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NeuroImage xxx (2015) xxx-xxx



Contents lists available at ScienceDirect

NeuroImage





journal homepage: www.elsevier.com/locate/ynimg

QI A perspective on the future role of brain pet imaging in exercise science

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6 ARTICLE INFO

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7	Article history:
8	Accepted 8 October 2015
9	Available online xxxx
10	Keywords:
11	Exercise
12	Physical exercise
13	Neuroprotection
14	Brain plasticity
15	Positron emission tomography
16	PET
17	Cerebral metabolism
18	FDG
19	Neuroreceptor
20	Neurotransmission
21	Ligand
22	Ligand activation
23	PET/MR

ABSTRACT

Positron Emission Tomography (PET) bears a unique potential for examining the effects of physical exercise 24 (acute or chronic) within the central nervous system in vivo, including cerebral metabolism, neuroreceptor oc- 25 cupancy, and neurotransmission. However, application of Neuro-PET in human exercise science is as yet surpris- 26 ingly sparse. To date the field has been dominated by non-invasive neuroelectrical techniques (EEG, MEG) and 27 structural/functional magnetic resonance imaging (sMRI/fMRI). Despite PET having certain inherent disadvan-28 tages, in particular radiation exposure and high costs limiting applicability at large scale, certain research ques- 29 tions in human exercise science can exclusively be addressed with PET: The "metabolic trapping" properties of 30 ¹⁸F-FDG PET as the most commonly used PET-tracer allow examining the neuronal mechanisms underlying var- 31 ious forms of acute exercise in a rather unconstrained manner, i.e. under realistic training scenarios outside the 32 scanner environment. Beyond acute effects, ¹⁸F-FDG PET measurements under resting conditions have a strong 33 prospective for unraveling the influence of regular physical activity on neuronal integrity and potentially neuro- 34 protective mechanisms in vivo, which is of special interest for aging and dementia research. Quantification of ce- 35 rebral glucose metabolism may allow determining the metabolic effects of exercise interventions in the entire 36 human brain and relating the regional cerebral rate of glucose metabolism (rCMRglc) with behavioral, neuropsy-37 chological, and physiological measures. Apart from FDG-PET, particularly interesting applications comprise PET 38 ligand studies that focus on dopaminergic and opioidergic neurotransmission, both key transmitter systems for 39 exercise-related psychophysiological effects, including mood changes, reward processing, antinociception, and 40 in its most extreme form 'exercise dependence'. PET ligand displacement approaches even allow quantifying spe-41 cific endogenous neurotransmitter release under acute exercise interventions, to which modern PET/MR hybrid 42 technology will be additionally fruitful. Experimental studies exploiting the unprecedented multimodal imaging 43 capacities of PET/MR in human exercise sciences are as yet pending. 44

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4850 Introduction

45 40

Regular physical exercise is associated with clear health benefits, not 51 only the cardiovascular improvements promoting 'physical health', but 52also central nervous system (CNS) effects believed to promote 'brain 53health' (Boecker et al., 2012). Physical activity can induce acute and 5455sustained psychophysiological effects, including mood changes (Boecker et al., 2008; Brene et al., 2007), hypoalgesia (Scheef et al., Q3 2012), stress reduction and anxiolysis (DeBoer et al., 2012). At the cog-5758nitive level, being by far the most intensively studied domain using exercise, improvements have been observed in hippocampus-dependent 59spatial and associative learning (Barak et al., 2014; Herting and Nagel, 60 61 2013); memory encoding/consolidation (Roig et al., 2013); as well as 62frontal lobe dependent functions such as selective attention, planning

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http://dx.doi.org/10.1016/j.neuroimage.2015.10.021 1053-8119/© 2015 Published by Elsevier Inc. and scheduling, inhibition of prepotent responses, task switching, and 63 working memory capacity (Guiney and Machado, 2013; Ratey and 64 Loehr, 2011). 65

While the impact of physical activity and aerobic fitness on child- 66 hood cognitive functions has only recently gained attention (Khan 67 and Hillman, 2014), there is a large body of literature in older adults 68 suggesting that exercise promotes neuroprotective mechanisms and as- 69 sociated plasticity of brain structure and function, counteracting age-70 related changes (Yau et al., 2014). On the other hand, physical inactivity 71 (i.e. sedentary behavior) increases the risk for developing chronic 72 disease conditions across the lifespan, in particular within the cardio/73 neurovascular spectrum. Despite considerable progress in unveiling 74 the underlying neurobiological mechanisms by which exercise 75 mediates neuroprotective mechanisms and improves cognitive 76 functioning, including neurotrophic factor release (Gomez-Pinilla, 77 2008; Vaynman and Gomez-Pinilla, 2006; Vaynman et al., 2004), 78 neurogenesis/angiogenesis (van Praag, 2008), and neuroplasticity 79 (Cotman and Berchtold, 2002), the central mechanisms mediating re- 80 ward and pleasure in athletes remain far less well understood. More- 81 over, the mechanisms necessary for initiating and maintaining a 82

