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## Resting state functional connectivity changes induced by prior brain state

### <sup>2</sup> are not network specific

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#### ABSTRACT

Resting state functional connectivity (rFC) is used to identify functionally related brain areas without requiring subjects to perform specific tasks. Previous work suggests that prior brain state, as determined by the activity en- 18 gaged in immediately prior to collection of resting state data, can influence the networks recovered by rFC 19 analyses. 20

We determined the prevalence and network specificity of rFC changes induced by manipulations of prior state 21 (including an unstructured (unconstrained) state, and language and motor tasks). Three blocks of rest data 22 (one after each of the specified prior states) were acquired on each of 25 subjects. We hypothesised that prior 23 state induced changes in rFC would be greatest within the networks most actively recruited by that prior state. 24 Changes in rFC were greatest following the motor task and, contrary to our hypothesis, were not network specific. 25 This was demonstrated by comparing (1) the timecourses within a set of ROIs selected on the basis of task- 26 related de/activation, and (2) seed-based whole brain voxel-wise connectivity maps, seeded from local maxima 27 in the task-related de/activation maps. Changes in connectivity strength tended to manifest as increases in rFC 28 relative to that in the unstructured rest state, with change maps resembling partially complete maps of the 29 primary sensory cortices and the cognitive control network. The majority of rFC changes occurred in areas mod- 30 erately (but not weakly) connected to the seeds. Constrained prior states were associated with lower across- 31 participant variance in rFC. 32

This systematic investigation of the effect of prior brain state on rFC indicates that the rFC changes induced by 33 prior brain state occur both in brain networks related to that brain activity *and* in networks nominally unrelated 34 to that brain activity. 35

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#### 41 Introduction

Resting state functional connectivity (rFC) has assumed a prominent position in the investigation of large scale neural networks in the human brain (Bandettini, 2009; Fox and Raichle, 2007; Greicius, 2008; van den Heuvel and Pol, 2010; Zuo et al., 2010). The networks revealed by rFC resemble those identified via task-related activation studies (Biswal et al., 1995). Further, rFC analyses are appealing as the data are comparatively easily acquired, and they can be performed even in clinical populations in whom task execution is compromised.

It is now apparent that rFC maps are not fixed, stable entities but rather exhibit variation across a variety of timescales, from seconds to

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http://dx.doi.org/10.1016/j.neuroimage.2014.11.037 1053-8119/© 2014 Published by Elsevier Inc. minutes to days (Chang and Glover, 2010; Guo et al., 2012; Hasson 52 et al., 2009; Kang et al., 2011; Mannfolk et al., 2011; Shehzad et al., 53 2009; Soares et al., 2013; Stevens et al., 2010; Wang et al., 2012; Zuo 54 et al., 2010). In the present study we focus on rFC changes occurring 55 over periods of minutes. Prior studies examining changes in connectivity at this time scale have compared rFC before and after some manipufit ation, such as execution of a motor task (Duff et al., 2008; Peltier et al., 58 2005), or a cognitive task such as language (Waites et al., 2005) or **Q4** working memory task (Gordon et al., 2014). Such studies converge on 60 evidence that prior brain state can influence subsequent rFC, with the 61 changes hypothesised to reflect factors such as fatigue (Esposito et al., 62 2014; Peltier et al., 2005), changes in cognitive set (Waites et al., 63 2005) and/or learning/consolidation (Gordon et al., 2014).

The potential influence of prior brain state on rs-fcMRI has impor- 65 tant ramifications for group studies. Many research centres uniformly 66 collect rest data across otherwise different experimental protocols, 67 and there is a strong attraction to pool such data in order to increase 68 power. The potential bias introduced by such pooling could also influ- 69 ence analyses based upon large, multicentre data sharing initiatives, 70

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such as the 1000 Functional Connectomes Project (www.nitrc.org/
 projects/fcon\_1000/).

These hypothesised mechanisms by which prior brain state influ-73 74 ences rFC, outlined above, suggest that any rFC changes should be network specific. For instance, if fatigue lies behind the rFC changes 7576observed following a finger movement task (Peltier et al., 2005), then 77 one might hypothesise that such changes are restricted to the motor 78system. The question of the specificity of these effects remains unclear. 79Gordon et al. (2014) examined connectivity within and between the 80 task positive network (TPN) and the default mode network (DMN) 81 immediately before and after execution of a working memory task. They observed alterations of rFC both within the TPN, and between the 82 TPN and DMN. This result is similar to the earlier work of Grigg and 83 84 Grady (2010), who showed variable connectivity from precuneus (in the DMN) to a set of brain regions resembling the TPN and primary 85 sensory cortices when comparing rest data before and after a period of 86 87 task execution. These data suggest that both intra- and inter-network changes in rFC can be induced by prior brain state. However compari-88 sons relative to the DMN may constitute a special case of inter-89 network change as the DMN has frequently been conceptualised as 90 diametrically opposed to other brain networks, particularly the TPN. 91

92Here we address the question of the network specificity of rFC 93 changes induced by immediately prior brain state using a novel experi-94 mental design. We collected three sets of rest data: an initial rest period acquired upon entering the scanner, a second rest period following ex-95ecution of an in-scanner language task, and a third rest period following 96 execution of an in-scanner motor task (with order of the language and 97 98 motor tasks counter-balanced). For each rest block we calculated seeded rFC analyses, with seeds located in the language network, the motor 99 network, and the default mode network. This design enabled us to eval-100 uate two hypotheses: (1) that systematic variation of prior brain state 101 102results in systematic group level alterations in rFC; and (2) that alter-103ations in rFC induced by prior brain state exhibit network specificity.

