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## Hydrogel nanocomposites as remote-controlled biomaterials

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#### Abstract

Nanocomposite hydrogels are a new class of intelligent materials which have recently attracted interest as biomaterials. In this study, magnetic nanocomposites of temperature-sensitive hydrogels have been developed and demonstrated to be responsive to alternating magnetic fields. Nanocomposites were synthesized by incorporation of superparamagnetic  $Fe_3O_4$  particles in negative temperature-sensitive poly(*N*-isopropylacrylamide) hydrogels. The systems were characterized for temperature-responsive swelling, remote heating on application of an alternating magnetic field and remote-controlled drug delivery applications. The rise in temperature in external alternating magnetic field depends on the  $Fe_3O_4$  particle loading of the system. Preliminary studies on remote-controlled drug release showed reduced release in the presence of an alternating magnetic field.

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#### 1. Introduction

Hydrogels are cross-linked hydrophilic polymers that can absorb water or biological fluids and swell several times of their dry volume. Due to the high level of water in their composition and their elastic structure, hydrogels are considered as excellent biocompatible materials [1]. There are numerous applications of hydrogels in the medical and pharmaceutical sectors, such as contact lenses, membranes for biosensors, sutures, drug delivery devices, and matrices for the repair and regeneration of tissues and organs [2–4].

Hydrogels can show swelling behavior depending on changes in the external environment. Some of the factors that can affect the swelling of responsive hydrogels include pH, ionic strength and temperature [5]. Hydrogels can also be made to respond to diverse external stimuli, such as light, electric current, ultrasound, and the presence of a magnetic field or a particular molecule. The unique property of responsiveness has resulted in their applications in sensors [6,7], self-regulated and externally actuated intelligent drug delivery systems [8–11] and microfluidic devices [12,13].

Hydrogel nanocomposites have recently attracted considerable attention due to their accelerated response and capability of action at a distance. The properties of the nanocomposites can be easily tailored by manipulating the properties of the hydrogel and the composite material. Hydrogel nanocomposites with magnetic particles have been demonstrated as potential candidates for pulsatile drug delivery and soft actuator applications. Zrinyi and co-workers reported that magnetic composites of poly (vinyl alcohol) undergo quick, controllable changes in response to an applied magnetic field and thus can be used in soft actuator-type applications [14,15]. Further studies on magnetic composites of N-isopropylacrylamide (NIP-AAm) have shown that magnetic particles do not affect the temperature sensitivity of the hydrogel network, including the lower critical transition temperature (LCST) [16].

One of the first approaches to achieve an externally controlled drug delivery system using biomaterials was by Langer and co-workers [17–20]. They embedded macroscale magnetic beads ( $\sim$ 1 mm diameter) in ethylene vinyl acetate along with various macromolecular drugs like insulin. Both in vivo and in vitro studies have shown that application of

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an oscillating magnetic field leads to increased release rates. The release rates could be modulated by altering the geometry of the implant – the position, orientation and magnetic strength of the embedded materials – as well as changing the amplitude and frequency of the magnetic field. Recently, Liu et al. demonstrated gelatin and poly(vinyl alcohol) hydrogels with Fe<sub>3</sub>O<sub>4</sub> nanoparticles as "on" and "off" drug delivery devices [21,22]. When a direct current magnetic field was applied there was reduced release, and when the field was switched off the drug was released rapidly. The release rate depends on the strength of the magnetic field, the particle size and the duration of the switching time.

For our current studies with magnetic nanocomposites, NIPAAm was used due to its temperature responsiveness, while superparamagnetic iron oxide (Fe<sub>3</sub>O<sub>4</sub>) nanoparticles (20-30 nm diameter) were used as they have been widely considered for remote heating in the case of hyperthermia [23–25]. The application of an alternating high-frequency magnetic field to the nanocomposite should lead to heat generation, which could drive the swelling transition of the hydrogel. This is the first demonstration utilizing an alternating magnetic field for the remote control of drug release from nanocomposite hydrogels, and we expect these systems to find application in implantable biomedical devices. Although this paper only demonstrates remote control for short release durations, the release profiles can be easily modulated by altering the nanocomposite hydrogel composition (e.g. physical size, cross-linking percentage, molecular weight between cross-links, etc.). Currently, additional studies are under way to look into systems that can demonstrate control over extended periods of time. In addition, on/off control of the release is possible, and is being studied. Fig. 1 includes a schematic of the nanocomposite systems for remote-controlled drug delivery in the case of negative and positive temperaturesensitive systems.

The synthesis and swelling behavior of NIPAAm-based magnetic nanocomposites has been described earlier with special emphasis on the effect of the type of cross-linker [26]. In this work, we report the characterization of the magnetic nanocomposites, which includes the effect of the degree of cross-linking on swelling behavior, the remote heating response on the application of an alternating magnetic field and the preliminary results of remote-controlled (RC) drug delivery.

### 2. Materials and methods

#### 2.1. Hydrogel synthesis

Hydrogel nanocomposites were synthesized by ultraviolet (UV) photopolymerization with various cross-linking densities and magnetic nanoparticle loadings. The hydrogel systems were based on *N*-isopropylacrylamide (Sigma– Aldrich) as the monomer with poly(ethylene glycol) 400 dimethacrylate (Polysciences, Inc) as the cross-linker. 2,2-Dimethoxy-2-phenylacetophenone (Sigma–Aldrich) was

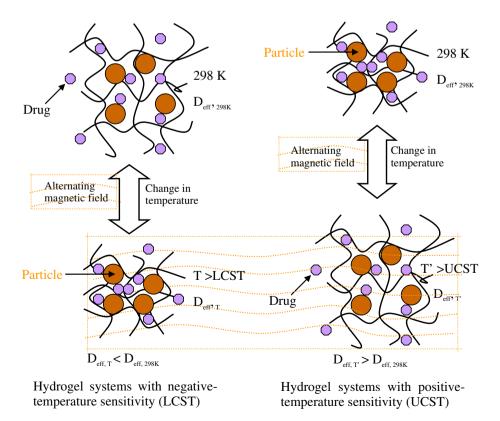


Fig. 1. Schematic of the proposed remote-controlled drug delivery system for negative and positive temperature-sensitive systems.

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