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Coupling between gamma-band power and cerebral blood volume during recurrent acute neocortical seizures

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ABSTRACT

Characterization of neural and hemodynamic biomarkers of epileptic activity that can be measured using non-18 invasive techniques is fundamental to the accurate identification of the epileptogenic zone (EZ) in the clinical 19 setting. Recently, oscillations at gamma-band frequencies and above (>30 Hz) have been suggested to provide 20 valuable localizing information of the EZ and track cortical activation associated with epileptogenic processes. Al-21 though a tight coupling between gamma-band activity and hemodynamic-based signals has been consistently 22 demonstrated in non-pathological conditions, very little is known about whether such a relationship is main- 23 tained in epilepsy and the laminar etiology of these signals. Confirmation of this relationship may elucidate the 24 underpinnings of perfusion-based signals in epilepsy and the potential value of localizing the EZ using hemody- 25 namic correlates of pathological rhythms. Here, we use concurrent multi-depth electrophysiology and 2-26 dimensional optical imaging spectroscopy to examine the coupling between multi-band neural activity and 27 cerebral blood volume (CBV) during recurrent acute focal neocortical seizures in the urethane-anesthetized 28 rat. We show a powerful correlation between gamma-band power (25–90 Hz) and CBV across cortical laminae, 29 in particular layer 5, and a close association between gamma measures and multi-unit activity (MUA). Our find- 30 ings provide insights into the laminar electrophysiological basis of perfusion-based imaging signals in the epilep-31 tic state and may have implications for further research using non-invasive multi-modal techniques to localize 32 epileptogenic tissue. 33

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39 Introduction

40 Understanding the effects of epilepsy on the neurovascular unit is fundamental to elucidating the pathophysiology of the disease and for 41 predicting, identifying and localizing epileptic activity. In medically in-42tractable focal epilepsies, the surgical removal of epileptogenic tissue 4344remains the most promising form of treatment. However, successful post-operative outcomes rely on an accurate delineation of the epilep-45togenic zone (EZ), defined as "the minimum amount of cortex that 46 47 must be resected (inactivated or completely disconnected) to produce seizure freedom" (Luders et al., 2006). As a result, there has been a 48 great deal of interest in characterizing potential biomarkers of epi-4950leptogenic networks, particularly those that may be measured using non-invasive techniques in order for there to be an appreciable clinical 5152application. Recent research, due in part to the advent of powerful dig-53ital broad-band electroencephalogram (EEG) systems, has suggested 54that pathological neural oscillations at gamma-frequencies and above

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http://dx.doi.org/10.1016/j.neuroimage.2014.04.014 1053-8119/© 2014 Published by Elsevier Inc. (>~30 Hz) are a valuable indicator of epileptogenic tissue in both neo- 55 cortical and mesiotemporal regions (Andrade-Valenca et al., 2011; 56 Bragin et al., 1999; Jirsch et al., 2006; Medvedev et al., 2011; Worrell 57 et al., 2004; Ziilmans et al., 2012). Furthermore, the clinical amenability 58 of blood-oxygenation level dependent (BOLD) functional magnetic res- 59 onance imaging (fMRI) has also led to it being combined with EEG to lo- 60 calize hemodynamic correlates of electrophysiological epileptic events 61 and aid identification of the EZ (Gotman et al., 2006; Salek-Haddadi 62 et al., 2006; Thornton et al., 2010). However, faithful interpretation of 63 fMRI data in terms of underlying neural activation relies on a detailed 64 understanding of neurovascular coupling, which can vary spatially 65 across laminae (Goense et al., 2012) and brain-regions (Devonshire 66 et al., 2012). A typical assumption that is made to facilitate analysis 67 and interpretation of neuroimaging data is that neurovascular coupling 68 is invariant across health and disease. Yet, since pathological brain states 69 such as epilepsy may be associated with altered neurovascular coupling 70 characteristics, the validity of this assumption has been the subject of 71 much investigation with varying methodologies and results (Hamandi 72 et al., 2008; Harris et al., 2013; Ma et al., 2012; Mirsattari et al., 2006; 73 Stefanovic et al., 2005; Voges et al., 2012; Zhao et al., 2009). Further 74