Please cite this article as: Boecker, H., Drzezga, A., A perspective on the future role of brain pet imaging in exercise science, NeuroImage (2015), http://dx.doi.org/10.1016/j.neuroimage.2015.10.021

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physically active lifestyle are still not understood, despite evidence for
heritability (Bray et al., 2009; Kelly and Pomp, 2013; Stubbe et al., 2006).

Animal research has contributed most to the improved understand-85 86 ing of exercise-induced CNS effects at behavioral (e.g. water maze-type tests), cellular (e.g. neurogenesis, neuroangiogenesis), and humoral 87 (e.g. neurotrophic factors, inflammatory cytokines) levels (Hotting 88 and Roder, 2013; van Praag, 2009; Vivar et al., 2013). For obvious rea-89 90 sons, the majority of the human studies in exercise research have 91 been limited to behavioral measures, as well as indirect assessments 92 of neurotrophic factors and neurotransmitters in blood. Today, different 93 functional neuroimaging techniques allow for the direct investigation of acute and chronic effects of physical exercise in the human brain, as well 94as the correlation of physiological in vivo signals with behavioral out-95comes recorded during and after exercise (Boecker et al., 2012). A 96 wide range of techniques has been applied to human exercise research, 97 ranging from electroencephalography (EEG), magnetoencephalography 98 (MEG), near infrared spectroscopy (NIRS), magnetic resonance imaging 99 (MRI), to positron emission tomography (PET), each method associated 100 with inherent differences in spatial and temporal resolution, availabili-101 ty, cost, and risks. It appears that the field of neuroimaging has an un-102precedented potential to unravel the neurobiology of human exercise, 103 covering a wide spectrum from structural plasticity in gray and white 104 105 matter, evoked neuronal responses, neuronal network dynamics, global and regional perfusion and metabolism, receptor binding studies and 106 107 neurotransmitter release.

In this 'perspective paper', we focus on the distinct, but as yet emerg-108 ing role of PET for studying exercise-induced functional changes in the 109110 human brain. So far, only a few PET studies have been published in exercise research. This shortage of research is difficult to retrace, as Neuro-111 PET is a 'gold standard' for quantifying cerebral metabolism and recep-112 tor binding in vivo. This 'perspective paper' emphasizes the current, but 113 114 more importantly, the potential future role of PET in the fields of meta-115bolic imaging, delayed metabolic imaging ('FDG activation studies'), neuroreceptor PET, PET ligand activations, and multimodal PET/MR, Be-116 yond acute physiological effects, the potential role of PET in examining 117 long-term neuro-preventive and restorative effects of exercise in clini-118 cal conditions is discussed, in particular in the eminent context of neu-119 120 rodegenerative diseases.

121 Brain pet measurements of glucose metabolism in

122 exercise physiology

123 Background, methodology and current applications of ¹⁸F-FDG brain PET

¹⁸F-fluoro-deoxy-glucose (¹⁸F-FDG) PET allows the measurement 124 and quantification of the regional cerebral rate of glucose metabolism 125126(rCMRglc). ¹⁸F-FDG uptake is directly proportional to regional neuronal activity (Kennedy et al., 1975). ¹⁸F-FDG PET measurements of rCMRglc 127can be conducted within different experimental settings for studying 128the mechanisms and consequences of movement and physical exercise; 129for a review of ¹⁸F-FDG PET studies in sports sciences please also see: 130131 (Tashiro et al., 2008). Studies have, for example, investigated (Sakurai et al., 2014)¹⁸F-FDG brain uptake during the performance of different 132movement types or exercise training, i.e. quantifying acute exercise-133dependent rCMRglc changes in the CNS. This is possible as ¹⁸F-FDG is 134trapped in the brain during an initial uptake phase of 10-30 minutes 135136 post injection. Consequently, the tracer can be applied during defined test conditions and the resulting changes in cerebral glucose metabo-137 lism can be measured subsequently, i.e. with temporal delay. This prin-138 cipally allows the visualization of "brain metabolic signatures" 139associated with different forms of exercise. Importantly, these 'metabol-140 ic trapping' properties make it possible to inject ¹⁸F-FDG even in realistic 141 sport settings outside the PET scanner, i.e. without the obvious con-142 straints of the imaging setup (as it is the case, e.g. in functional MRI-143 studies). Also to be considered are defined control conditions (including 144 145 'active control conditions' in identical environments), as these provide means for experimentally controlling unspecific (not exercise related)146effects. It needs to be mentioned, however, that such an experimental147approach will reflect a mean image of brain activation/deactivation dur-148ing the tracer uptake phase, i.e. the results cannot be compared to clas-149sical brain activation studies which aim for the isolated localization of150brain regions specifically activated by processing of a dedicated task.151

