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## Materials Letters

journal homepage: www.elsevier.com/locate/matlet



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#### ARTICLE INFO

Article history: Received 25 November 2014 Accepted 14 February 2015 Available online 21 February 2015

Keywords: Polyphosphate Regenerative medicine SaOS-2 cells Morphogenetic activity Tissue engineering

#### ABSTRACT

Polyphosphate [polyP] has been proven to elicit morphogenetic activity on bone cells. By applying mild reaction conditions, a Ca-polyP material that displays a hardness of  $\approx$  1.3 GPa has been fabricated. The Ca-polyP granules are prone to hydrolytic degradation during in vitro incubation of the cells, suggesting that this property is associated with the observed bioactivity.

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#### 1. Introduction

The need for suitable biofabricated bone graft materials, due to the shortage and risks of autogeneic and allogeneic implants, drives the development of new biosynthetic bone substitutes [1]. Besides of cell-based bone graft substitutes, ceramic-based materials have been proven to be useful bone scaffolds for implants. Among the calcium phosphate-based ceramics, hydroxyapatite (HA),  $\beta$ -tricalcium phosphate ( $\beta$ -TCP) and bioactive glass gained upmost relevance [2–4].

Since all of those mineralic implant materials are fabricated at temperatures higher than 800 °C and in turn are not, or only at a limited degree, osteoinductive like the bioglass, we tried to develop a new potential biomaterial perhaps likewise suitable to be used as bone implant. This new material is based on polyphosphate [polyP]. Previously, polyP has been used, after calcination, as a potential scaffold for bone implants [5]. The polymer was integrated into different inorganic matrices which had been sintered at 550–1000 °C, a process during which the amorphous material was transformed into a crystalline one [6]. Those sintered polyP samples displayed a highly edged morphology; the cubes were of large sizes with  $> 100 \,\mu$ m [7,8]. The material displayed both biocompatibility and degradability [9] but elicit no osteoinductive activity. PolyP is a natural polymer that has been found in bone-forming cells [10] as well as in platelets [11]. We described

http://dx.doi.org/10.1016/j.matlet.2015.02.070 0167-577X/© 2015 Elsevier B.V. All rights reserved. that polyP has an inductive effect on osteoblasts [12], mainly as an anabolic polymer that stimulates differentiation of bone cells and mineralization [13,14] (reviewed in: [15,16]). Interesting, polyP induces the enzyme alkaline phosphatase [ALP] [13], an enzyme that degrades polyP [17]. In the present study we describe an amorphous, polyP-based biomaterial that is fabricated at ambient temperature.

#### 2. Experimental section

Preparation of calcium polyphosphate nanospheres: Na-polyphosphate (Na-polyP of an average chain of 40 phosphate units) was obtained from Chemische Fabrik Budenheim (Budenheim; Germany). Na-polyP (10 g) was dissolved in 500 ml of distilled water and the pH was adjusted to 10 with a 1 M NaOH aqueous solution. A solution of 14 g of calcium chloride dihydrate (C3306 Sigma) or of 28 g of CaCl<sub>2</sub> in 250 ml was added dropwise (1 ml/min) to the Na-polyP solution, adjusting steadily the pH to 10 at room temperature. The suspension formed was stirred for 4 h. The particles formed were collected by washing twice with ethanol. Then the particles were dried at 60 °C. The Ca-polyP material obtained by addition of 14 and 28 g of CaCl<sub>2</sub> were named as "Ca-polyP1" and "Ca-polyP2", respectively

The Ca-polyP material obtained by addition of 14 g of CaCl<sub>2</sub> was named "Ca-polyP1", and the one with 28 g of CaCl<sub>2</sub> was termed "Ca-polyP2".

*Chemical characterization by FTIR:* Fourier transformed infrared (FTIR) spectroscopy was measured by using a Varian 660-IR





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spectrometer with Golden Gate ATR auxiliary (Agilent, Darmstadt; Germany).

*Scanning electron microscopy:* For the scanning electron microscopic (SEM) analyses a HITACHI SU 8000 electron microscope (Hitachi High-Technologies Europe GmbH, Krefeld, Germany) was employed.