#### 104 Material and methods

#### 105 Participants

106Twenty-five healthy volunteers participated in the study (17 male;107age, mean  $\pm$  SD: 24.6  $\pm$  5.5 years, range: 17–40). All protocols were approved by the relevant institutional Human Research Ethics Committee.

#### 109 In-scanner procedures and cognitive activation paradigms

Subjects were scanned continuously for 450 volumes, alternating 110 between periods of "extended rest" (90 volumes) and block design 111 112 "task" periods (90 volumes) according to the following sequence: rest1, task1, rest2, task2, and rest3. During the extended rest periods, 113 subjects viewed a black screen and were instructed to stay awake 114 with eyes open, and refrain from any overt or covert cognitive or 115motor activities. During the task periods, subjects performed one of 116 117 two block design tasks: a language task - Orthographic Lexical Retrieval 118 (OLR), and a motor task – finger tapping (MOTOR); task order was counter-balanced across subjects. Both block design tasks alternated be-119tween 10 TRs of active phase and 10 TRs of baseline phase, completing 120four active phases embedded within five baseline phases. During the 121122baseline phases of both tasks, subjects viewed a black screen with a white cross ("+") at the centre, and were instructed to relax. During 123the active phase of the OLR task (Wood et al., 2001), a covert adaptation 124of the Controlled Oral Word Association Test (Strauss et al., 2006), a let-125ter was displayed at the centre of the screen, and then after five TRs an-126other letter was presented. Participants were instructed to think of as 127 many words as possible beginning with the current letter, but to avoid 128using proper nouns or numbers, repeating words or adding a suffix to 129a previously retrieved word. During the active phase of the MOTOR 130131 task, the word "Move" was presented at the centre of the screen, and subjects were required to tap their left index finger in time with a1321.0 Hz metronome played to them over headphones. The metronome133was also played throughout the baseline period of the MOTOR task, dur-134ing which the words "Don't Move" were presented.135

We refer to the resting state data collected during the initial period136as unstructured, and that collected after the OLR and MOTOR tasks as137post-OLR and post-MOTOR, respectively. Unstructured refers to the fact138that, relative to the post-OLR and post-MOTOR rest periods, the prior139brain state in the unstructured rest is not as tightly constrained across140participants.141

#### Image acquisition

The fMRI studies were carried out with a 3 T GE Signa LX whole body 143 scanner (General Electric, Milwaukee, WI), using a standard birdcage 144 quadrature head coil. Functional images were acquired as a series of 145 gradient-recalled echo planar imaging (GR-EPI) volumes (TE = 40 ms). 146 Images for the first 13 participants were acquired using a TR of 3.6 s at 147 a voxel resolution of 1.95 mm  $\times$  1.95 mm  $\times$  (4 mm thick +1 mm gap) 148 (25 oblique slices); images for the final 12 participants were acquired 149 using a TR of 3.2 s at a voxel resolution of 3.44 mm  $\times$  3.44 mm 150 (3.2 mm thick +0.2 mm gap) (40 oblique slices). The data from the 151 two different scanners therefore contained the same number of image 152 volumes, corresponding to slightly different total experiment durations. 153 Due to a technical error the initial rest period for one participant 154 contained 50 rather than 90 volumes.

Image processing

The collected images were pre-processed using Statistical Parametric Mapping software (SPM8 release 4667; Wellcome Department of 158 Imaging Neuroscience, London, UK) with the aid of the iBrain<sup>TM</sup> analysis 159 toolbox for SPM (Abbott et al., 2011) and iBrain<sup>TM</sup> (Abbott and Jackson, 160 2001). Images were first slice-time corrected, realigned, then spatially 161 normalised to an in-house EPI template (constructed from 30 healthy 162 control brains not including the present participants, as described in detail in Waites et al. (2005)) that approximates the SPM standard space 164 (Montreal Neurological Institute). Normalised images were written 165 out at  $2 \times 2 \times 2$  mm resolution, then smoothed with an isotropic 166 Gaussian kernel (full-width-at-half-maximum = 8 mm). 167

#### Analysis of activation paradigms

Statistical analysis of the functional imaging data was conducted in 169 SPM8 with the aid of the iBrain<sup>™</sup> analysis toolbox for SPM using a gen- 170 eral linear model. Standard single subject analyses were conducted on 171 each participant's OLR and MOTOR tasks. The BOLD response of the 172 task compared to baseline state was modelled assuming the SPM canon-173 ical hemodynamic response function (HRF), and comprised the effect of 174 interest. In addition, the six rigid body transformation parameters esti- 175 mated during image realignment were included in the model as effects 176 of no interest. Prior to estimation, the fMRI data and design matrix were 177 high-pass filtered (cut-off = 128 s) and pre-whitened using a first- 178order autoregressive process (Friston et al., 2002). Session specific 179 grand mean scaling was used. From these analyses we used contrasts 180 of parameter estimates of task against baseline (OLR-baseline and 181 MOTOR-baseline) as inputs to group level one-sample t-tests of the 182 OLR and MOTOR tasks. 183

#### Seed selection

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For analyses of rFC we selected seeds on the basis of task-related activation on the OLR and MOTOR paradigms. We adopted this approach for consistency with our previous published work, examining prior brain state effects on functional connectivity in the language system (Waites et al., 2006). Specifically, we defined five motor and five 189

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