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Q23 Dynamic functional connectivity using state-based dynamic community 2 structure: Method and application to opioid analgesia

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ABSTRACT

We present a new method, State-based dynamic community structure, that detects time-dependent community structure in networks of brain regions. Most analyses of functional connectivity assume that network behavior is 15 static in time, or differs between task conditions with known timing. Our goal is to determine whether brain net- 16 work topology remains stationary over time, or if changes in network organization occur at unknown time 17 points. Changes in network organization may be related to shifts in neurological state, such as those associated 18 with learning, drug uptake or experimental conditions. Using a hidden Markov stochastic block model, we define 19 a time-dependent community structure. We apply this approach to data from a functional magnetic resonance 20 imaging experiment examining how contextual factors influence drug-induced analgesia. Results reveal that net- 21 works involved in pain, working memory, and emotion show distinct profiles of time-varying connectivity. 22 © 2014 Elsevier Inc. All rights reserved. 23

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28 Introduction

The explosion of several new topics in neuroimaging, including 29large-scale resting state studies (Van Dijk et al., 2012; Zuo et al., 2012; 30 Smith et al., 2013), studies of psychopathology (Jafri et al., 2008; 31 Greicius, 2008), and pharmacological functional magnetic resonance 32 imaging (phfMRI) (Schwarz et al., 2007; Honey and Bullmore, 2004) 33 has led to exciting innovations in methods for functional connectivity. 34 Two emerging themes are the need for dynamic connectivity methods 35 36 that allow for changes in connectivity over time, and network models 37 that capture the complex structure of connectivity. In this paper we introduce a new method. State-based dynamic community structure 38 (SDCS), that combines these approaches to identify distinct functional 39 connectivity states with respect to the organization of networks of 40 41brain regions into communities of brain regions. This method is particularly well-suited for experimental contexts in which the timing of 42shifts between states cannot necessarily be specified a priori. 43

A growing body of work (Beckmann et al., 2005; De Luca et al., 2006;
Damoiseaux et al., 2006; Ferrarini et al., 2009; Fair et al., 2009) has suggested that brain functional connectivity networks exhibit complex
structure such that the whole-brain network can be represented as a
collection of subnetworks, where each subnetwork is comprised of a
set of spatially distributed brain regions. Recent work (Bassett et al.,
2011a, 2011b; Bowman et al., 2012; Schwatz et al., 2009; Shen et al.,

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2010), (Meunier et al., 2009) has shown that these subnetworks can 51 be illustrated as "communities" or modules of "nodes". Nodes within a 52 community are highly connected and/or share some properties with re-53 spect to connectivity. Methods that estimate this network structure by 54 partitioning a collection of brain regions into subgroups can provide 55 complementary information to descriptive measures of the global prop-56 erties of the functional connectivity network (Bullmore and Sporns, 57 2009) such as degree distributions (number of connections per node), 58 clustering coefficients, and small world properties (Bullmore and 59 Sporns, 2009; Rubinov and Sporns, 2010; Sporns et al., 2004; Simpson 60 et al., 2013).

Several recent developments in fMRI analysis methods are motivat- 62 ed by the recognition that functional connectivity characteristics are dy- 63 namic, fluctuating over time with changes in mental states and other 64 physiological processes (Hutchison et al., 2013). Recent work has incor- 65 porated temporal dynamics into the varied descriptions of functional 66 connectivity properties, providing a flexible alternative to standard 67 approaches that assume network behavior is static over time, or differs 68 between task conditions with known timing. Changes in network char- 69 acteristics include shifts in the strength of connection between a given 70 pair or group of nodes, the degree distribution or clustering coefficient 71 of the network as a whole, or other global network properties. Dynamic 72 connectivity regression (Cribben et al., 2012) provides a method for de-73 tecting change points in an fMRI time series based on the connectivity 74 graph of a group of selected regions. Dynamics of spatial activation com-75 ponents have been estimated using dynamic ICA (Allen et al., 2012) and 76 dynamic principal components analysis (Leonardi et al., 2013). The 77 characteristics of the functional connectivity network have been 78

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shown to differ according to various task demands (Hutchison et al.,
2013), and psychoactive drug conditions (Greicius, 2008; Boveroux
et al., 2010). Of particular relevance to this paper, the dynamics of the
modular structure of the functional connectivity network have been explored in resting state (Jones et al., 2012), learning (Bassett et al., 2011a,
2011b), and studies of emotion (Kinnison et al., 2012).

Recent developments in techniques for dynamic networks in neuro-85 86 imaging data have occurred alongside new approaches to general 87 dynamic network analysis problems, and in particular, work on dynam-88 ic community structure. Popular approaches include extensions of 89 network partitioning algorithms based on modularity maximization or related "quality functions" to time-dependent networks, often by incor-90 91porating temporal smoothness into the quality function (Mucha et al., 2010; Kawadia and Sreenivasan, 2012; Chakrabarti et al., 2006; Chen 92et al., 2013). Other algorithms are based on incremental updates to esti-93 mates of community structure (Cazabet et al., 2010; Nguyen et al., 94 2011). Applications of Dynamic network models to fMRI data must ad-95 96 dress its particular characteristics, specifically low signal to noise ratio, relative lack of temporal resolution, and the related lack of observable 97 instantaneous, or at least temporally identified, connections (cf EEG or 98 email data). As will be discussed, we pursue an approach based on a sto-99 chastic generative model for network data, rather than an algorithmic 100 101 method, and focus on identifying district states with respect to commu-102 nity structure.

