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Short Communication

A novel cardiac spectral envelope extraction algorithm using a single-degree-of-freedom vibration model

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ABSTRACT

A novel cardiac spectral envelope extraction method was developed to acquire the optimal envelope information in the frequency domain to differentiate normal heart sounds and valvular heart disorders for further analysis. This automatic algorithm was based on the vibration model of a mass–spring–damper system. To acquire the best spectral envelope information from both a normal heart sound signal and an aortic regurgitation murmur signal, the morphological influence of two analytical parameters, the natural frequency p (range: 1–100 Hz) and the damping factor ζ (range: 10–500%), on the single-degree-of-freedom model was evaluated using the root mean square error. The cardiac spectral envelope curve could be optimized at the natural frequency of 35 ± 5 Hz and the damping factor of $70 \pm 8\%$. The spectral envelope extracted by the single-degree-of-freedom model showed more informative and efficient morphological characteristics than that extracted by an autoregressive power spectrum density model reported previously.

1. Introduction

A spectral envelope is the shape of the power spectrum of a signal. It is an important tool for the identification of specific sounds or signals [1] and provides a simple and conspicuous representation of the intrinsic properties of a signal [2,3]. Various spectral envelope estimation methods, including linear predictive coding (LPC), autoregressive moving average modeling, cepstrum analysis, and the discrete cepstrum, have been proposed to extract the spectral envelope of a biomedical signal [4]. LPC is a method used to compute an autoregressive (AR) model to replicate a desired power spectrum as the transfer function of an all-pole filter with order p. This estimation falls below the true spectrum and exceeds the true spectrum in regions that drop suddenly. Therefore, there are considerable mismatching errors between a true spectrum and its corresponding LPC envelope [5].

In a previous study [6], we reported a novel heart murmur classification method using the envelope curve of the power spectral density (PSD) in the frequency domain. It shows obviously that the cardiac spectral information itself and its shape are determined by the activity and mechanical and geometric properties of the heart valves. The cardiac spectral shape can be used to evaluate the functions of the cardiovascular system [7]. The envelope was estimated by the normalized AR modeling of the PSD waveforms for a heart sound. This algorithm showed superior performance with high sensitivity and specificity. Furthermore, in order to extract single characteristic peaks from the spectral envelope, a multi-Gaussian model was used. Each Gaussian profile showed distinct cardiac hemodynamic sequences for normal heart sounds and murmurs [7]. However, we could not ignore the presence of a mismatch between the true spectrum and the extracted envelope. Although the order of the AR model was selected using the Akaike information criterion (AIC) [8], the mismatching error directly affects the single characteristic peaks. Therefore, a new spectral envelope method to decrease the number of mismatching errors is needed.

In a previous study [3], we developed a cardiac envelope extraction algorithm based on a single-degree-of-freedom analytical model in the time domain. This algorithm showed good performance compared to two popular envelope extraction algorithms, including the Shannon envelope, based on the normalized average Shannon energy, and the Hilbert envelope, based on the Hilbert transform [2]. Therefore, we developed a novel spectral envelope extraction algorithm based on a single-degree-of-freedom

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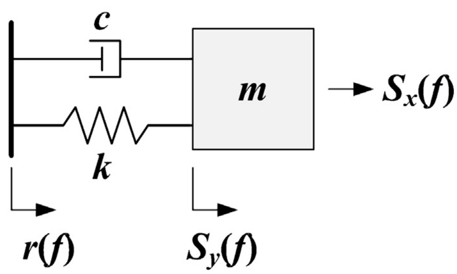

Fig. 1. A single-degree-of-freedom vibration model to extract the cardiac spectral envelope information. Here, m denotes the mass, c denotes the damping coefficient, k denotes the coefficient of the spring, $r(f)$ denotes the rack displacement, $S_x(f)$ denotes the input waveform, and $S_y(f)$ denotes the output response.

vibration model controlled by the natural frequency and the damping factor. The proposed mass–spring–damper model was optimized by the root mean square error measure and its morphology was compared with the results of the AR-PSD estimation method.

2. Cardiac spectral envelope extraction method

2.1. Collection of cardiac sounds

Eight normal cardiac sounds were recorded from eight healthy subjects (aged 28 ± 9 yr) with no history of heart complications using a self-constructed stethoscope system, and eight aortic regurgitation murmurs were selected from eight patients without other coexistent heart valvular disorders (aged 72 ± 16 yr) in medical textbooks authorized by a cardiovascular specialist [2]. All signals had 16 bit-depth and a sampling frequency of 8000 Hz. Additional signal processing to eliminate a fundamental power interference of 60 Hz and its harmonics was not applied to any given signal $x(t)$, $t = 1, \ldots, N$, where N denotes the number of data points.

