



Q1 Antimicrobial silver-filled silica nanorattles with low immunotoxicity in  
Q2 dendritic cells

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10 **Abstract**

11 The progression in the use of orthopedic implants has led to an increase in the absolute number of implant infections, triggering a search  
12 for more effective antibacterial coatings. Nanorattles have recently gained interest in biomedical applications such as drug delivery, as  
13 encapsulation of the cargo inside the hollow structure provides a physical protection from the surrounding environment. Here, silver-  
14 containing silica nanorattles (Ag@SiO<sub>2</sub>) were evaluated for their antimicrobial potential and for their impact on cells of the immune system.  
15 We show that Ag@SiO<sub>2</sub> nanorattles exhibited a clear antibacterial effect against *Escherichia coli* as well as *Staphylococcus aureus* found in  
16 post-operative infections. Immunotoxicological analyses showed that the particles were taken up through an active phagocytic process by  
17 dendritic cells of the immune system and did not affect their viability nor induce unwanted immunological effects. Silver-containing silica  
18 nanorattles thus fulfill several prerequisites for an antibacterial coating on surgical implants.

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20 *Key words:* Silver nanoparticles; Silica nanocontainers; Nanorattles; Dendritic cells; Immunoresponse; Antimicrobial properties

21 *Abbreviations:* AgNPs, silver nanoparticles; Ag@SiO<sub>2</sub>, silver-containing nanorattles; Ag@FITC-SiO<sub>2</sub>, silver-containing fluorescent nanorattles; TEM, transmission electron microscope; FTIR, Fourier transform infrared spectroscopy; DLS, dynamic light scattering; FITC, fluorescein; BMDC, bone marrow-derived dendritic cells.

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Each year, a large number of patients undergo joint replacement surgery. Postoperative prosthetic joint infection is a severe complication after arthroplasty that affects 1% to 3% of patients,<sup>1</sup> leading initially to surgical and antibiotic treatment and frequently ending with a need for replacement of the implant.<sup>2,3</sup> It is thus of great importance to develop intelligent nanomaterials which prevent infections and are biocompatible at the same time.<sup>4</sup>

With the emergence of bacterial resistance to conventional antibiotics, silver-based compounds and silver nanoparticles again enjoy rising popularity<sup>5–12</sup> as antimicrobial and healing agents.<sup>13,14</sup> Undoubtedly, the greatest advantage of silver originates from its multidirectional mode of action against microbes. In contrast to single-target antibiotics, the development of resistance is thus more difficult and requires several sequential mutations in the bacterial cell.<sup>14,15</sup> At concentrations within a therapeutic window, silver does not exhibit adverse effects toward mammalian cells while at the same time preventing bacterial survival.<sup>14</sup>

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Ag(I)-containing coordination polymers demonstrate good biocompatibility as well as antimicrobial activity, making them promising candidates to fight biomaterial-related infections.<sup>16–18</sup> However, despite their excellent properties, silver is released rapidly during the first weeks after synthesis, leading to a short-term efficacy. For a better controlled, long-term release of silver cations, we propose to use encapsulated silver nanoparticles (AgNPs) as a source of silver cations<sup>19,20</sup> in an inorganic nanocarrier. Nanorattles composed of silica shells may serve as alternatives for silver-based drug delivery because of the possibility of drug loading in their cavity.<sup>21–24</sup> These nanorattles present a strong advantage as they provide a physical barrier for drug protection against the biological environment.<sup>25,26</sup>

Nanoparticles can exhibit immunological effects: particulate material can induce the secretion of proinflammatory cytokines by cells of the immune system<sup>27</sup> or on the contrary suppress immune functions.<sup>28</sup> It is furthermore well established that following arthroplasty, nano-sized debris detach from the implant through wear mechanisms.<sup>29</sup> These debris can interact both locally and systemically with immune cells and induce the release of pro-inflammatory cytokines such as IL-6. In the case of NP designed for biomedical applications such as implant coating, it is therefore critical to carefully assess the impact of particles on the activity of immune cells.

Despite the exceptional antimicrobial properties of AgNPs against bacteria,<sup>30</sup> fungi<sup>31</sup> and viruses,<sup>32</sup> few studies on the preparation of antibacterial nanorattles have been reported so far. Wei et al<sup>33</sup> described Ag@Fe<sub>2</sub>O<sub>3</sub> nanorattles with conjugated glucose. This system serves as an example of multifunctional nanorattles in which glucose captures the bacteria, silver kills them and the magnetic shell allows the efficient removal of the nanorattles from the contaminated drinking water.

Here, we report the synthesis of silica nanorattles filled with silver (Ag@SiO<sub>2</sub>) made by a microemulsion approach.<sup>34</sup> A first screen to assess whether the Ag@SiO<sub>2</sub> particles fulfill a set of requirements in order to be considered for the coating of orthopedic implants was carried out. Antibacterial properties of Ag@SiO<sub>2</sub> were tested against both gram-negative and gram-positive bacteria, while the cytotoxicity and the proinflammatory activity were determined with primary immune cells. Additionally, we generated for the first time AgNPs encapsulated inside fluorescent silica shells (Ag@FITC-SiO<sub>2</sub>) to determine cellular uptake.

