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Interfacial behavior of PEGylated lipids and their effect on the stability of squalenoyl-drug nanoassemblies

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ABSTRACT

Squalenoyl-gemcitabine (Sq-Gem) and squalenoyl-deoxycytidine (Sq-ddC) are amphiphilic prodrugs that self-assemble in water to form nanoassemblies (NAs) with well-defined structures and size. However, like other drug nanocarriers, these nanoassemblies are rapidly cleared from the blood stream by the reticuloendothelial system. By adding squalenoyl-PEG (Sq-PEG) or cholesterol-PEG (Chol-PEG) to the squalenoyl prodrugs, composite nanoassemblies (CNAs) were formed, with different sizes and structures. The effect of the PEG-lipids on the formation and stability of these nanoassemblies was assessed by transmission electron microscopy, quasi-elastic light scattering and surface tension measurements in various conditions. The results revealed different stabilities with time for Sq-ddC and Sq-Gem nanoassemblies in aqueous medium, the latter being much less stable than the former. They also demonstrated that the presence of Sq-PEG or Chol-PEG in composite Sq-ddC nanoassemblies contributed to their rapid destabilization. The analysis of the adsorption kinetics of Sq-PEG into a prodrug monolayer below and above its critical aggregation concentration allowed getting a better insight into prodrug-lipopolymer molecular interactions, and their consequences on the formation of composite prodrug nanoassemblies.

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⁶ **1. Introduction**

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Biocompatible nanostructures formed by self-assembling of amphiphilic prodrugs show remarkable therapeutic potential as they combine high drug loading, improved drug controlled release, and reduced toxicity compared to common nanocarriers. They are particularly appropriate for drugs with critical limitations like low oral bioavailability, rapid metabolism, short circulation half-life, induced resistance and severe side-effects. Many systems have been developed over the last decade, such as long-chain alkyl or cholesteryl conjugates of nucleoside anticancer and antiviral agents forming colloidal dispersions (Jin et al., 2006, 2009, 2012b). In 2006, Couvreur and co-workers have proposed an original strategy to increase the therapeutic index of nucleoside analogues by coupling them to the acyclic isoprenoid chain of squalene (Sq). Squalene is a natural nontoxic lipid, widely distributed in the nature and precursor

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21 in cholesterol biosynthesis (Desmaële et al., 2012; Dosio et al., 2013; 22 Reddy and Couvreur, 2009). Remarkably, coupling squalene to 23 nucleosides analogues led to amphiphilic prodrugs, which self-24 organized in water as nanoassemblies (NAs) of 100-300 nm in 25 diameter, irrespective of the nucleoside analogue used and the 26 location of the covalent linkage. This has been assigned to the highly 27 coiled and compact conformation of the squalene moiety in water 28 (Cattel et al., 1992). This strategy has been first successfully applied to 29 gemcitabine, a pyrimidine nucleoside analogue used in chemother-30 apy to treat non small-cell lung cancer, pancreatic, bladder, ovarian 31 and breast cancers (Eli Lilly Co., 1997; Sandler and Ettinger, 1999). The 32 squalenoyl gemcitabine nanoassemblies (Sq-Gem) were found to 33 exhibit superior anticancer activity in vitro in human cancer cells and 34 in gemcitabine-resistant murine leukemia cells, as well as in vivo in 35 experimental leukemia both after intravenous and oral adminis-36 tration (Couvreur et al., 2006; Reddy et al., 2007, 2008a, 2008b). The 37 squalenoylation of other antiretroviral nucleosides (including 38 2',3'-dideoxycytidine, ddC) also led to more potent drugs when 39 tested in primary cultures of HIV-infected lymphocytes (Hillaireau 40 et al., 2013). High-resolution synchrotron X-ray diffraction and 41 electron microscopy studies revealed that whereas Sq-Gem 42 molecules were packed in inverse hexagonal phases (Couvreur

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et al., 2008), Sq-ddC molecules organized in an inverse bicontinuous
cubic phase in equilibrium with excess water (Bekkara-Aounallah
et al., 2008).

