



Bridging the gap between chemistry, physiology, and evolution: Quantifying the functionality of sperm whale myoglobin mutants

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ABSTRACT

This work merges a large set of previously reported thermochemical data for myoglobin (Mb) mutants with a physiological model of O₂-transport and -storage. The model allows a quantification of the functional proficiency of myoglobin (Mb) mutants under various physiological conditions, i.e. O₂-consumption rate resembling workload, O₂ partial pressure resembling hypoxic stress, muscle cell size, and Mb concentration, resembling different organism-specific and compensatory variables. We find that O₂-storage and -transport are distinct functions that rank mutants and wild type differently depending on O₂ partial pressure. Specifically, the wild type is near-optimal for storage at all conditions, but for transport only at severely hypoxic conditions. At normoxic conditions, low-affinity mutants are in fact better O₂-transporters because they still have empty sites for O₂, giving rise to a larger [MbO₂] gradient (more varying saturation curve). The distributions of functionality reveal that many mutants are near-neutral with respect to function, whereas only a few are strongly affected, and the variation in functionality increases dramatically at lower O₂ pressure. These results together show that conserved residues in wild type (WT) Mb were fixated under a selection pressure of low P_{O₂}.

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1. Introduction

Due to its central position in protein science, myoglobin (Mb) is often called the 'hydrogen atom of biology' (Frauenfelder et al., 2003). As the first protein whose three-dimensional structure was revealed at atomic resolution (Kendrew et al., 1958), it has been the subject of extensive experimental and theoretical research. Mb is a monomeric protein of approximately 16 kDa which is generally abundant in muscles (both cardiac and skeletal) of vertebrates and in the body wall of invertebrates (Suzuki and Imai, 1998). Mb increases the availability of oxygen in muscle cells by taking up the oxygen released by hemoglobin in blood, thereby providing O₂ during muscle contraction, when blood flow through capillaries is restricted. A cornerstone of muscle metabolism is thus the ability of Mb to enhance the supply of O₂ to the mitochondria (Wittenberg, 1970).

Direct storage of O₂ has been considered the main function of Mb, based on the observation of elevated concentrations of Mb in diving mammals (Guyton et al., 1995; Ponganis et al., 2002) and increased expression of Mb at higher altitudes (Gimenez et al., 1977; Terrados et al., 1990). In contrast, it has been a matter of controversy whether Mb can contribute significantly to active O₂ transport within the cell: Despite the smaller diffusion coefficient of Mb compared to free O₂, the high concentration of Mb in working heart and muscle cells, more than thirty-

fold than that of free O₂, confers an advantage in transporting O₂ from the sarcolemma to the mitochondria (Wittenberg and Wittenberg, 2003). *In vitro* studies have indeed confirmed that O₂ diffuses faster in Mb solution than in Mb-free solution (Wittenberg and Wittenberg, 1989), and Mb exhibits sufficient mobility and O₂-carrying ability to compete effectively with free O₂. *In vivo*, however, the role of Mb in O₂ diffusion has remained obscure for decades (Gros et al., 2010).

From a theoretical perspective, models have elaborated on the classical work by Krogh (1919) to clarify the problem (Groebe, 1995). Since these models were based on variable quantities such as concentrations and diffusion coefficients in muscle tissues, acceptance of Mb-facilitated diffusion has languished in absence of definitive experimental confirmation (Lin et al., 2007a).

Recently, pulsed-field gradient NMR and Fluorescence Recovery After Photobleaching (FRAP) methods enabled precise measurement of the endogenous diffusion coefficient of Mb in myocardial and skeletal muscle cells (Papadopoulos et al., 2001; Lin et al., 2007a,b). Following these results, it was then argued that Mb probably has no significant contribution to O₂ transport under normoxic conditions, while its importance increases as the oxygen pressure declines and the cell experiences hypoxia.

