Quantification of Myocardial Blood Flow in Absolute Terms Using ⁸²Rb PET Imaging



The RUBY-10 Study

Sergey V. Nesterov, MD, PhD, PMP,*† Emmanuel Deshayes, MD, MSc,‡§ Roberto Sciagrà, MD,||
Leonardo Settimo, MD,|| Jerome M. Declerck, PhD,¶ Xiao-Bo Pan, PhD,¶ Keiichiro Yoshinaga, MD, PhD,#
Chietsugu Katoh, MD, PhD,# Piotr J. Slomka, PhD,** Guido Germano, PhD,** Chunlei Han, MD, PhD,*
Ville Aalto, MSc,* Adam M. Alessio, PhD,†† Edward P. Ficaro, PhD,‡‡ Benjamin C. Lee, PhD,§§
Stephan G. Nekolla, PhD,|||| Kilem L. Gwet, PhD,¶¶ Robert A. deKemp, PhD, PENG, PPhys,## Ran Klein, PhD,##
John Dickson, PhD,*** James A. Case, MD, PhD,††† Timothy Bateman, MD, PhD,††† John O. Prior, MD, PhD,‡
Juhani M. Knuuti, MD, PhD*

ABSTRACT

OBJECTIVES The purpose of this study was to compare myocardial blood flow (MBF) and myocardial flow reserve (MFR) estimates from rubidium-82 positron emission tomography (⁸²Rb PET) data using 10 software packages (SPs) based on 8 tracer kinetic models.

BACKGROUND It is unknown how MBF and MFR values from existing SPs agree for 82Rb PET.

METHODS Rest and stress ⁸²Rb PET scans of 48 patients with suspected or known coronary artery disease were analyzed in 10 centers. Each center used 1 of 10 SPs to analyze global and regional MBF using the different kinetic models implemented. Values were considered to agree if they simultaneously had an intraclass correlation coefficient >0.75 and a difference <20% of the median across all programs.

RESULTS The most common model evaluated was the Ottawa Heart Institute 1-tissue compartment model (OHI-1-TCM). MBF values from 7 of 8 SPs implementing this model agreed best. Values from 2 other models (alternative 1-TCM and Axially distributed) also agreed well, with occasional differences. The MBF results from other models (e.g., 2-TCM and retention) were less in agreement with values from OHI-1-TCM.

CONCLUSIONS SPs using the most common kinetic model—OHI-1-TCM—provided consistent results in measuring global and regional MBF values, suggesting that they may be used interchangeably to process data acquired with a common imaging protocol. (J Am Coll Cardiol Img 2014;7:1119–27) © 2014 by the American College of Cardiology Foundation.

From the *Turku PET Centre, University of Turku and Turku University Hospital, Turku, Finland; †IM Sechenov Institute of Evolutionary Physiology and Biochemistry RAS, St. Petersburg, Russia; †Lausanne University Hospital, Lausanne, Switzerland; §Regional Cancer Institute of Montpellier (ICM)-Val d'Aurelle, Montpellier, France; ||University of Florence, Florence, Italy; ¶Siemens Molecular Imaging, Oxford, United Kingdom; #Hokkaido University Graduate School of Medicine, Sapporo, Japan; **Cedars-Sinai Medical Center, Los Angeles, California; ††University of Washington, Seattle, Washington; ‡‡University of Michigan Health Systems, Ann Arbor, Michigan; §§INVIA Medical Imaging Solutions, Ann Arbor, Michigan; ||||Department of Nuclear Medicine, Technical University, Munich, Germany; ¶¶Advanced Analytics LLC, Gaithersburg, Maryland; ##National Cardiac PET Center, University of Ottawa Heart Institute, Ottawa, Ontario, Canada; ***University College London, London, United Kingdom; and †††Cardiovascular Imaging Technologies, Kansas City, Missouri. This study was conducted within the Finnish Centre of Excellence in Cardiovascular and Metabolic Diseases supported by the Academy of Finland, University of Turku, Turku University Hospital, and Åbo Akademi University; and was supported in part by grants from the Japanese Ministry of Education, Science and Culture (No. 1959135), Northern Advancement Center for Science & Technology (H23-S2-17), and the U.S. National Institutes of Health grant K25-HL086713. Cedars-Sinai receives royalties from the licensing of QPET software, a minority of which is shared with developers, including Drs. Slomka and Germano. Dr. Slomka has received grant support from Siemens Healthcare. Dr. Alessio has received a research grant from GE Healthcare; and has served as a consultant for Lantheus Medical Imaging. Dr. Ficaro has received revenue shares from the sale of Corridor4DM and is the owner of INVIA Medical Imaging Solutions. Dr. Lee has received financial support from and is an employee of INVIA Medical Imaging Solutions. Drs. deKemp and Klein have received revenue shares from the sale of FlowQuant; and have