46 It has been well established in earlier studies that drug-loaded 47 nanocarriers are rapidly removed from the blood stream by the 48 reticulo-endothelial system, and cannot reach their target (for 49 example a tumor). A preferred strategy to dramatically increase 50 their blood half-lives is the covalent coupling of poly(ethylene 51 glycol) (PEG) chains (PEGylation) at their surface (Gref et al., 1994; 52 Needham and Kim, 2000; Peracchia et al., 1998). For Sq-ddC, 53 PEGylation could seem unnecessary since macrophages are the 54 main HIV reservoirs (Aquaro et al., 2002; Jin et al., 2009). However, 55 it has been shown that HIV reservoirs located in the brain are 56 particularly difficult to eradicate, because it necessitates passage of 57 the nanocarriers across the blood-brain barrier (BBB) (Lafeuillade 58 and Stevenson, 2011; Namanja et al., 2012; Thompson et al., 2011). 59 Crossing BBB was shown to be possible by coating the nanocarriers 60 with PEG shells and appropriate ligands (Huang et al., 2013; Lu 61 et al., 2014,; Zhang et al., 2014). PEGylation may also favor 62 stabilization of nanoparticles intended for oral delivery (Belogui 63 et al., 2013; Hillaireau et al., 2013; Shen et al., 2013; Yoncheva et al., 64 2005). Pioneering studies have shown that PEGylation of Sq-ddC 65 and Sq-Gem nanoassemblies was possible. Composite NAs (CNAs) 66 were formed by co-nanoprecipitation using prodrugs mixed with 67 either cholesterol-PEG (Chol-PEG) or squalene-PEG (Sq-PEG), in 68 the absence of any other surfactant. The preparation procedure was 69 successful, as in all cases monodisperse colloidal suspensions of 80 70 upto 200 nm in diameter CNAs were obtained without aggregates, 71 whatever the weight ratio (from 1:0.002 to 1:0.7) between the 72 squalenoyl nucleoside analogue and the PEG-lipid (Bekkara-73 Aounallah et al., 2008). The higher the PEG ratio was, the smaller 74 the size of the resulting nanoassemblies. Similarly, Duhem et al. 75 (2014) have recently reported that the addition of TPGS₂₀₀₀ to 76 *N*-doxorubicin- α -D-tocopherol succinate significantly reduced the 77 size of prodrug aggregates.

78 Many questions remain to fully understand the formation of the 79 CNAs and their supramolecular organization, which are crucial for 80 their use in biomedical applications. It is anticipated that the PEG 81 coating, responsible for the increased in vivo half-lives, establishes 82 during NAs formation at the interface between the organic droplets 83 and the aqueous phase. However, when preparing CNAs, there 84 might be competition at the interface between Sq-ddC and Chol-85 PEG or Sq-PEG molecules. Physico-chemical studies at the 86 interfaces would, therefore, be decisive for a better understanding 87 of the CNAs formation. Besides, crucial information could be 88 obtained on the stability of the resulting CNAs.

89 The present study shows new data on the interfacial behavior of 90 Sq-ddC, Sq-Gem and Chol-PEG or Sq-PEG mixtures, as well as on 91 the stability of composite nanoassemblies. We have first deter-92 mined the critical aggregation concentration of Chol-PEG and Sq-93 PEG, studied the interfacial behavior of prodrug nanoassemblies 94 and composite PEG/prodrug nanoassemblies at the free air/water 95 interface. The analysis of the kinetics of films formation, changes in 96 morphology of nanoassemblies upon addition of the PEGylated 97 lipids, and adsorption of a PEG-lipid into a prodrug monolayer, 98 below and above its critical aggregation concentration allowed to 99 get a better insight into the organization and stability of CNAs in 100 the presence of Sq-PEG and Chol-PEG.