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research is therefore needed to elucidate the extent to which neuro-75 76 vascular coupling characteristics are preserved in the epileptic state, in order to improve interpretation of neuroimaging data in the disorder 77 78 and ensure the legitimacy of routine assumptions which make such techniques more practicable. Under normal conditions, local field po-79 tential (LFP) activity, and in particular the gamma-band component of 80 the LFP, is thought to be a more reliable predictor of perfusion-based 81 82 signals than multi-unit spiking activity (MUA), although the neurophys-83 iological basis for this remains a topic of intense research (Goense and 84 Logothetis, 2008; Logothetis et al., 2001; Niessing et al., 2005; Nir 85 et al., 2007; Sumiyoshi et al., 2012). These reports underscore the poten-86 tial value for non-invasive perfusion-based neuroimaging studies to probe cognitive processes. However, while there are considerable re-87 88 ports of pathological gamma activity in clinical (Doesburg et al., 2013; 89 Fisher et al., 1992; Herrmann and Demiralp, 2005; Wu et al., 2008) and experimental (Köhling et al., 2000; Medvedev, 2002; Traub et al., 90 91 2005) epilepsy, whether pathological gamma activity is preferentially 92coupled with hemodynamic signals in the epileptic state is untested. Confirmation of this relationship would suggest a common neural 93 driver of perfusion-related signals in health and epilepsy and, since 94 gamma-band neural measures are strongly co-localized to the EZ, high-95 light the potential for EEG-neuroimaging paradigms to further delineate 96 97 the EZ through localization of hemodynamic correlates of pathological 98 gamma activity.

With the above in mind, we sought to examine the laminar electro-99 physiological underpinnings of seizure-related hemodynamic signals 100 during recurrent ictal discharges in the urethane-anesthetized rat 101 102using the well-established 4-aminopyridine (4-AP) acute model of focal neocortical epilepsy. This model provides an ideal framework to 103 examine neurovascular coupling in epilepsy, since seizures recur spon-104 taneously and evolve through similar stages as spontaneous events in 105the human brain (Harris et al., 2013; Ma et al., 2012; Zhao et al., 106 1072009). Using simultaneous high resolution two-dimensional optical 108 imaging spectroscopy (2D-OIS), we show a powerful linear correlation between cerebral blood volume (CBV) and gamma-band power across 109all cortical laminae, which was most pronounced in layer 5. Further-110 more we show that seizure-related gamma-band activity was most 111 112 closely coupled to multi-unit activity in deeper laminae nearest the presumed EZ. Our findings provide insights into the laminar evolution of 113 neural measures during recurrent seizures and perfusion-based imag-114 ing of seizure events for clinical purposes. 115

116 Materials and methods

117 All procedures described were approved by the UK Home Office under the Animals (Scientific procedures) Act of 1986. Female hooded 118 119Lister rats (total N = 8 weighing 260–400 g) were kept in a 12-hr dark/light cycle environment at a temperature of 22 °C, with food and 120water provided ad libitum. The animals were anesthetized with ure-121 thane (1.25 g/kg) intraperitoneally, with atropine being administered 122subcutaneously (0.4 mg/kg) to reduce mucous secretions during sur-123124gery. Depth of anesthesia was monitored throughout and supplementa-125ry doses of urethane (0.1 ml) were administered if necessary. We chose to use urethane anesthesia (ethyl carbamate) as it preserves excitatory/ 126inhibitory synaptic transmission, unlike many general anesthetics 127(Sceniak and MacIver, 2006) and provides a persistent and steady 128129depth of surgical anesthesia, reminiscent of natural sleep (Pagliardini et al., 2013). Moreover, neurovascular coupling is preserved under ure-130thane anesthesia, not only insofar that a single whisker deflection elicits 131 a hemodynamic response in the rat somatosensory cortex (Berwick 132et al., 2008) but also during CO₂ challenge (Kennerley et al., 2011), 133which has led to it being a common choice in neuroimaging studies in 134 rat and neurovascular coupling characteristics to be well-documented 135during both task-related events (e.g. Berwick et al., 2008; Devor et al., 136 2005; Harris et al., 2013; Huttunen et al., 2008; Kennerley et al., 2011) 137 138 and resting-state fluctuations (Bruyns-Haylett et al., 2013). It has also been shown that neither the spatial-temporal pattern of the evoked hemodynamic response (Devor et al., 2005), nor the relationship between neural activity and BOLD fMRI responses (Huttunen et al., 2008), differs between urethane and alpha-chloralose, another anesthetic routinely used in fMRI studies and whose neurovascular coupling characteristics in turn are comparable to a number of other agents (Franceschini et al., 2010). 145

