

SHORT COMMUNICATION

## A new teaching model of the systemic circulation that incorporates reservoir characteristics



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**KEYWORDS** 

Wave intensity analysis; Hydraulic model; Systemic circulation; Arterial-ventricular coupling; Elastance; Compliance **Abstract** A hydraulic teaching model of the human systemic circulation is proposed, based on the principles of the reservoir-wave approach. Reservoir characteristics are portrayed by the arterial tall-and-narrow and venous short-and-wide columns, the relative compliances of which are signified by their diameters. Wave characteristics are represented by proximal arterial and venous resistances; rapid left ventricular ejection and rapid right atrial filling cause flow-dependent pressure drops across the respective resistances. (The value of the proximal arterial resistance is numerically equal to the characteristic impedance.) The pressure drop across the proximal arterial resistance, excess pressure, is understood to be fundamentally wave-related and has been shown to be a measure of the efficiency of cardiac-vascular coupling. Excess pressure also predicts an incremental risk of cardiovascular morbidity and largely accounts for the hysteresis evidenced by an open aortic pressure-volume loop. © 2015 Association for Research into Arterial Structure and Physiology. Published by Elsevier B.V. All rights reserved.

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Recent conceptual advances regarding wave travel in the systemic circulation point to the need of a new teaching diagram that would represent these advances semiquantitatively, intuitively, and accurately.

With this new teaching diagram (Fig. 1), we consider the heart to be a pulsating, reciprocating pump that, by generating waves that increase pressure and velocity, transfers blood from the low-pressure/high-compliance venous reservoir (on the right) to a high-pressure/low-compliance arterial reservoir (on the left), somewhat similar to the model proposed by Shoukas and Sagawa.<sup>1</sup> The reservoirs are separated functionally by a resistance — conventionally, by systemic vascular resistance but, as explained below, by a series of resistances that we have defined.<sup>2</sup> The higher the cardiac output, the higher the pressure in the arterial reservoir and the lower the pressure in the venous reservoir. Blood flows passively from the arterial to the venous reservoir via the microcirculatory resistance (v.i.).



Figure 1 A hydraulic model of the systemic circulation illustrating the essential features of the reservoir-wave approach. The left ventricle is represented by the cylinder and piston, coupled to a crank. Pressure transducers are represented schematically. Note that arterial  $(P_{A-res})$  and venous (P<sub>V-res</sub>) pressures are measured at the bottom of their respective reservoirs, thus reflecting the height of the column of liquid, measured in mmHg. The dark-blue segments at the tops of the arterial and venous reservoirs indicate the typical amplitudes of the changes in reservoir pressures. Aortic root (Paortic root) and right atrial (Pright atrium) pressures are respectively higher and lower than their reservoir pressures, because of the flow-related pressure drops across the large artery (R<sub>large artery</sub>) and large vein (R<sub>large veins</sub>) resistances. The relative magnitudes of the resistances are represented by their lengths and correspond approximately to the values calculated from data measured in the normal dog.<sup>37</sup> The Starling resistor between the arterial reservoir  $(R_{A-res})$  and venous reservoir  $(R_{V-res})$ res) resistances is represented schematically as a pressurized chamber ( $P_{\infty}$ ) that encloses a collapsible segment of tubing.

Guyton's approach to the relation between venous return (cardiac output in the steady state) and systemic venous pressure<sup>3</sup> is well-known but Levy<sup>4</sup> offered a provocative alternative interpretation in which the inverse relation between cardiac output and central venous pressure was explained as increasing cardiac output depleting the venous reservoir, as shown in Fig. 1. Further, we developed an approach whereby the mobilization of peripherally stored blood, sometimes attributed to "increased venous return", is represented instead by a shift in a venous pressure—volume relationship toward the pressure axis.<sup>5–10</sup> Shifts in the venous pressure—volume relationship occur over several seconds or minutes.

Wave intensity analysis (WIA) and the reservoir-wave approach (RWA) focus on individual cardiac cycles which, with this new teaching model, we attempt to accommodate. WIA was developed by Parker and his colleagues.<sup>11,12</sup> Wave intensity is calculated from the differentials of pressure and velocity and has the outstanding features of being able to discriminate forward from backward waves and to identify their character - whether they increase (compression waves) or decrease (decompression waves) pressure as they pass. However, it later became clear to us that although waves change pressure, pressures may also change if the volume of an elastic vessel changes or if the elastance of a cardiac chamber changes.<sup>13</sup> Thus, we modified WIA such that the volume- or elastancedependent change in pressure is calculated first and then subtracted from the measured pressure.<sup>13</sup> This yields "excess pressure",14 which we interpret as being fundamentally wave-related. We have called this modified analvsis the RWA.<sup>15,16</sup> The essential concepts of the RWA are illustrated in Fig. 2,<sup>15</sup> in which changes in reservoir pressure may thought to be analogous tidal excursions over which changes in wave pressure may be superimposed.

The new model (Fig. 1) differs from the previous one<sup>9</sup> by the presence of a cyclic pump with inflow and outflow valves and a detailed representation of the arterio-venous resistance (systemic vascular resistance). A resistor between the left ventricle ( $R_{large artery}$ ) and the arterial reservoir and another, between the venous reservoir and the right atrium ( $R_{large vein}$ ), have been added. As others have done,<sup>4</sup> the pulmonary circulation has been ignored for simplicity at the current time. However, an equivalent pulmonary model could be constructed, based on the recent findings of Bouwmeester et al.<sup>17–19</sup> Also, the



**Figure 2** A figure illustrating the concept that changes in measured aortic pressure are equal to the sum of the changes in reservoir pressure and wave (excess) pressure. (From Tyberg et al.<sup>15</sup> with permission of Elsevier Ireland Ltd.)

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