¹⁰¹ **2. Material and methods**

¹⁰² 2.1. Materials

¹⁰³ Zalcitabine (2',3'-dideoxycytidine, ddC, Mw: 211 g mol⁻¹) and
¹⁰⁴ squalene were purchased from Sigma–Aldrich Chemical Co., France.
¹⁰⁵ Gemcitabine hydrochloride (Sq-Gem, Mw: 299.66 g mol⁻¹) was

106 provided by Sequoia Research Products (UK). The squalenoyl 107 nucleoside analogues Sq-ddC $(593.9 \,\mathrm{g}\,\mathrm{mol}^{-1})$ and Sq-Gem 108 $(645.82 \text{ g mol}^{-1})$ were synthesized by covalent coupling with 109 1,1',2-tris-nor-squalenic acid (Sq-Ac) onto the amino group of the 110 nucleosides heterocycle as previously described (Couvreur et al., 111 2006). Squalene-poly(ethyleneglycol) (Sq-PEG, 2380 g mol^{-1}) was 112 synthesized and characterized as reported earlier (Bekkara-Aou-113 nallah et al., 2008). Cholesterol-poly(ethyleneglycol) (Chol-PEG) 114 (1982 g mol⁻¹) was supplied from NOF Europe (Belgium). Ultrapure water (γ = 72.4 mN m⁻¹ at 22 °C) was produced by a Millipore 115 116 Synergy 185 apparatus coupled with a RiOs5, with a resistivity of 117 18.2 M Ω /cm. Prior to experiments, glassware was cleaned in a TFD4 118 solution (Franklab) and abundantly rinsed with ultrapure water.

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3. Methods

3.1. Preparation of the nanoassemblies

Sq-Gem and Sq-ddC nanoassemblies (1.55 mM and 1.68 mM, respectively) were prepared by nanoprecipitation. Briefly, a prodrug was dissolved in acetone (10 mg mL^{-1}) and added dropwise under stirring (500 rpm) into 2 mL water. Composite nanoassemblies (CNAs) were prepared by co-nanoprecipitation of a prodrug with either Chol-PEG or Sq-PEG. Precipitation of nanoassemblies occurred spontaneously at room temperature. After solvent evaporation under reduced pressure, an aqueous suspension of nanoassemblies was obtained. Different Chol-PEG or Sq-PEG molar ratios were tested, ranging from 0.05% to 21%. Squalenic acid (Sq-Ac) could also self-aggregate and form nanoassemblies, but x-ray diffraction analysis showed none of the structures observed for Sq-Gem or Sq-ddC nanoparticles. Apparently, the Sq-Ac nanoassemblies were not organized enough to produce a diffraction spectrum. They also showed poor stability with time.

For all experiments, the composite nanoassemblies were freshly prepared and used within 24 h (conservation at 4°C). Their size and polydispersity index (PDI) were measured immediately after preparation, by quasi-elastic light scattering (QELS) (Zetasizer 4, Malvern Instruments Ltd., UK). The selected angle was 90° and the measurement was made using a 50 μ g mL⁻¹ concentration in MilliQ[®] water.

The morphology of nanoassemblies and composite nanoassemblies was visualized using transmission electron microscopy (TEM), directly or after freeze-fracture (FF-TEM). For direct TEM observations, 5 μ L of aqueous nanoassemblies suspensions were deposited onto a 600 mesh copper grid coated with a very thin carbon film. Grids were washed with 5 μ L of aqueous 2% (w/v) uranyl acetate, dried and observed in annular dark-field, in a LEO-Zeiss 902 electron microscope. For FF-TEM observations, 1 mL of nanoassemblies suspension (1 mg mL⁻¹) was incubated with glycerol (30% v/v), used as a cryoprotectant. A drop of each sample was placed on a copper support, immediately frozen in liquid propane, and then kept in liquid nitrogen. Fracturing and shadowing were performed in a Balzers BAF 400 freeze-etching unit. The replicas were washed in THF and distilled water, and placed on copper grids. Observations were made under a TEM JEOL 100SX.

3.2. Surface tension measurements

Equilibrium surface tensions γ of the Chol-PEG and Sq-PEG160solutions were measured at 22 ± 1 °C by the Wilhelmy plate161method using a digital tensiometer (K10ST, Krüss, Germany). The162surface tension of NAs and CNAs was measured with time, without163detaching the plate from the interface. The thermostated164measurement cells were enclosed in a chamber under saturated165vapor pressure to limit water evaporation during the experiments166

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