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Neural architecture underlying classification of face perception paradigms

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Introduction

ABSTRACT

We present a novel strategy for deriving a classification system of functional neuroimaging paradigms that 25 relies on hierarchical clustering of experiments archived in the BrainMap database. The goal of our proof-of-26 concept application was to examine the underlying neural architecture of the face perception literature 27 from a meta-analytic perspective, as these studies include a wide range of tasks. Task-based results 28 exhibiting similar activation patterns were grouped as similar, while tasks activating different brain net-29 works were classified as functionally distinct. We identified four sub-classes of face tasks: (1) Visuospatial 30 Attention and Visuomotor Coordination to Faces, (2) Perception and Recognition of Faces, (3) Social 31 Processing and Episodic Recall of Faces, and (4) Face Naming and Lexical Retrieval. Interpretation of these 32 sub-classes supports an extension of a well-known model of face perception to include a core system for 33 visual analysis and extended systems for personal information, emotion, and salience processing. Overall, 34 these results demonstrate that a large-scale data mining approach can inform the evolution of theoretical 35 cognitive models by probing the range of behavioral manipulations across experimental tasks.

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43 As more resources are being developed and deployed for the management, sharing, and meta-analysis of "big data" in neuroimaging, 44 the development of knowledge representation systems has likewise 45accelerated to enable objective and succinct descriptions of these 4647data, including neurotechnological, neuroanatomical, and cognitive parameters. However, cognitive data descriptors are relatively under-48 developed compared to those from the neurotechnological and 49 50neuroanatomical domains. That is, as a community we are relatively more confident regarding data annotations differentiating sub-class 51 or type of MRI scan (e.g., T2* or EPI images) or brain structure 5253(e.g., hippocampus or amygdala) than in differentiating data that re-54lates to memory (e.g., episodic or working). Nevertheless, semantic

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http://dx.doi.org/10.1016/j.neuroimage.2015.06.044 1053-8119/© 2015 Published by Elsevier Inc. representation of cognitive and perceptual mental processes is a neces- 55 sary component of large-scale, community-wide, and consensus-based 56 mapping of structure-function correspondences in the human brain. 57 Such a representation must include the full and robust definitions of 58 mental processes; however, the identification and standardization of 59 terms we use to describe the multitude and diversity of cognitive and 60 perceptual functions is an inexact science. As a result, many alternative 61 and often competitive terminologies exist. With the rise of high profile, 62 high-impact projects such as the Human Connectome Project (Van 63 Essen et al., 2013; Toga et al., 2012), the BRAIN Initiative (BRAIN 64 Working Group, 2014), the Human Brain Project (Markram, 2012), 65 and the RDoCs framework (Insel et al., 2010), the need for knowledge 66 representations of cognitive aspects of neuroscience data has reached 67 a critical point. Our community goal of mapping the human brain 68 will surely require definition and standardization of the terms that 69 are used to describe human thought and mental processes, as well as 70 the behavioral tasks used to elicit them during neuroscience 71 experiments. 72

Here, we propose and validate a strategy for deriving a classification 73 system of functional neuroimaging paradigms using a proof-of-concept 74

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application. Our aim was to develop a meta-analytic data mining 75 76 approach for paradigm classification based on neurobiological evidence 77 provided by functional activation patterns, with the intent that such 78 a strategy may mitigate the challenges associated with a lack of paradigm-related semantic consensus within a given domain. The 79 overall premise of this work is that differences in activation patterns 80 across studies should be captured and leveraged as they indicate 81 meaningful segregations in brain function. Under this premise, tasks 82 83 activating similar brain networks should be grouped as functionally 84 similar in a cognitive schema, while tasks demonstrating differential 85 activation patterns should be classified as functionally distinct.

As an exemplar domain, we demonstrate our approach in the 86 context of face discrimination, as this category of neuroimaging tasks 87 88 is highly heterogeneous and commonly employed across numerous perceptual, cognitive, and affective studies in both healthy and diseased 89 populations. These studies broadly include visual stimulus presentation 90 of human faces in which participants passively view faces or actively 91 92discriminate one or more aspects or features of face presentation (e.g., old/new, male/female, and happy/sad/angry/fearful). Faces can 93 be used as stimuli for classical conditioning, lip-reading, and naming 94 tasks, or to cue autobiographical memory retrieval, emotion induction, 95 or social processing. Given the wide scope of face tasks in the literature, 96 97 our aim was to establish a neuroinformatics procedure capable of objectively decomposing the collective group into meaningful sub-categories. 98 Using meta-analytic data reported across a diverse range of studies 99 archived in the BrainMap database, we sought to determine if multiple 100 functional networks distributed across the brain are differentially 101 102recruited for various task paradigms. Our ultimate goal was threefold: to develop a paradigm classification strategy for use by cognitive ontol-103 ogies, to examine the underlying neural architecture of face perception 104 from a meta-analytic perspective, and, more broadly, to assess whether 105106 an evidence-based data mining approach can inform the evolution of existing cognitive models. 107

