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Technical Section

Improving spatial perception of vascular models using supporting anchors and illustrative visualization $\stackrel{\star}{\sim}$

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ABSTRACT

Incorrect spatial interpretation of 3D vascular models is a main perceptional problem in medical visualization. For improved depth perception, we propose supporting anchors between vascular trees and a cylindrical cutaway that serves as an insight for a virtual resection surface or a path for a tumor ablation. The supporting anchors are optimally arranged in a circular manner such that the depth can be perceived without time-consuming interaction. For improved shape perception and distance-encoding, we additionally employ a novel and fast hatching approach that produces results comparable to state-of-theart techniques. The advantages of our new visualization approach are demonstrated using the example of laparoscopic liver surgery and confirmed in a quantitative user study with 81 participants. The results show that participants were able to assess relative distances more precisely and were most confident using our illustrative visualization approach.

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1 1. Introduction

During medical interventions, it is often important to under-2 stand the morphology of vascular structures and its spatial re-3 4 lation to surrounding risk structures such as tumors. Therefore, 5 high-quality vascular 3D models, reconstructed from computed tomography (CT), are applied using direct or indirect volume ren-6 7 dering techniques [1] and medical augmented reality visualization 8 [2-4]. The vascular models often portray complex geometries and 9 therefore demand cognitive effort and user interaction.

While the interaction with a 3D model (scaling, rotation, pan-10 ning) can be easily integrated in surgery planning, such interaction 11 is hard to perform during an intervention due to the constraints of 12 a sterile room [5]. This is complicated by the fact that physicians 13 often request a multilayer visualization to display different depth 14 layers of an anatomical object, e.g., vascular structures and tumors 15 underneath an organ surface, in which layers are rendered on top 16 of each other. An effective multilayer visualization of the depth lay-17 18 ers that represents the medical image data during an intervention 19 is hampered by structures (vessels, organ surface, tumors, etc.) that

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http://dx.doi.org/10.1016/j.cag.2017.02.002 0097-8493/© 2017 Published by Elsevier Ltd. occlude each other. Adding object transparency may aggravate the
perception of relative depth distances between virtual 3D objects
(layer clutter). Therefore, a visualization to support medical inter-
ventions should encode essential information as the location, spa-
tiality, and distances to important anatomical structures in a clear
and non-misleading way.20

In this work, we introduce an illustrative visualization approach 26 that faces the above-mentioned problems and aims to improve 27 spatial perception for medical augmented reality visualization. We 28 introduce supporting anchors that are based on supporting lines in-29 troduced by Lawonn et al. [6]. Supporting lines proved to be a 30 strong depth cue in 3D vascular visualization. However, this ap-31 proach cannot be applied to augmented reality visualization, as 32 they used a floor to project their supporting lines onto, which en-33 tails a direction that is not given. Another disadvantage of their 34 approach is that the lines were placed manually. To improve upon 35 this method, we present an algorithm that automatically finds 36 the optimal positions for the supporting anchors. In addition, we 37 present a new hatching technique for complex vascular structures. 38 Compared to state-of-the-art hatching approaches, the new tech-39 nique enables lower memory usage and faster computation time, 40 while showing comparable visualization results. In this work, the 41 hatching technique is utilized to convey shape and encode the dis-42 tance between vessels and tumors. 43

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The advantages of our approach were confirmed in a quantitae user study with 81 participants. Because Kersten-Oertel et al. the rendering style for occluded objects, e.g., using a wireframe 105 representation [25] or transparency [26]. 106

2.2. Improving spatial perception using line drawings

tive user study with 81 participants. Because Kersten-Oertel et al.
[7] rated pseudo-chromadepth rendering as the best depth cue
for vascular visualization, we compared our illustrative visualization technique with pseudo-chromadepth rendering [8], and Phong
shading [9] without an explicit depth cue.

50 2. Related work

Incorrect spatial interpretation is the most common perceptual problem in augmented reality (AR) applications [10]. The need to assess spatial information from superimposed 3D models precisely during an intervention has led to the development of several techniques that improve spatial perception in AR.

56 2.1. Improving spatial perception for medical visualization

Stereoscopic vision improves the spatial assessment of 57 computer-generated images [11–14]. Therefore, autostereoscopic 58 monitors or head-mounted displays can be of great value in the 59 operating room (OR). For many surgeons, additional hardware 60 is cumbersome or difficult to use within the constraints of the 61 62 OR [15]. In addition, the benefit of stereoscopic vision is taskdependent, and the results of Kersten-Oertel et al. [15] indicate 63 that it does not provide effective spatial cues for the depth 64 judgment of 3D vascular models. 65

66 Computer-generated monoscopic depth cues have been pro-67 posed to improve spatial perception. Kinetic depth, especially motion parallax, provides depth cues in many AR applications [16,17]. 68 A virtual window was introduced by Sielhorst et al., which sim-69 70 ulates a view of the patient's viscera [18]. The window plane is slightly textured to improve spatial perception through partial oc-71 72 clusion when using a tracked head-mounted display. Projection of guidance graphics, such as entry points and surgical plans, onto an 73 organ surface while tracking the operator's head using projector-74 based AR has been proposed [19,20]. A disadvantage of kinetic 75 76 depth is that the operator's head needs to be tracked. This leads 77 to additional hardware in the OR, and forces operators to continuously move their head to improve the spatial impression. 78

