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# ZnS nanoparticles electrodeposited onto ITO electrode as a platform for fabrication of enzyme-based biosensors of glucose

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#### ABSTRACT

The electrochemical and photoelectrochemical biosensors based on glucose oxidase (GOD) and ZnS nanoparticles modified indium tin oxide (ITO) electrode were investigated. The ZnS nanoparticles were electrodeposited directly on the surface of ITO electrode. The enzyme was immobilized on ZnS/ITO electrode surface by sol–gel method to fabricate glucose biosensor. GOD could electrocatalyze the reduction of dissolved oxygen, which resulted in a great increase of the reduction peak current. The reduction peak current decreased linearly with the addition of glucose, which could be used for glucose detection. Moreover, ZnS nanoparticles deposited on ITO electrode surface showed good photocurrent response under illumination. A photoelectrochemical biosensor for the detection of glucose was also developed by monitoring the decreases in the cathodic peak photocurrent. The results indicated that ZnS nanoparticles deposited on ITO substrate were a good candidate material for the immobilization of enzyme in glucose biosensor construction.

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#### 1. Introduction

In recent decades, Quantum dots (QDs) have attracted worldwide attention and have been extensively studied due to their unique physical and chemical properties [1–3]. For examples, QDs have high photoluminescence quantum efficiency, size-tunable fluorescence emission wavelength and long luminescence lifetimes, which are gradually replacing the conventional organic dyes in various biomedical applications [4–6]. In the luminescent probes and labeling, CdE (E=S, Se, Te) have developed fast and have been commonly used. However, CdE are poisonous and likely to pollute the environment. The inhalation of CdE dust can substantially affect the bone (bone weakness) and kidneys (impairment), and the CdE is carcinogenic to humans [7,8].

ZnS, another semiconductor, is nontoxic to human body, and is very cheap and abundant [7–10]. It is the most suitable candidate to fabricate CdE–ZnS core–shell structures, which could reduce the toxic problems of CdE, and at the same time could maintain CdE's excellent fluorescence properties [11–13]. On the other hand, the ZnS band gap energy is about 3.7 eV, which enables it to be transparent to almost all wavelength of the solar spectrum [14,15]. It appears to be a very promising material for photocatalysis because of the repaid generation of electron–hole pairs by photoexcitation and highly negative reduction potentials of excited electrons [16–19].

Recently, QDs have also been used to immobilize protein for the fabrication of electrochemical biosensors [20,21] and photoelectrochemical biosensors [22,23]. A few papers have reported that the direct electron

transfer between enzyme and electrode could be realized using CdE nanoparticles and CdE–ZnS core–shell nanostructures[21,24,25]. It was also reported that ZnS nanoparticles can be used to fabricate a reagentless uric acid biosensor [26]. Moreover, Impellizzeri et al. indicated that ZnS shell seems to dominate the electrochemical properties of CdE–ZnS core–shell nanoparticles, while having a modest effect on their optical properties [13]. Therefore, in QDs, ZnS nanoparticles seem to be more favorable in the application of enzyme based biosensors because of simple preparation, low cost and less toxicity.

In order to fabricate electrochemical biosensors, ZnS nanoparticles must be supported on the solid electrode surface. The use of suitable linker molecules, such as 1-ethyl-3-(3-dimethylaminopropryl) carbodiimide. would be a representative method. The ZnS-modified electrode then immobilized protein to formulate enzyme electrode. However, this method with linker molecules suffers some complexity and disadvantages. It is because they need three steps: i) preparation of ZnS nanoparticles with organic stabilizers, such as Cetyltrimethylammonium (CTA) [27], trioctylphosphine oxide (TOPO) [11,21], sodium bis(2-ethylhexy) sulfosuccinate [28], mercaptoacetic acid [29] and other surfactants [30–32], which may result in relative poor stability and bioactivity of enzyme; ii) surface modification with linker molecules, which may influence its electrocatalytic properties; iii) combination of ZnS nanoparticles with linker molecules. The organic reagents may be toxic and result in a poor contact between the nanoparticles and electrode. Therefore, it is still a challenge to seek simpler method for fabrication of electrochemical biosensor based on ZnS nanoparticles.

