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## Glucose Oxidase and Horseradish Peroxidase Like Activities of Cuprous Oxide/Polypyrrole Composites



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#### ABSTRACT

Cu<sub>2</sub>O/Ppy composites coated linen texture (LT) papers possess enzyme activities of glucose oxidase (GOx) and horseradish peroxidase (HRP) in alkaline solution (0.5 M NaOH). At the potential of 0 V vs. Ag/AgCl reference electrode,  $H_2O_2$  was produced through oxidation of glucose on the functional LT paper electrode in the presence of  $O_2$ . The as-produced  $H_2O_2$  was reduced on the electrode at the potential of -0.57 V vs. Ag/AgCl reference electrode. Cyclic voltammograms (CVs) reveal that Cu(1)/Cu(II), Cu(II)/Cu(I), and Cu(1)/Cu transitions occur at *ca*. 0, -0.57, and -0.85 V respectively. The electrode allows detections of glucose and  $H_2O_2$  down to 0.16 and 0.41 mM, respectively. The high catalytic activity of the Cu<sub>2</sub>O/Ppy composites is attributed to the stable coatings of Ppy and the high-index facets of Cu<sub>2</sub>O octahedra and microflowers. Having advantages of a low onset potential (*ca*. -0.02 V), high sensitivity (28  $\mu$ A mM<sup>-1</sup> cm<sup>-2</sup>), and selectivity, the stable and durable LT paper electrode has been validated for the quantitation of glucose in blood samples, showing its great potential for monitoring blood glucose levels.

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### 1. Introduction

According to world health organization (WHO), 422 millions of people in the world are affected by diabetes, which reflects the importance of low-cost and simple techniques for accurate monitoring of blood glucose levels [1,2]. The blood glucose concentrations in diabetic patients are in the range of 9-40 mM, which are higher than that (3-8 mM) of healthy people [3]. Various optical and electrochemical sensing systems have been used for the detection of glucose [4–10]. Electrochemical systems are more attractive, mainly because of their simplicity, cost effectiveness, sensitivity, and selectivity [1,7,11–13]. To provide selectivity toward glucose, most of the electrochemical systems require glucose oxidase (GOx) that catalyzes  $\beta$ -D-glucose to glucono- $\delta$ -lactone and  $H_2O_2$  in the presence of  $O_2$  [7,11,13,14]. The as-produced glucono- $\delta$ -lactone is subsequently converted to gluconic acid through hydrolysis. By monitoring the current generated from reduction of  $H_2O_2$ , the concentration of glucose can be determined [13]. Although these approaches are sensitive and selective, durability and short self-life of the electrodes are two other issues.

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http://dx.doi.org/10.1016/j.electacta.2016.08.071 0013-4686/© 2016 Elsevier Ltd. All rights reserved. Several nanomaterials have been used as enzyme mimics for the electrochemical detection of glucose [15–24]. Although GOx is not required, catalysts like Fe<sub>2</sub>O<sub>3</sub> [15], Ni [16,22], and Ag [17] provide poor selectivity and low catalytic activity. On the other hand, use of high-cost Co<sub>3</sub>O<sub>4</sub> [18], Au [20], or Pt [23] nanomaterials is a concern. Less-expensive metallic copper (Cu) and its oxides (e.g. CuO and Cu<sub>2</sub>O) have become popular for the detection of glucose [21,25]. When compared to spherical like Cu/CuO<sub>x</sub> nanoparticles [26,27], hierarchical nano/microstructures such as nanowires [24] and nanorods [21] having greater reaction sites and higher surface energy are more electrochemically active toward glucose. It has also been shown that crystal facets of Cu<sub>2</sub>O play an important role in the glucose oxidation [28].

Oxidation of glucose on a Cu electrode forms products such as gluconic acid (pka 3.60) through four steps: (i) adsorption of glucose onto the surface of Cu(I) or Cu(II) hydroxides/oxides, (ii) formation of Cu(III) species, (iii) formation of glucose/copper complexes, and (iv) C—C bond cleavage [29]. Under alkaline conditions, several oxidized products, including gluconic acid, glucuronic acid, and formic acid have been detected, which suggests that different mechanisms likely occur in the glucose oxidation [30]. Because it is extremely difficult to isolate the products, simple and innovative strategies for the identification

and quantification of each of the products are highly demanded for providing a detailed mechanism for glucose oxidation.