Mb binds O₂ with a 1:1 stoichiometry at its heme group. This side of the heme is referred to as distal, the other as proximal. More than 40 years ago, it was proposed that O₂-binding involves the side-chain of the distal histidine 64 at the E7 helical position (Perutz and Mathews, 1966). Beside this 'histidine-gate' hypothesis, it was also shown that ligands may escape through the interior of the protein

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where hydrophobic Xe-binding cavities are observed (Tilton et al., 1984). Ligand binding to Mb then follows a multi-state scheme where internal states and distal cavities play a major role (Fig. 1-a) (Ostermann et al., 2000). Here, B states represent a number of ligand positions in the distal ‘pocket’ with differing rates of binding to the heme group. In the C state, the ligand is relocating between multiple states such as Xe1 and Xe2 cavities within the protein matrix (Scott et al., 2001). The current view is that the majority of ligands (~70–80%) enter and exit from the distal histidine gate (Scott et al., 2001; Elber, 2010) and thus, the kinetics is adequately interpreted in terms of an effective two-step scheme (Fig. 1-b).

Much insight into the pathways and kinetics of ligand binding to Mb has been obtained from studies of its site-directed mutants (Varadarajan et al., 1985; Springer and Sligar, 1987). By measuring the O₂ binding parameters of 90 sperm whale Mb mutants at 27 different positions, a mapping of the pathways for O₂ entry and exit was achieved (Scott et al., 2001). These investigations show that His E7 stabilizes bound O₂ about 1000-fold, most likely because of the formation of a strong hydrogen bond between O and N_εH of the imidazole group (Olson, 2008).

In general, the molecular evolution of the globin superfamily can be traced back ~4000 Myr to a common ancestor, which was among the basic protein components required for life (Suzuki and Imai, 1998; Wajcman et al., 2009). Mammalian Mb is thought to have diverged from another common ancestor about 600 Myr ago at the beginning of Cambrian period, and sequence alignments reveal a highly conserved distal pocket within all of these (Romero-Herrera et al., 1973).

The molecular evolution of the heme group can be partly rationalized through the positive selection of the porphyrin structure to satisfy the reversible spin-crossover upon O₂ binding to porphyrin, which is a necessary first condition for reversible binding of molecular O₂ to Mb (Jensen and Ryde, 2004). In this work, we investigate how the physiological function is further refined by the properties of the surrounding protein, i.e. the sequence-dependent thermochemistry of O₂-binding, by putting these data into a physiological framework and changing the physiological variables of O₂ partial pressure (P_{O₂}), cell size, Mb concentration, and metabolic rate.

To this end, we quantify transport and storage proficiency as functions of physiological variables in the same way that “reversible binding” and “near-degeneracy” of spin states were used to quantify the functional proficiency of porphyrin and iron, specifically (Jensen and Ryde, 2003, 2004). We then investigate why and how selection pressure conserves the wild-type Mb. It is found that the relative importance of storage and transport varies from one mutant to another and is greatly affected by physiological and environmental conditions, and that the WT appears to have been selected under hypoxic conditions where other mutants are much less proficient.

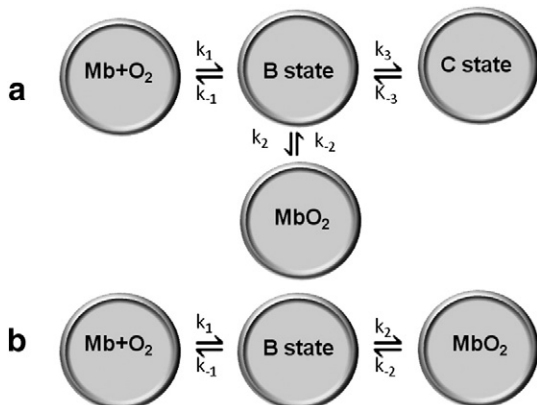


Fig. 1. Kinetics of O₂ binding to Mb. a) The C state accounts for internal cavities while in b) mainly the B state is involved under physiological conditions.