In this paper, we introduce a dynamic network analysis technique, 103 State-based dynamic community structure (SDCS), that identifies dis-104 tinct temporal states with respect to community structure over time 105106 without a priori assumptions on the timing or type of changes in structure. Previous approaches to dynamic connectivity have largely used 107simple measures of connectivity, or have been confined to a small num-108 ber of predefined regions and do not scale up easily to larger networks. 109110 As discussed in Hutchison et al. (2013), the sliding window approaches 111 employed in many dynamic connectivity studies are difficult to interpret and induce spurious fluctuations under stable connectivity condi-112 tions. By contrast, the SCDS approach is able to capture complex 113changes, estimating the temporal and graphical structure of the net-114 work in an integrated manner. We characterize the organization of 115116 the network using the stochastic block model (Nowicki and Snijders, 2001), a statistical model for describing community structure. The 117 goal of this approach is to estimate whether and how this network 118 structure shifts over time in experiments with possible state-related 119 120 changes in psychological activity. A change in the organization of the connectivity network could consist of, for example, a shift from a state 121 in which connectivity is highly modular, *i.e.* connectivity is concentrated 122123 within subnetworks of regions, to a state in which the pattern of connectivity is less modular and more integrated throughout the network. 124

125SDCS identifies state-based changes using a Hidden Markov model, a widely used method for identifying latent properties of time series data. 126Under this framework, we assume that there is an underlying, unob-127served state property associated with the network at each point in 128time, and these states may shift at unknown times. The Hidden Markov 129130model allows us to estimate the properties of the underlying states, and 131 identify where likely shifts between states have occurred. Thus, we can assess whether the functional connectivity network is stationary in time 132with respect to structural organization, or whether there are shifts in 133structure, and identify the distinct structural patterns of the functional 134135connectivity network. State-space models have been used previously in related fMRI problems, including studies of changes in effective con-136 nectivity for EEG/MEG data under a Dynamic Causal Model (Olier et al., 137 2013), and in multivariate state-space models for brain function (Janoos 138 et al., 2013). 139

We apply the SDCS functional connectivity method to fMRI data acquired during a study of opioid- and expectancy-based pain modulation
(Atlas et al., 2012). Our previous paper used voxel-wise event-related
analyses to test whether opioid drug effects on pain-evoked responses
differ as a function of belief (*i.e.* during Open, relative to Hidden,

administration). In the present analysis, we use SDCS to examine the 145 timecourse of connectivity within regions associated with psychological 146 processes thought to underlie placebo effects and pain modulation: pain 147 processing, emotion, and executive function/ working memory (Atlas 148 and Wager, 2013). We build on our previous work by testing whether 149 different networks have different timecourses of connectivity during 150 Open Drug administration, irrespective of task design. Because our 151 task involved changes on the order of minutes (due to the pharmacokinetics of the opioid analgesic) as well as shifts in context (baseline, instructions signaling onset and offset of drug infusion, post-infusion 154 washout period), the present analysis can determine whether distinct 155 functional networks and their within-network organization are differentially influenced by these factors. 157

Methods

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The method for estimating time-dependent functional network 159 structure consists of three stages. First, the total time interval is divided 160 into a series of non-overlapping windows and the functional connectivity network is estimated independently in each window, as described in 162 the section Network representation. Next, a hidden Markov model is fit **Q6** to the sequence of estimated networks to identify possible distinct **Q7** connectivity states and the most likely locations in time of meaningful 165 shifts in community structure. The procedure for identifying connectivity states and the change points between them is described in the 167 section Changes over time. Finally, the estimates of functional connectivity structure for each of the identified states are refined using 169 MCMC. A schematic is shown in Fig. 1.

Network representation

Before estimating dynamic community structure, the brain regions 172 comprising the network and the measure of connectivity must be 173 defined, as well as the time windows on which the SDCS algorithm 174 will operate. In this paper, we focused on connectivity within parcels 175 of multi-voxel regions defined based on *a priori* functional and anatomical boundaries, examined 150-second windows (75 TRs), and used 177 thresholded coherence as a measure of connectivity. We discuss each 178 of these decisions and associated methods in more detail below. Though 179 the application of our method involves making choices about how to define regions and the length of time windows to integrate over, the SDCS 181 method is general and does not depend on particular choices of region 182 definition and time windowing. Different choices will likely be optimal 183 for different applications. 184

In network modeling of fMRI data, we have a choice in the definition 185 of the nodes and edges. Voxels themselves can be used as nodes, as in 186 ICA or seed region analysis, or voxels can be segmented into spatially 187 contiguous groups, which are then treated as nodes in the functional 188 connectivity network. While a single voxel approach has the advantage 189 of introducing fewer assumptions on the network, a higher-level repre-190 sentation of connectivity can provide complementary information 191 about patterns of connectivity which can't be attributed to spatial adja-192 cency. In this work, we were primarily interested in brain networks in- 193 volved in pain processing, working memory, or emotion, as each of 194 these processes has been implicated in expectancy-based pain modula- 195 tion (Atlas and Wager, 2013). We therefore used meta analyses to iden-196 tify brain regions consistently activated by working memory (Wager 197 and Smith, 2003) and emotion (Kober et al., 2008) as well as a mega- 198 analysis of five previous studies of thermal pain to identify regions 199 involved in pain processing (Atlas et al., 2010). We note that meta- 200 analysis and mega-analysis provide ways to pool across previous stud- 201 ies to identify regions that are most likely to be activated by a given pro- 202 cess. Thus they provide a principled way to identify functional networks 203 a priori irrespective of specific experimental details such as fMRI field 204 strength, study population, study location, etc. Details of these methods 205 have been described in detail in previous work (Wager et al., 2007; 206

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