ABBREVIATIONS AND ACRONYMS

CAD = coronary artery disease

ICC = intraclass correlation

LV = left ventricle

MBF = myocardial blood flow

MFR = myocardial flow reserve

RCA = right coronary artery

SP = software package

TCM = tissue compartment model easuring myocardial blood flow (MBF) in absolute terms with positron emission tomography (PET) is now possible in clinical routine practice (1). These measurements at rest and under stress can be completed quickly (2,3), and the reconstructed dynamic images can be analyzed in a few minutes by the majority of the available software packages (SPs) (4). The analysis produces left ventricle (LV) absolute MBF values measured in ml/min/g at rest and under stress as well as the myocardial flow reserve (MFR)—the ratio of

stress to rest MBF expressed as a unitless number. These values provide unique information regarding diagnosis and monitoring of coronary artery disease (CAD), microvascular health (5), multivessel CAD (6), and risk stratification (7). Although recent studies have shown the diagnostic and prognostic value of MBF quantification over the standard relative image analysis (6,8,9), and use of the generator-produced rubidium-82 (82Rb) (10,11) has brought MBF quantification closer to the clinic, its integration into clinical routine practice remains underutilized (5).

SEE PAGE 1128

To convert imaging data to quantitative MBF parameters, measured radioactivity concentration values need to be transformed into milliliters of blood per minute per gram of myocardial tissue (ml/min/g) by applying tracer kinetic modeling to dynamic PET images. Thus, any numerical value that any professional receives from 82Rb PET is a result of this transformation. At least 8 different models have been proposed (12-19) for 82Rb. Although deKemp et al. (20) and Tahari et al. (21) had addressed the reproducibility of 82Rb PET analysis methods for MBF quantification, they had focused on a limited number of methods; therefore, a comprehensive comparison study was needed to analyze the current situation in 82Rb PET quantification to help establish common and robust methods to support collaborative multicenter clinical trials.

The objective of the RUBY project was to compare all currently available SPs that can analyze $^{82}\mathrm{Rb}$ PET

MBF studies. The criteria for inclusion were the presence of the software in the peer-reviewed literature (16,18,19,22-26) and the willingness of the development team to collaborate according to same ground rules, including blind analysis of the same selected patient datasets. For further details on the 10 compared SPs, please see Table 1 and "The Evaluated Software Packages" section in the Online Appendix; for the side-by-side comparison of the packages, see Table 1 in Saraste et al. (4).

METHODS

IMAGE ACQUISITION. All 82Rb PET studies were performed at the Department of Nuclear Medicine of the University Hospital of Lausanne (Switzerland), according to the routine clinical practice. The study protocol was approved by the local ethics committee. Written informed consent was obtained from each patient prior to the study. Forty-eight patients with suspected or known CAD underwent rest and adenosine-induced stress ⁸²Rb PET. Patients were studied after an overnight fast and were instructed to refrain from caffeine- or theophyllinecontaining products or medications for 24 h before the ⁸²Rb PET study. During the study, patients were instructed to breathe normally. For further details about the PET image acquisition, please see the Online Appendix.

IMAGE ANALYSIS. The reconstructed rest and stress images were delivered to 10 facilities located in 10 centers across 7 countries. Each investigator used 1 SP and, by the rules of this project, had been blinded to results of the image analysis of the other readers before sharing his or her results (see the Online Appendix for details of the study design).

In general, all of the 10 packages implemented variations of a 1-tissue compartment model (TCM) (27). A total of 7 packages implemented by the Ottawa Heart Institute 1-TCM model (OHI-1-TCM) (14). An eighth package also used this model; however, it used a shorter 2.5-min dynamic sequence (8×12s, 2×27s) interpolated from the original image data. Additionally, 1 SP implemented an axially-distributed blood flow model (18)—AD_Ref18, and another used a 2-TCM

served as consultants to and received revenue shares from Jubilant-DraxImage. Dr. deKemp has received royalties from technologies licensed to Jubilant DraxImage and INVIA Medical Imaging Solutions. Drs. Case and Bateman are owners of Cardio-vascular Imaging Technologies, which licenses and sells ImagenQ. Dr. Bateman has served on the advisory board of Lantheus Medical Imaging, GE, and FluoroPharma. Dr. Knuuti has served as a consultant to Lantheus Medical Imaging. All other authors have reported that they have no relationships relevant to the contents of this paper to disclose. Drs. Nesterov and Deshayes contributed equally to this work as first authors. Drs. Prior and Knuuti contributed equally to this work as senior authors.

Download English Version:

https://daneshyari.com/en/article/5980365

Download Persian Version:

https://daneshyari.com/article/5980365

<u>Daneshyari.com</u>