Different mechanisms have been suggested for glucose oxidation on various electrodes such as Cu<sub>2</sub>O and metallic Cu electrodes [30,31]. On the surfaces of Cu/Cu<sub>2</sub>O, glucose as an enediol form is oxidized by various surface states of Cu through the transitions I-III [29,32]. The oxidation is mainly mediated by Cu(II)/Cu(III) transition to form gluconic or glucuronic acid and then to form formate and carbonate through C—C bond cleavage [27]. Surface properties of the electrode play a significant role in determining its electrochemical activity. For example, conducting polymers such as polyaniline and polypyrole (Ppy) coated on the Cu/Cu<sub>2</sub>O surfaces can increase the conductivity and stability of the electrode and thus can reduce the overpotential for glucose oxidation [33-35]. Ppy is commonly used to control Cu<sub>2</sub>O structures, mainly due to its greater electrochemical stability over a wide potential window [33]. Glucose oxidation on Cu<sub>2</sub>O/Ppy electrodes in 0.1 M NaOH occurs in the potential range of 0 to 0.8 V [36]. Although the electrodes are useful for monitoring glucose levels in blood samples, mechanisms for glucose oxidation on the electrodes are still unclear.

In this study, we used Cu<sub>2</sub>O/Ppy linen texture (LT) paper electrodes for the electrochemical oxidation of glucose in wide potential windows (-0.75 to 0.6 V and -1.2 to 0.6 V) under alkaline conditions (0.5 M NaOH). The Cu<sub>2</sub>O/Ppy composites exhibited enzyme mimic activity of GOx to catalyze glucose in the presence of O<sub>2</sub> to form H<sub>2</sub>O<sub>2</sub> at 0 V vs. Ag/AgCl reference electrode. The composites also showed enzyme mimic activity of horseradish peroxidase (HRP) to reduce as-produced  $H_2O_2$  at -0.57 V vs. Ag/ AgCl reference electrode. The functional LT paper electrode exhibited high selectivity toward glucose, with minimum interferences from various biological compounds. The high catalytic activity of the Cu<sub>2</sub>O/Ppy LT paper electrode is attributed to the high-index facets of Cu<sub>2</sub>O structures. We proposed a detailed mechanism for glucose oxidation on the paper electrode. Practicality of the functional LT paper electrodes was validated by the quantitation of glucose in human blood samples.

#### 2. Experimental

#### 2.1. Materials

Catechin hydrate (98%) was obtained from Sigma Aldrich (St. Louis, MO, USA). Copper (II) nitrate trihydrate (Cu (NO<sub>3</sub>)<sub>2</sub>.3H<sub>2</sub>O, 80%) was purchased from Showa (Tokyo, Japan). Pyrrole (99.5%) was obtained from Acros Organics (Geel, Belgium) and used without any further purification. Sodium hydroxide (pellet, 98.9%) was purchased from J.T. Baker (Phillipsburg, NJ, USA). Nafion 117 (5 wt%) was procured from Fluka (Buchs, Switzerland). Acetaminophen (>99.8 wt%), L-ascorbic acid (>99.8 wt%), Cu<sub>2</sub>O particles  $(<5 \,\mu\text{m})$ , cysteine (>99.8 wt%), ß-D-glucose (>99.8 wt%), and uric acid (>99.8 wt%%) were purchased from Sigma (St. Louis, MO, USA). LT paper (A4 size,  $6 \times 2.5$  cm with GSM of 247.5 g m<sup>-2</sup>) was purchased from Sun Hong (Taipei, Taiwan). Terephthalic acid (TA) was purchased from Janssen Chimica (Beerse, Belgium). All aqueous solutions were prepared in ultrapure water (18.2 M $\Omega$  cm) produced by a Milli-Q ultrapure system of Millipore (Billerica, MA, USA).