2.2. Wavelet-based pre-processing

The wavelet decomposition using the Daubechies mother wavelet (Db10) with nine scales was used to eliminate the uninteresting frequency components from an original signal. The approximations at three and nine scales were selected to eliminate high-frequency contents over 500 Hz and low-frequency contents below 7 Hz, respectively. The pre-processed signals had the frequency characteristics of 7–500 Hz. The normalization was applied by setting the variance of the signal to a value of 1.

2.3. Single-degree-of-freedom vibration model

Consider a wide sense stationary (WSS) random process dataset $x(t)$ with the autocorrelation function $R_x(\tau)$. The PSD of $x(t)$ is given by the Fourier transform of its autocorrelation function as

$$S_x(f) = \int_{-\infty}^{\infty} R_x(\tau) e^{-j2\pi f \tau}\, d\tau. \quad (1)$$

Consider a one-dimensional spring–mass–damper system (Fig. 1), where m denotes the mass, c denotes the damping coefficient, and k denotes the coefficient of the spring. This single-degree-of-freedom analytical model with the input $S_x(f)$ and the output response $S_y(f)$ is given by

$$m\ddot{S}_y(f) + c\dot{S}_y(f) + kS_y(f) = S_x(f), \quad (2)$$

where $r(f)$ denotes the rack displacement $r(f) = 0$. Eq. (2) may be written as

$$\ddot{S}_Y(f) + 2p\zeta\dot{S}_Y(f) + p^2 S_Y(f) = S_X(f), \quad (3)$$

where $p = \sqrt{k/m}$, $\zeta = c/2\sqrt{mk}$, and $S_X(f) = S_x(f)/m$. This vibration model could be controlled by two analytical parameters, p and ζ, defined as the natural frequency (Hz) and the damping factor (%), respectively. The cross-correlation function was used to compensate for time delays by applying the low natural frequency to the cardiac spectral envelope. We compensated for the relative time delay by selecting the maximum peak of cross-correlation between two signals,

$$S_Y(f) = S_y(f - |\max(|CC(f)|)|), \quad (4)$$

where $CC(f)$ denotes the cross-correlation between the input spectrum $S_x(f)$ and output response $S_y(f)$. A resulting signal was computed by applying the square root $P(f) = e^{0.5 \ln S_Y(f)}$, and the normalized waveform $P(f)$ was called the cardiac spectral envelope curve. This automatic algorithm was implemented using the MATLAB software (MathWorks Inc., Natick, MA, USA).

2.4. Validation

The proposed cardiac spectral envelope extraction algorithm was evaluated by the root mean square error (RMSE) between the input waveform $S_x(f)$ and the output waveform $P(f)$ on a single-degree-of-freedom vibration model as

$$RMSE = \sqrt{\frac{1}{M}\int_{f=1}^{M} (P(f) - S_x(f))^2}, \quad (5)$$

where M denotes the maximum frequency index of the target range $M = 500$ Hz. The optimal natural frequency and damping factor were selected by the derivative of RMSE (dRMSE).

2.5. Statistical analyses

Quantitative data are expressed as means ± standard deviations. Statistical analyses were performed using a two-tailed Student's t-test to compare the mean values obtained from two groups, using the frequency index of the maximum peak ($Fmax$) in the spectral envelopes [6]. P-values less than 0.05 were considered statistically significant.

3. Experimental results

The effects of two analytical parameters on the morphology of the cardiac spectral envelope were investigated to acquire the optimal spectral envelope information. We first evaluated the effect of the natural frequency p over a range of 1–100 Hz on the cardiac spectral envelopes for normal heart sounds (Fig. 2A) and aortic regurgitation murmurs (Fig. 2B) under setup conditions where the damping factor ζ was 70.7%. A murmur led to a significant shift in $Fmax$ (main peak) and a high density at a high frequency index (greater than 200 Hz) in the spectral envelopes compared to the normal heart sound ($P < 0.0001$ *vs.* the normal cardiac spectral envelope). These differences were due to the presence of a diastolic murmur, when the aortic valve was incapable of preventing the backflow of blood from the aorta into the left ventricle during ventricular diastole [7]. The normal cardiac spectral envelopes showed that a natural frequency p of 1–15 Hz led to a single main peak with $Fmax = 77.24 \pm 18.51$ Hz, while a p of 18–100 Hz led to multiple peaks and $Fmax = 38.42 \pm 2.70$ Hz ($P < 0.0001$ *vs.* that for $p = 1$–15 Hz). In particular, a p less than 15 Hz led to a dull envelope while a p greater than 18 Hz led to a low-noise sharp envelope.