¹⁸F-FDG PET was hitherto employed for direct assessments of brain 152 metabolism during unaccustomed treadmill walking, i.e. by comparing 153 rest and 25 min of treadmill walking (Shimada et al., 2013). ¹⁸F-FDG 154 PET revealed relative metabolic increases during treadmill walking in 155 the primary sensorimotor areas, occipital lobe, and anterior and posteri- 156 or lobe of the cerebellum (Shimada et al., 2013). Further division into 157 low and high step-length variability groups (based on step length re- 158 cordings), allowed these researchers to relate walking-induced rCMRglc 159 changes with parameters of gait. Activation of the primary sensorimotor 160 cortex, prefrontal cortex, and temporal lobe were associated with gait 161 adaptability during unaccustomed treadmill walking (Shimada et al., 162 2013). In another study, ¹⁸F-FDG was injected while subjects either 163 walked or purely imagined walking. Both, real and imagined locomo- 164 tion activated a "basic locomotion network", including frontal cortex, 165 cerebellum, ponto-mesencephalic tegmentum, parahippocampal, fusi- 166 form and occipital gyri; whereas the multisensory vestibular cortices 167 were deactivated. Differential activity was identified in primary motor 168 and somatosensory cortices for real steady-state locomotion, whereas 169 imagined modulatory locomotion was associated with relatively elevat- 170 ed metabolism in the supplementary motor cortex and basal ganglia (la 171 Fougere et al., 2010). Two recent studies by Kindred et al. have also used 172 ¹⁸F-FDG PET to integrate brain and muscle responses during task perfor- 173 mance: relatively higher ¹⁸F-FDG uptake was found during a position 174 task than during a force task in occipital and temporal cortices, possibly 175 reflecting enhanced processing of visuospatial feedback (Kindred et al., 176 2015a). In another study (Kindred et al., 2015b), eight healthy controls 177 performed 15 min of treadmill walking at a self-selected pace, during 178 which ¹⁸F-FDG was injected. In several task-related brain areas, they 179 found "strong to moderate correlations" between ¹⁸F-FDG uptake and 180 walking speed; the ¹⁸F-FDG uptake was altered in eight patients with 181 multiple sclerosis (Kindred et al., 2015b). 182

Exercise training was also investigated using this approach: Tashiro 183 et al. examined rCMRglc changes in 17 healthy male volunteers induced 184 by free running in upright posture (Tashiro et al., 2001). Participants 185 were divided randomly into two groups, either performing a 4-5 km 186 run, or simply resting. Running augmented energy consumption partic- 187 ularly in the parieto-occipital region that was interpreted as being due 188 to relatively higher energy costs for integrating multimodal sensory in- 189 formation during running rather than for generating motor output. Rel- 190 ative increases of glucose uptake during running were also found in 191 temporo-parietal association cortex, occipital cortex, premotor cortex 192 and cerebellar vermis. As to be expected, activity in the primary senso- 193 rimotor cortex was highest in the 'leg motor area'. Another study 194 (Kemppainen et al., 2005) assessed how 'high intensity exercise' affects 195 regional and global brain glucose uptake. Scans were acquired in 14 196 male volunteers after 35 min of bicycle exercise (intensities correspond-197 ing to 30, 55 and 75%) with ¹⁸F-FDG being injected 10 min after the start 198 of the exercise. Kemppainen et al. observed that glucose uptake de- 199 creased as exercise intensity increased, the mean decrease from the 200 lowest to the highest exercise intensity being 32% globally 201 (Kemppainen et al., 2005). Interestingly, brain glucose uptake correlat- 202 ed inversely with the measured lactate accumulation during exercise 203 (Kemppainen et al., 2005). 204

These data indicate that by using the "metabolic trapping" proper-205 ties of ¹⁸F-FDG PET, deeper insights can be gained into the mechanisms 206 of different kinds of movement; moreover, the potential to correlate 207 rCMRglc with parameters of locomotion, endurance exercise, and even 208 neuropsychological effects bears an enormous potential; similar studies 209 can also be conducted using delayed single photon emission computed 210 tomography (SPECT) perfusion imaging, although at typically lower 211

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