108 Methods

109 Meta-analytic data extraction and pre-processing

The BrainMap database (Fox and Lancaster, 2002; Laird et al., 2005a, 110 2011a) currently archives brain activation locations from over 11,900 111 functional magnetic resonance imaging (fMRI) or positron emission 112 tomography (PET) experiments (from over 2,400 journal articles). 113 These experiments have been manually annotated with metadata that 114 describe the experimental design of each archived study. Our study 115 focused on a subset of tasks within BrainMap that were annotated 116 with the paradigm class of "Face Monitor or Discrimination"; the 117 118 relevant experiments were identified and downloaded for further analysis using the desktop search engine application, BrainMap Sleuth 119(http://www.brainmap.org/sleuth). Search results were filtered to in-120clude only face tasks performed by healthy adults to limit any potential 121bias due to effects of age, disease, or treatment differences. Information 122123about the specific behavioral task performed by participants in each 124experiment, along with the experiment name, sample size, and stereotaxic coordinates of activation were exported as a tab-delimited text 125file. Exported coordinates reported in MNI space (Evans et al., 1993; 126Collins et al., 1994) were transformed to Talairach space (Talairach 127128and Tournoux, 1988) using the Lancaster transform function icbm2tal (Lancaster et al., 2007). icbm2tal was developed using global affine 129transforms to accommodate spatial disparity between Talairach and 130MNI coordinates as compared to the earlier mni2tal transform (Brett 131 et al., 2001), and to minimize meta-analytic spatial dissonance due to 132template differences (Laird et al., 2010). Modeled activation (MA) 133 maps were generated by modeling each coordinate of activation as a 134spherical Gaussian distribution of uncertainty to represent the probabil-135ity of activation for each voxel, centered upon the experiment's activa-136 137 tion foci (Fig. 1, Step 1). The algorithm includes an estimation of the inter-subject and inter-laboratory variability associated with each 138 experiment, and is weighted by the number of subjects included in 139 each experiment (Eickhoff et al., 2009). The per-experiment MA proba-140 bility maps were converted into feature vectors of voxel values and 141 concatenated horizontally to form an array of size *n* experiments by 142 *p* voxels. 143

Correlation matrix based hierarchical clustering analysis

After generating the $n \ge p$ matrix of MA probability maps, we 145 employed a pairwise correlation analysis in which correlation coeffi- 146 cients were calculated for each *n* experiment compared to every other 147 n experiment, to assess similarity of spatial topography across MA 148 maps. Hence, the *n* X *p* array of MA maps was transformed into an *n* X 149 n correlation matrix that captured the similarity of whole-brain 150 modeled activation images across face discrimination experiments 151 (Fig. 1, Step 2). Experiments within the *n* X *n* correlation matrix were 152 subsequently grouped into clusters using hierarchical clustering analy- 153 sis, an agglomerative unsupervised classifier (Fig. 1, Step 3). Previous 154 implementation of correlation matrix based hierarchical clustering of 155 resting state fMRI data (Liu et al., 2012; Keilholz et al., 2010) and hierar- 156 chical clustering of BrainMap-based meta-analytic images (Laird et al., 157 2011b) demonstrated optimal clustering using the average linkage algo- 158 rithm and 1 - r as the distance between clusters, where r is the 159 Pearson's correlation coefficient. Following initial testing for optimal 160 performance, these parameters were adopted in the present study. 161 Notably, Pearson's correlation distance maximizes the effects of direc- 162 tion, rather than magnitude, of the two observational vectors, thus 163 identifying correlated MA maps as being topologically similar and 164 anti-correlated MA maps as dissimilar. 165

The resultant dendrogram was examined to identify sets of experiments that clustered together. Selecting a clustering solution yielding an optimal parcellation of BrainMap experiments relied on two measures. The cophenetic distance between clusters at a specific model order (i.e., number of clusters) describes the dissimilarity between sub-clusters, and is intrinsically higher at low model orders (e.g., a two-cluster solution). Importantly, the relative difference in cophenetic distances when transitioning from model order *x* to the next highest model order x + 1 can be informative when examining if cluster separation results in vastly different solutions. Therefore, we sought to substantially different activation patterns respective to each cluster by maximizing the relative difference, d_c , in cophenetic distances c_x and r_{x+1} , as model order, *x*, increased: 179

$$d_c = \frac{c_{x+1} - c_x}{c_{x+1}}.$$
 (1)

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Related to the above measure of difference in cophenetic distances is the impact that increasing model order has on separating clusters into 182 sub-clusters of proportionate number of variables (e.g., experiments). 183 Increasing the cluster solution could potentially yield a segregation of 184 experiments in which one sub-cluster dominates with a disproportion-185 ately large number of experiments. Therefore, we sought to minimize 186 the effect of cluster segregation by calculating the maximum density 187 of experiment separation. Essentially, we aimed to determine if increas-188 ing model order resulted in a disproportionate divergence of experi-189 ments. For example, if cluster i_0 , consisted of n_0 experiments at model 190 order x, and separated into clusters i_1 and i_2 , with n_1 and n_2 experiments, 191 respectively, then the density of experiment separation, d_s is calculated as: 193

$$d_s = \frac{n_1}{n_0}, n_1 \ge n_2. \tag{2}$$

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