## Methods

### *Synthesis of nanocontainers and nanorattles*

Non-fluorescent and fluorescent nanorattles were prepared under argon according to the compositions shown in Table S1. First, 1.4 mL of water or AgNO<sub>3</sub> (AppliChem, Darmstadt, Germany) aqueous solution (0.01 or 0.05 or 0.1 M) was slowly injected under vigorous stirring into a mixture consisting of 29.6 g of cyclohexane (Sigma-Aldrich, Buchs, Switzerland) and 3.5 mL of Igepal CO-520 (Sigma-Aldrich, Buchs, Switzerland) at 28 °C. After 2 hours, 75 µL of hydrazine monohydrate (Fluka, Buchs, Switzerland) was added and left for 2 hours. Then, silica precursors were added dropwise: first, the non-fluorescent ones

(200 µL of tetraethyl orthosilicate (Sigma-Aldrich, Buchs, 96 Switzerland), 50 µL of 12.5 v/v% ethanolic solution of 97 APTMS) and after 1 hour, the fluorescent one (50 µL of 98 ethanolic solution of FITC-APTMS). After another hour, 500 µL 99 of 28-30% aqueous NH<sub>3</sub> was slowly injected and the reaction 100 was stirred for 36 hours. The microemulsion was destabilized by 101 addition of 25 mL ethanol. The resulting precipitate was 102 collected under centrifugation (15,000 rpm, 30 min, room 103 temperature), washed twice with 25 mL ethanol and 25 mL 104 ultrapure water (15,000 rpm, 15 min, room temperature). Final 105 washing with 20 mL warm ultrapure water (60 °C, 40 min, 106 stirring) followed by centrifugation (15,000 rpm, 15 min, room 107 temperature) resulted in the formation of the void in the silica 108 spheres. Calcination of non-fluorescent NPs was performed 109 during TGA analysis (SDTA/TGA 851°, Mettler Toledo AG, 110 Greifensee, Switzerland) using aluminum crucibles (40 µL). The 111 measurement was conducted in the presence of nitrogen gas and 112 air to provide combustion of organic residues. The temperature 113 ranged from 25 to 600 °C, with a heating rate of 10 K min<sup>-1</sup>. 114

### *Characterization of nanocontainers and nanorattles*

Morphology of the samples is characterized by transmission 116 electron microscopy (TEM) (CM-100 Biotwin Transmission 117 Electron Microscope, FEI/Philips, Hillsboro, Oregon, USA) at 118 the operating voltage of 80 kV, in bright field mode. Sample 119 preparation included a sonication of NPs in ultra-pure water. A 120 drop of diluted suspension was deposited on the TEM grid 121 (Electron Microscopy Sciences, CF 300-Cu, Carbon Film on 300 122 Square Mesh Copper Grids) and let to dry. 123

UV-Vis spectra of nanoparticle suspensions were recorded with 124 UV/Vis Spectrometer (Lambda40, Perkin Elmer, Schwerzenbach, 125 Switzerland) at wavelengths ranging from 250 to 800 nm. The 126 fluorescence spectra were measured by using a Luminescence 127 Spectrometer LS 50B (Perkin Elmer, Schwerzenbach, Switzerland) 128 and the Software FL Win Lab. The samples were excited at  $\lambda =$  129 492 nm and the spectra were measured within  $\lambda = 400-600$  nm 130 (Ex. Slit = 5.0, Scan Speed = 100). 131

### *Silver loading and release*

The amount of silver for each type of nanorattle was 133 determined by ICP after resuspension in nitric acid (32.5%) 134 with ultrasonication. For the silver loading 2-4 mg of Ag@SiO<sub>2</sub> 135 nanorattles were suspended in concentrated nitric acid to reach 136 0.3 mg mL<sup>-1</sup> and sonicated for about 3 hours before ICP 137 measurements. For silver release analysis 10 mg of Ag@SiO<sub>2</sub> 138 nanorattles were resuspended in 5 mL water by vortexing and 139 sonication (30 min). After dilution to a concentration of 0.2 mg 140 mL<sup>-1</sup> the suspension was split into samples of 1 mL. Those were 141 shaken at 37 °C (200 rpm) in the dark for the required time 142 periods. After centrifugation (2 h, 17,000 rpm) 0.5 mL of the 143 supernatant was taken for ICP analysis. Each time point was 144 analyzed in triplicate. 145

### *Spread plate method*

Ag@SiO<sub>2</sub>-3 nanorattles were resuspended in filtrated distilled 147 water and sonicated for 30 minutes. In general, first 100 µL of 148 Ag@SiO<sub>2</sub> suspension and then 10<sup>3</sup> to 10<sup>6</sup> cfu mL<sup>-1</sup> of 149

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