covered with a glass plate and light-cured on each side for 40 s with a light-curing unit (L.E. Demetron, Kerr, Orange, CA, USA) with an output above $1000\ \text{mW}/\text{cm}^2$.

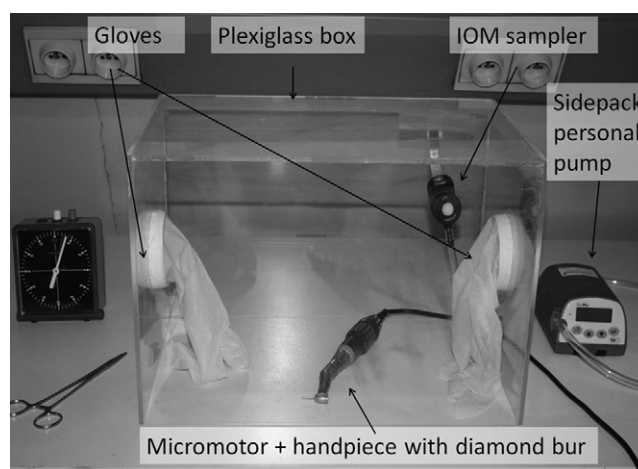


Fig. 1 – In vitro test set-up for the gravimetric analysis of supra-micron (> $1\ \mu\text{m}$) respirable dust. Standardized composite blocks were ground in a custom-made plexiglass box with two openings at the sides sealed with disposable gloves, enabling manipulation of the specimens and the bur. The IOM inhalable dust sampler was hanging in the box.

2.1. Gravimetric analysis of supra-micron (> $1\ \mu\text{m}$) respirable dust

Entire blocks of composite were ground in vitro using a dental bur, and the composite dust was collected using an IOM personal inhalable aerosol sampler (225-70A, SKC, Eighty Four, PA, USA) and quantified gravimetrically. The IOM sampler was connected to a personal sampling pump (SP 350 side-pack personal sampling pump, TSI, Shoreview, MN, USA). The IOM sampler contained a cassette in which two filters were fixed: (1) a polyurethane foam disc (Multidust foam disc, 225-772 SKC) and (2) a glass-fiber filter with a pore size of $1\ \mu\text{m}$ (225-702 SKC). While the large inhalable size particles ($5-10\ \mu\text{m}$) are deposited on the foam, the smaller respirable (< $5\ \mu\text{m}$) particles pass the foam and are deposited on the glass fiber filter. The filters were acclimatized overnight. Before the experiment, the glass-fiber filters fixed in the cassette were carefully weighed with a microbalance (ME, Sartorius, Göttingen, Germany). The air flow of the pump ($41/\text{min}$) was calibrated with the Gilibrator-2 (Gilian, Sensidyne, Schauenburg International GmbH, Mülheim, Germany) [14].

The experiment was carried out in a custom-made well-sealed plexiglass box ($27\ \text{mm} \times 27\ \text{mm} \times 42\ \text{mm}$) with two openings at the sides sealed with disposable gloves, enabling manipulation of the specimens and the bur (Fig. 1). The composite block was held with a forceps during grinding with a rough diamond bur (842314014 Komet, Lemgo, Germany, grain size $100\ \mu\text{m}$) in a Kavo Intracompact handpiece (200,000 rpm) connected to an electric micromotor (EWL K9, Kavo, Biberach, Germany) and the entire block was ground ensuring that exactly the same amount of composite was ground for each block. The pump was started right before the composite was ground, and left on for 10 min. For each composite block, a new bur was used. After grinding each block of composite, the foam discs were carefully removed and the cassette with the

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