The electrodeposition of nanomaterials on the electrode surface is a simple method as well as high surface areas which are solidly attached to the solid substrate. In this paper, ZnS nanoparticles are directly

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electrodeposited on the surface of indium tin oxide (ITO) electrode without using any link molecules and organic solvents. The sol–gel (SG) technology was employed to immobilize the glucose oxidase (GOD) on the ZnS film. The direct electron transfer of GOD is realized at the GOD-SG/ZnS/ITO electrode. The obtained biosensor can catalyze the reduction of oxygen and determine the concentration of glucose. The photocatalytic property of ZnS nanoparticles is also investigated and the glucose sensing sensitivity of the biosensor under illumination is higher than that without illumination.

#### 2. Experimental

#### 2.1. Materials

Zinc chloride (ZnCl<sub>2</sub>) was obtained from Sinopharm Chemical Reagent Co., Ltd. Sodium thiosulphate (Na<sub>2</sub>S<sub>2</sub>O<sub>3</sub>) and glucose were purchased from Shanghai Chemical Reagent Company (Shanghai, China). Glucose oxidase (from Aspergillus niger, 155,000 Ug $^{-1}$ ) was purchased from Sigma Chemical Company. A 1000 U mL $^{-1}$  GOD stock solution was stored at 4 °C. PVA stock solution of 0.25 was prepared by dissolving polyvinyl alcohol (PVA-124, average degree of polymerization was 2400–2500, Shanghai Chemical Reagent Plant imported from Japan). Na<sub>2</sub>HPO<sub>4</sub> and NaH<sub>2</sub>PO<sub>4</sub> were employed to prepare the 0.02 M phosphate buffer solutions (pH 7.0). Indium tin oxide glass (1.1 mm thickness, less than 100  $\Omega$ ) was purchased from Suzhou NSG Electronics Co., Ltd. (Suzhou, China). All chemicals were analytical grade and were used as received without further purification. All solutions were made up with twice-distilled deionized water through the study.

#### 2.2. Apparatus

Cyclic voltammetric experiments were performed with a CHI830B electrochemical workstation (Shanghai Chenhua Apparatus Inc., China). A traditional three-electrode configuration was used, with an ITO modified electrode, a platinum wire counter electrode and a saturated calomel reference electrode (SCE) served as working electrode, auxiliary electrode and reference electrode, respectively. All potentials were reported with respect to SCE electrode. The photoelectrochemical measures were performed with a Xenon lamp (350 W) as irradiation source. All the measurements were carried out at a room temperature with the electrolyte which was deoxygenated by purged with nitrogen for at least 10 min prior to experiments, and a nitrogen atmosphere was maintained over the solution during the performance. Scanning electron microscopy (SEM) was run with an S-4700 scanning electron microanalyzer (Hitachi, Japan).

#### 2.3. Fabrication of ZnS/ITO electrode

ZnS/ITO modified electrode was prepared using electrochemical deposition [8,33]. Briefly, a sheet of ITO (0.6  $\times$  3.0 cm) was ultrasonicated with dilute ammonia, absolute ethanol and deionized water for approximately 5 min, respectively. Then, the ITO electrode was immersed in the mixed solution containing 4.0 mL of 2 mM Na $_2$ S $_2$ O $_3$  solution, 4.0 mL of 0.1 M ZnCl $_2$  in a total 10 mL (if necessary add some HCl to adjust pH between 2 to 3) at 50 °C. The electrolysis was carried out in the potential range from -0.4 to -1.0 V at 50 mV/s for 40 cycles in cyclic voltammetry. After deposition, the electrode was removed from the solution and washed with water.