2. Theoretical background

2.1. Saturation expression

The saturation of Mb by O₂ (S), can be expressed in terms of the Hill equation (Hill, 1936):

$$S = \frac{(P_{O_2})^n}{(P_{50})^n + (P_{O_2})^n} \quad (1)$$

where P_{O₂} is the oxygen partial pressure, n is the oxygen binding cooperativity index, and P₅₀ is the value of P_{O₂} at which S = 0.5. For Mb with only one subunit, n = 1 and saturation can be described using the bimolecular oxygenation equilibrium:



$$S = \frac{[\text{MbO}_2]}{C_{\text{Mb}}} = \frac{K_{O_2}[\text{O}_2]}{K_{O_2}[\text{O}_2] + 1} \quad (3)$$

Here, saturation is defined as $S = \frac{[\text{MbO}_2]}{C_{\text{Mb}}}$, $K_{O_2} = \frac{[\text{MbO}_2]}{[\text{O}_2][\text{Mb}]}$ is the bimolecular oxygenation equilibrium constant, and C_{Mb} is the total concentration of Mb in the cell, which is equal to the sum of [Mb] and [MbO₂]. Eq. (3) can be converted to (1) using $P_{50} = \frac{1}{K_{O_2} \alpha_{O_2}}$ and $[\text{O}_2] = \alpha_{O_2} P_{O_2}$, where α_{O₂} is the oxygen solubility constant in the sarcoplasm. In the general case of two-step binding (Fig. 1-b), using the equilibrium constants K₁ and K₂, S takes the form:

$$S = \frac{K_1 K_2 [\text{O}_2]}{K_1 K_2 [\text{O}_2] + K_1 [\text{O}_2] + 1} = \frac{K_{O_2} \alpha_{O_2} P_{O_2}}{\alpha_{O_2} P_{O_2} (K_{O_2} + K_1) + 1} \quad (4)$$

The second equality in Eq. (4) holds by using $K_{O_2} = K_1 K_2$ and $[\text{O}_2] = \alpha_{O_2} P_{O_2}$, and the half saturation pressure can be calculated as $P_{50} = \frac{1}{\alpha_{O_2} (K_{O_2} + K_1)}$. For all mutants studied here $K_{O_2} \gg K_1$ and Eq. (4) reduces to Eq. (3), but this may not always be the case.

2.2. Muscle tissue and oxygen delivery

To model oxygen delivery within the muscle cell, we applied the Krogh cylinder model in a revised, state-of-the-art form (Groebe, 1995). As shown in Fig. 2, the model consists of three concentric cylinders representing capillaries (inner region), space between red blood cells and sarcolemma, or cell free regions (middle), and the muscle tissue as the outer region. We consider only radial oxygen diffusion and assume chemical equilibrium at all times, since both the radial and longitudinal diffusion coefficients of Mb are similar within our scope (Groebe, 1995; Lin et al., 2007b). The radial distance (r) is used as a generalized coordinate. With this theoretical framework, P_{O₂} is derived as:

$$P_{O_2}(r) = \frac{1}{2} \left(P^*(r) - \frac{D_{\text{Mb}} C_{\text{Mb}}}{D_{O_2} \alpha_{O_2}} - P_{50} \right) + \frac{1}{2} \sqrt{\left(P^*(r) - \frac{D_{\text{Mb}} C_{\text{Mb}}}{D_{O_2} \alpha_{O_2}} - P_{50} \right)^2 + 4P^*(r)P_{50}} \quad (5)$$

where D_{O₂} (m² s⁻¹) and D_{Mb} (m² s⁻¹) are the free oxygen and Mb diffusion coefficients in the cell, C_{Mb} (mol L⁻¹) and α_{O₂} (mol L⁻¹ mmHg⁻¹) are the total concentration of Mb and the oxygen solubility in muscle tissue.

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