#### 2.2. Characterization

A JSM-1200EX II transmission electron microscope from JEOL (Tokyo, Japan) and a Hitachi S-2400 scanning electron microscope from Hitachi High-Technologies (Tokyo, Japan) equipped with an energy-dispersive X-ray spectrometer (EDS) were employed to investigate the morphology and composition of Cu<sub>2</sub>O/Ppy

composites. A Philips Tecnai F20 G2 FEI-TEM (Roanoke, VA, USA) was used to record high-angle annular dark-field scanning transmission electron microscopy (HAADF-STEM) images. STEM measurements were taken using formvar/carbon film Cu grids (200 meshes; Agar Scientific) coated with aliquots  $(2 \mu L)$  of Cu<sub>2</sub>O/ Ppy composites which were separated from the LT paper by soaking in aqueous solution and sonicating for 10 min. Prior to scanning electron microscopy (SEM) measurements, a Cu<sub>2</sub>O/Ppy LT paper  $(1 \times 1 \text{ cm}^2)$  was dried overnight at ambient conditions (27 °C). X-ray diffraction (XRD) pattern of Cu<sub>2</sub>O/Ppy composites was obtained using a PANalytical X'Pert PRO diffractometer from PANalytical B.V. (EA Almelo, Netherlands) and Cu-Ka radiation  $(\lambda = 0.15418 \text{ nm})$ . Prior to XRD analysis, the samples were prepared on Si substrates and dried overnight. The hydroxyl (OH<sup>•</sup>) radical formed during the electrochemical oxidation of glucose was determined by fluorescence. Aliquots  $(300 \,\mu\text{L})$  of the liquid products were taken from the electrochemical cell and then mixed with aqueous solution of TA (3 mM, 100 µL). The fluorescence of the product, 2-hydroxyterephthalic acid (TAOH), was recorded using a Cary Eclipse fluorescence spectrophotometer from Varian (Palo Alto, CA, USA). After electrolysis of glucose (5 mM) in 0.5 M NaOH solution on the Cu<sub>2</sub>O/Ppy electrode for 43200 s, aliquots (10 µL) of the product solution were taken from the electrochemical cell and mixed with HgTe nanostructures  $(10 \,\mu L)$  for SALDI-MS measurements [37]. About  $2 \,\mu L$  of this mixture was pipetted onto a stainless-steel 96-well MALDI target (Bruker Daltonics) and dried at ambient conditions. As controls, aliquots (10 µL) of glucose and gluconic acid solutions were used instead of the electrolyzed solution. SALDI-MS spectra of the sample were recorded using a reflectron-type time of flight (TOF) mass spectrometer purchased from Biflex III, Bruker (Bremen, Germany) equipped with a 1.25-m flight tube. SALDI-MS spectra of glucose and gluconic acid (controls) were recorded in positive and negative-ion modes, respectively. All the samples were irradiated by a nitrogen laser (emission at 337 nm) with a frequency of 10 Hz and pulse duration of 4 ns. The ions generated during laser desorption were stabilized within a delayed extraction period of 200 ns and accelerated through a linear TOF reflection before reaching the mass analyzer. An accelerating voltage of 20 kV was used. Each mass spectrum was obtained after 300 laser pulses.

#### 2.3. Fabrication of Cu<sub>2</sub>O/Ppy LT paper electrodes

The Cu<sub>2</sub>O/Ppy composites coated on LT papers were prepared according to the literature [38]. Briefly, the pyrrole coated LT paper (0.011 g cm<sup>-2</sup>,  $6 \times 2.5$  cm) was reacted with a mixture of Cu (NO<sub>3</sub>)<sub>2</sub> (3 mL, 0.1 M) and NaOH (30 mL, 7.5 M) for 30 min to form the Cu<sup>2</sup> <sup>+</sup>/pyrrole complexes. Then, catechin (60 mg) was added into this solution, which was heated at 80 °C for 1 h to complete oxidative polymerization of pyrrole and reduction of Cu<sup>2+</sup> ions to form PPy and Cu<sub>2</sub>O particles, respectively [38,39]. The as-prepared Cu<sub>2</sub>O/Ppy LT paper was soaked in 100 mL of ultrapure water for 10 min to remove excess NaOH and dried overnight prior to electrochemical experiments.

#### 2.4. Electrochemical oxidation of glucose

A 50-ml three-necked glass cell was used in each electrochemical experiment. The Cu<sub>2</sub>O/Ppy (mass loading: 0.  $2 \text{ mg cm}^{-2}$ ) LT paper fixed with a Cu tape (0.5 cm) on one end was used as a working electrode. The area of the working electrode in contact with the solution was about 5 cm<sup>2</sup>, which was considered as the final working area. All potentials were measured against an Ag/ AgCl electrode. A Pt wire with 0.5 mm diameter was used as a counter electrode. Prior to each electrochemical measurement, O<sub>2</sub> gas was purged into the electrolyte solution for 30 min. During the Download English Version:

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