Color coding can also be employed to encode depth and inter-79 object distance in AR. Ropinski et al. [8] introduced pseudo-80 81 chromadepth rendering as an enhancement of the chromadepth rendering, where the number of hues were reduced. According to a 82 user study by Kersten-Oertel et al. [15], pseudo-chromadepth ren-83 dering allows for the best relative depth assessments for vascular 84 structures. However, a recent study by Lawonn et al. [6] showed 85 86 that illustrative rendering techniques could improve depth as-87 sessment results over pseudo-chromadepth rendering. In addition, 88 multiple viewports are proposed as a method to improve the spa-89 tial perception for AR. To visualize inter-object distances in AR en-90 vironments, seamless switching between an AR view and a virtual 91 reality (VR) view was proposed [21]. Bichlmeier et al. [22] presented virtual mirrors, a render-to-texture approach, which pro-92 vides additional views of the model. The interpretation of partial 93 self-occlusions inside complex models is particularly improved. 94

The correct display of occlusion between 3D virtual models and 95 96 real objects, e.g., patient, operator, and instruments, on a 2D sur-97 face is important to convey spatial relations. An information fil-98 ter based on intra-operative distance measures was introduced to reduce occlusion of anatomical structures by virtual overlays [23]. 99 Fischer et al. [24] propose providing a distance map of the real 100 scene using a time-of-flight (TOF) camera. By performing registra-101 tion between the distance map and virtual 3D models, the distance 102 map is used to decide which objects are rendered at the front and 103 to control the rendering style. A common approach is to change 104

Feature Lines. Line-drawing techniques illustratively visualize the 108 object's shape. These can be divided into two groups: feature lines 109 and hatching. The first view-independent approach was presented 110 by Interrante et al. [27], who used curvature measures to deter-111 mine the ridges and valleys of the surface. Because this approach is 112 not view-dependent, DeCarlo et al. [28] introduced suggestive con-113 tours. Their method cannot depict salient regions of convex struc-114 tures. Thus, Judd et al. [29] combined the ridges and valley method 115 with a view-dependent curvature measure to detect even convex 116 structures. An illumination-based approach was introduced by Xie 117 et al. [30]. They used the shading of the surface to determine the 118 most prominent regions. As this approach is only based on shad-119 ing, it is possible to influence the result by adding more light 120 sources such that noisy regions are illustrated with less clutter. A 121 similar approach was introduced by Zhang et al. [31]. They gener-122 alized the Laplacian-of-Gaussian, a well-known technique that il-123 lustrates features in images, to surfaces. This approach was then 124 adapted to the difference-of-Gaussian that was known in image-125 space before by Zhang et al. [32]. Feature line techniques can en-126 hance spatial cues on the surface, but they cannot give a spatial 127 impression of the surface [33]. 128

Hatching. Most hatching methods use principle curvature direc-129 tions (PCDs) to orient the directions of the lines. Hertzmann and 130 Zorin [34] determined the PCDs and smoothed them afterwards. 131 Then, they generated streamlines to obtain a hatched result. Praun 132 et al. [35] presented a real-time hatching method. They built 133 lapped textures which represent the different shading levels on a 134 surface and projected them onto the surface. Zander et al. [36] pre-135 sented a hatching method which is based on generating stream-136 lines around the whole surface. For this, the PCDs were calculated 137 and smoothed accordingly. Then, they were used to generate the 138 hatching strokes represented as streamlines. In addition, the PCDs 139 ensure that neighboring streamlines have a minimum distance, to 140 prevent too many streamlines from occurring in a region. Tietjen 141 et al. [37] presented examples for the combination of classical and 142 illustrative rendering techniques on surfaces and volumes to pro-143 vide expressive focus-and-context visualizations for medical appli-144 cations. 145

Lawonn et al. [38] presented ConFIS – a hatching technique that 146 illustrates the surface at feature regions and at the contour. The 147 work of Ritter et al. [39] is close to our work and is guided by 148 a similar set of requirements and application scenarios. They in-149 troduced a hatching method which is not applicable in a frame-150 coherent manner. In addition, they presented a distance-encoding 151 stripe texture which requires distortion-free texture coordinates. 152 For complex vascular structures, as in our case, these are hard to 153 calculate automatically, which limits the applicability of their ap-154 proach. Furthermore, the stripe texture covers the whole object 155 surface and thus can hardly be combined with other illustrative 156 rendering techniques [4]. 157

Focus-and-context visualization. Illustrative rendering techniques 158 can also improve the spatial perception for focus-and-context vi-159 sualization. Different cutaway approaches to achieve interactive 160 frame rates were introduced by Diepstraten et al. [40]. Viola et al. 161 [41] proposed a technique to illustrate view-dependent cutaway 162 surface generation. Their method is based on volume rendering, 163 where segmented objects have an importance, which is used to de-164 fine the cutaway. An approach where the user needs to cut a hole 165 in the surface to reveal the underlying objects was presented by 166

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