*XRD analysis:* X-ray diffraction (XRD) of the dried powder samples was conducted on a Philips PW 1820 diffractometer with monochromatic Cu-K<sub> $\alpha$ </sub> radiation ( $\lambda$ =1.5418 Å, 40 kV, 30 mA, 5 s,  $\Delta\theta$ =0.02) [18].

Cells and cell culture conditions: Human osteogenic sarcoma cells. SaOS-2 cells. were used for the experiments and cultivated in McCov's medium with fetal calf serum [FCS] [19]. Cultivation of the cells was performed in 24-well plates;  $3 \times 10^4$  cells were seeded per well. After an initial incubation period of 3 d, the cultures were supplemented with a solution of 10 µg/mL of Na-polyP, supplemented with CaCl<sub>2</sub> in a 2:1 stoichiometric ratio, in order to compensate for the chelating activity of polyP as described [13], or with a suspension of  $10 \mu g/mL$  of the two polyP samples, prepared here, with Ca-polyP1, Ca-polyP2, nano-hydroxyapatite (HA; 677418 Sigma-Aldrich) or β-TCP (13204 Sigma-Aldrich); in the controls none of those materials were added. Then the cells were continued to be incubated in the presence of the osteogenic cocktail [OC]. After a 7 d incubation period the cells were either stained with Alizarin Red S to assess the extent of mineralization [20] or subjected to qRT-PCR [quantitative real-time RT-PCR] analysis [19].

*Determination of the hardness:* The hardness of the polyphosphate material Ca-polyP2 was determined by a ferruled optical fiber-based nanoindenter [21].

*Polyp degradation in vitro:* SaOS-2 cells were incubated with  $50 \mu g/mL$  of solid Ca-polyP2 and incubated in the standard assay

for 1 or 7 d. In parallel assays 50  $\mu$ g/mL of solid Ca-polyP2 had been incubated for 1 or 7 d in PBS [phosphate buffered saline] in a final volume of 1.5 ml. Then samples (50  $\mu$ l) were taken and assayed for the chain length of polyP [17].

Statistical analysis: The results were statistically evaluated using the paired Student's *t*-test [22].

### 3. Results and discussion

*FTIR analyses:* The two phosphate materials, Ca-polyP1 and Ca-polyP2, were characterized by FTIR and compared with the spectrum obtained for Na-polyP (Fig. 1). The complete spectra between the wavenumbers 4000 and 600 cm<sup>-1</sup> are shown in Fig. 1A, while segments between 1400 and 600 cm<sup>-1</sup> are given in Fig. 1B. However, the spectra of Ca-polyP showed the same characteristic features as those of the described polyP samples [23]. However, the peaks are shifted in the Ca-polyP1 and Ca-polyP2 samples if compared the Na-polyP spectrum. This shifting is also seen for other bands in the Ca-polyP spectra; they even increase by increasing the Ca<sup>2+</sup> content in the polyP.

The XRD patterns for Na-polyP, Ca-PolyP1 and Ca-Polyp2, shown in Fig. 1C, indicate a clear amorphous phase, with a broad peak from 20° to 40° for Na-polyP and centered around 30° for Ca-polyP.

Morphology of polyP samples: The three samples, Na-polyP, Ca-polyP1 and Ca-polyP2, were analyzed by SEM (Fig. 2). The Na-polyP particles, of a non-regular shapes, often show a tapered morphology (Fig. 2A and B). The sizes of the particles vary between 1 and 300  $\mu$ m with an average size of  $\approx$  100  $\mu$ m. Likewise non-regular shapes show the Ca-polyP1 particles (Fig. 2C and D). They are smaller than the Na-polyP particles with an average



Fig. 1. FTIR spectra and XRD pattern of Na-polyP, Ca-polyP1 and Ca-polyP2; (A) wavenumbers 4000–600 cm<sup>-1</sup> and (B) wavenumbers 1400–600 cm<sup>-1</sup>. (C) XRD analysis.

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