A homoeothermic blanket (Harvard Apparatus) and rectal probe 146 were used to maintain core body temperature at 37 °C. The animals 147 were tracheotomized to allow artificial ventilation with pressurized 148 room air and monitoring of end-tidal CO₂. Blood-gas and end-tidal 149 CO2 measurements were used to adjust ventilator parameters and 150 maintain the animal within normal physiological limits (average values: 151 $pO_2 = 92 \text{ mm Hg} \pm 9.2, pCO_2 = 31 \text{ mm Hg} \pm 5.3$). The left femoral ar- 152 tery and vein were cannulated to allow the measurement of arterial 153 blood pressure and phenylephrine infusion (0.13 to 0.26 mg/h to main- 154 tain normotension between 100 and 110 mm Hg), respectively. The an-155 imal was secured in a stereotaxic frame (throughout experimentation), 156 and the skull overlying coordinates 2 mm anterior to lambda to 2 mm 157 anterior of bregma, and from 1 to 6 mm from midline, was thinned to 158 translucency, in order to expose the somatosensory cortex. A circular 159 plastic 'well' was located over the cranial window and filled with saline 160 to reduce optical specularities from the brain surface during imaging. 161

The potassium channel blocker 4-aminopyridine (4-AP, Sigma, 162 15 mM, 1 μ) was used to elicit focal seizure-like discharges (Ma et al., 163 2012; Zhao et al., 2009) in the right vibrissal cortex (RVC). After a 30 s baseline recording period, 4-AP was infused at a depth of 1500 μ m (i.e. layer 6) via a fluidic port on the multi-channel microelectrode (Neuronexus Technologies, Ann Arbor, MI, USA) over a 5 minute period (0.2 μ l/min) using a 10 μ l Hamilton syringe and syringe pump (World Precision Instruments Inc., FL, USA). Recordings were made for 50 min following regional injection of 4-AP.

Two-dimensional optical imaging spectroscopy (2D-OIS) was 171 employed to produce 2D images over time of total hemoglobin concen- 172 tration (Hbt). Under the reasonable assumption of a constant hemato- 173 crit, Hbt can be further interpreted as cerebral blood volume (CBV) 174 and will therefore be referred to as the latter in ensuing text (with 175 the exception of when reporting micro-molar concentrations of Hbt). 176 This technique has been described in detail previously (Berwick et al., 177 2008). Briefly, illumination of the cortex was conducted at four 178 different wavelengths (495 \pm 31 nm, 559 \pm 16 nm, 575 \pm 14 nm and 179 587 ± 9 nm FWHM) using a Lamda DG-4 high speed filter changer 180 (Sutter Instrument Company, Novata, CA, USA). Image data were re- 181 corded using a Dalsa 1M30P camera (Billerica, MA, USA, each pixel 182 representing ~75 μ m²), synchronized to the filter switching (effective 183 frame rate of 8 Hz/wavelength). These were then subjected to spectral 184 analysis consisting of a path length scaling algorithm (PLSA) employing 185 a modified Beer-Lambert law in conjunction with a path-length correc- 186 tion factor for each wavelength used, based on Monte Carlo simulations 187 of light transport through tissue. After each experiment, a 'dark baseline' 188 image data-set was obtained, in which the cortex was not illuminated, 189 and later subtracted from 2D-OIS data in order to account for electrical 190 noise arising from the camera system. 191

In order to localize the region of the somatosensory 'barrel' cortex 192 and guide implantation of the multi-channel electrode into the said 193 area, a preparatory 2D-OIS experiment was conducted in each animal. 194 This technique has also been described in detail previously (Berwick 195 et al., 2008). Briefly, the left mystacial pad was electrically stimulated 196 using subcutaneous electrodes (30 trials, 2 s, 5 Hz, 1.2 mA intensity 197 and 0.3 ms pulse width) and recorded image data subjected to the 198 aforementioned spectral analysis. Spatiotemporal changes in Hbt were 199 analyzed using statistical parametric mapping (SPM) in which each 200 pixel's timeseries was regressed against a design matrix representing 201 a direct current (DC) offset, ramp, and 'boxcar' function of the same du- 202 ration as the stimulation. This produced a *z*-score activation map in 203 which pixels within 50% of the maximum *z*-score were used to identify 204

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