#### 2.4. Synthesis of GOD-SG/ZnS/ITO electrode

The preparation of silica colloidal sol was done according to the previous report [34]. Briefly, Na<sub>2</sub>SiO<sub>3</sub>·9H<sub>2</sub>O was stored at 110 °C for 12 h. After cooling down, the resulting solution was adjusted with 3 M HCl to specific gravity of 1.38. Then, the silica sol was fabricated by ion-exchange method from the diluted (addition of same volume

water) solution. Dip the ZnS/ITO electrode in the following solution: 0.3 mL of 1000 U/mL GOD, 0.3 mL of silica sol solution, 0.1 mL of 0.25 PVA in each milliliter. Then dry the electrode under nitrogen atmosphere. The enzyme electrode (defined as GOD-SG/ZnS/ITO) was stored at 4 °C in a refrigerator when not in use. For comparison, the SG/ZnS/ITO was prepared by the same method but without addition of GOD and GOD-SG/ITO was fabricated by the same method on ITO electrode. The GOD/ZnS/ITO electrode was fabricated by immersing the ZnS/ITO electrode in GOD solution for 2 h.

#### 3. Results and discussion

#### 3.1. Characteristics of ZnS/ITO modified electrode

ZnS nanoparticles were deposited directly on ITO surface by electrochemical method. Although the exact mechanism of the consecutive electrochemical or electrochemical-chemical steps is still not clear, the cathodic deposition of MS from electrolyte of M<sup>2+</sup> and  $S_2O_3^{2-}$ ions was not a doubt [35]. The ZnS/ITO modified electrode was almost colorless. It turned brownish back after addition of a drop of Pb(NO<sub>3</sub>)<sub>2</sub> solution. This indicates that S element was existent. The composition of Zn was demonstrated by ICP-AES after the nanoparticles were dissolved in acid. The XRD patterns were recorded for the deposited products before and after treated at 500 °C in Fig. 1A. No pronounced ZnS or Zn peak was observed in the product before and after treated at 500 °C in N2 environment. After treated at 500 °C in air atmosphere, several new small peaks located at 35.8°, 56.1°, and 62.3° were observed, which is attributed to ZnO crystalline of (101), (110), and (103) planes[36]. These results indicate that the crystallinity of ZnS electrodeposited on ITO substrate was very low.

The SEM is also employed to evaluate the physical appearance and surface features of the nanomaterials. The image of bare ITO surface was rather smooth (Fig. 1B). It is observed that ZnS nanoparticles were grown successfully on the ITO surface with quasi-spherical (Fig. 1C). The average diameter of these nanoparticles was around 20 nm. The coverage of the nanoparticles on substrate surface could be controlled by adjusting the potential and electrodeposition cycles. From the scrape in the film, it can clearly be seen that the silica solgel film was formed onto the ZnS/ITO surface (Fig. 1D).

#### 3.2. Electrochemical behavior of the GOD-SG/ZnS/ITO electrode

The GOD was immobilized on ZnS/ITO surface by sol–gel technique. Therefore, enzyme was embedded in the silica sol-gel network. Fig. 2 shows the typical cyclic voltammograms at the different modified electrodes in 0.02 M phosphate buffer solution (pH 7.0). There were no obvious redox peaks at the bare ITO and SG/ZnS/ITO electrodes. A very little peak was observed at GOD-SG/ITO electrode. However, a pair of stable and well-defined redox peaks was obtained at the GOD-SG/ ZnS/ITO electrode, which was also much higher than that obtained at the GOD/ZnS/ITO electrode. It suggests that ZnS nanoparticles promote the electron transfer between the enzyme embedded in silica sol-gel network and electrode without the help of mediators. The formal potential  $(E^0)$  was -0.45 V with a small peak potential separation ( $\Delta Ep$ ) of 30 mV. This value was smaller than that of 94 mV at GOD/Au modified electrode [37], 78 mV at GOD/carbon ionic liquid electrode (CILE) modified electrode [38], 56 mV at GOD/NdPO<sub>4</sub> NPs/Chitosan modified electrode [39] and 35 mV at GOD/SnO2-Au/modified electrode [40]. This demonstrates that ZnS nanoparticles are favorable in the preparation of enzyme-based electrochemical biosensors.

Fig. 3 shows the CVs of the GOD-SG/ZnS/ITO electrode at different scan rates in 0.02 M phosphate buffer solution (pH 7.0). The peak-to-peak separation increased gradually with the increase of scan rate. The oxidation peak shifted to more positive potentials and the reduction peak shifted to more negative potentials. Both the anodic and

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