



# Selective electrochemical polymerization of 1-naphthylamine on carbon electrodes and its pH sensing behavior in non-invasive body fluids useful in clinical applications

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## ABSTRACT

pH value of a non-invasive sample is an important biomarker in diagnosing certain clinical disorders of a human body. Herein, we report, a stable, surface-confined and redox active poly(1-naphthylamine) (PNPA) on multi-walled carbon nanotube modified gold and pencil graphite electrodes (Au/MWCNT@PNPA and PGE@PNPA) prepared via electrochemical polymerization of 1-naphthylamine (1-NPA) in pH 7 phosphate buffer solution for sensitive and selective pH monitoring of non-invasive samples (saliva, tears and urine). Control experiment with 2-NPA isomer failed to show such redox feature, indicating the selective electrochemical polymerization of 1-NPA. Physicochemical characterizations of MWCNT@PNPA by SEM, TEM, XPS, Raman, FTIR, UV–vis (an ethanolic extract) and several control electrochemical experiments revealed that 4th (para) position of 1-NPA isomer is involved in the initiation of electro-polymerization on a carbon surface and followed by a stable redox polymer formation. Interestingly, the redox peak responsible for pH sensing showed negligible to permissible level of alteration with several biochemicals. As a diverse application, selective monitoring of bacterial (*E. coli*) growth was demonstrated using this new electrochemical pH sensor system with result comparable to that of conventional pH sensor.

## 1. Introduction

Non-invasive samples like urine, saliva, sweat and tears are alternate diagnostic fluids to direct blood [1,2]. The pH value of such non-invasive samples is assumed to be a biomarker for direct information about acid-base balance of human body and helpful in assessing certain clinical disorders [1–3]. For instance, urinary crystals formation upon altering the pH of urine [4]. Similarly, pH of saliva is an indicator for oral diseases such as dental caries, periodontitis and oral malodor [5]. Meanwhile, tear fluid pH also contributes to the health and function of the anterior ocular tissues [6]. Thus, a simple, sensitive and quick measurement of pH of non-invasive samples is a significant research interest in clinical analytical chemistry.

For the measurement of pH, several spectroscopic methods based on

UV–vis, fluorescence and Nuclear Magnetic Resonance (NMR) and potentiometric techniques have been reported. For example, monolithic silica doped alizarin red [7], 4-((p-nitrophenyl)azo) phenol and 2-methoxy-4-((4-nitrophenyl)azo)phenol dyes immobilized triacetyl cellulose membrane [8] and a Donor– $\pi$ –Acceptor heterocyclic azo chromosphere [9] as pH sensitive absorbance systems by UV–vis spectroscopy; 4-(p-*N,N*-dimethylamino phenyl methylene)-2-phenyl-5-oxazolone embedded plasticized PVC polymer film [10], 4-trifluoromethylcarbostyryl derivative of diethylene triaminepentaacetic acid-europium (III)-complex entrapped sol–gel and ormosil [11] and bromocresol purple sol–gel modified thin film [12] as pH sensitive fluorescence systems for pH sensing were reported. For NMR based pH measurement, a concentrated acidic aqueous solution buffered by fluoride ion in the pH 1.5–4.5 range, wherein, the fluoride <sup>19</sup>F chemical

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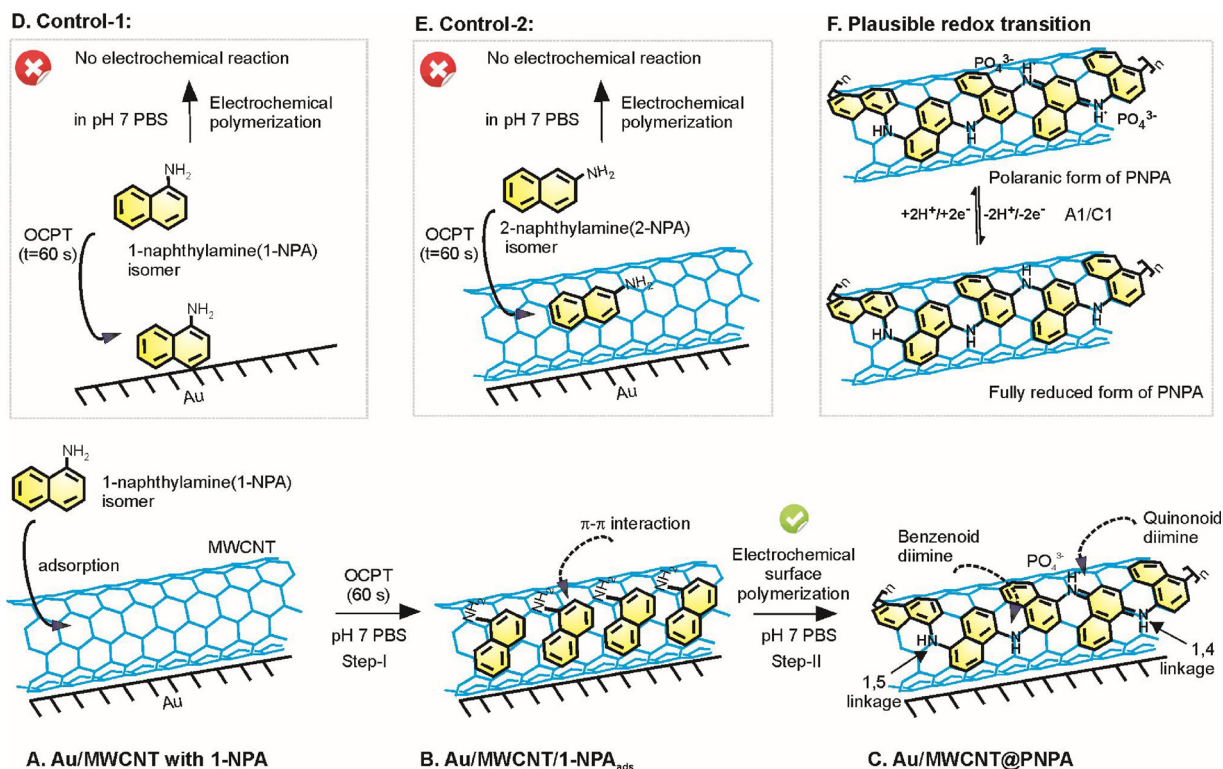
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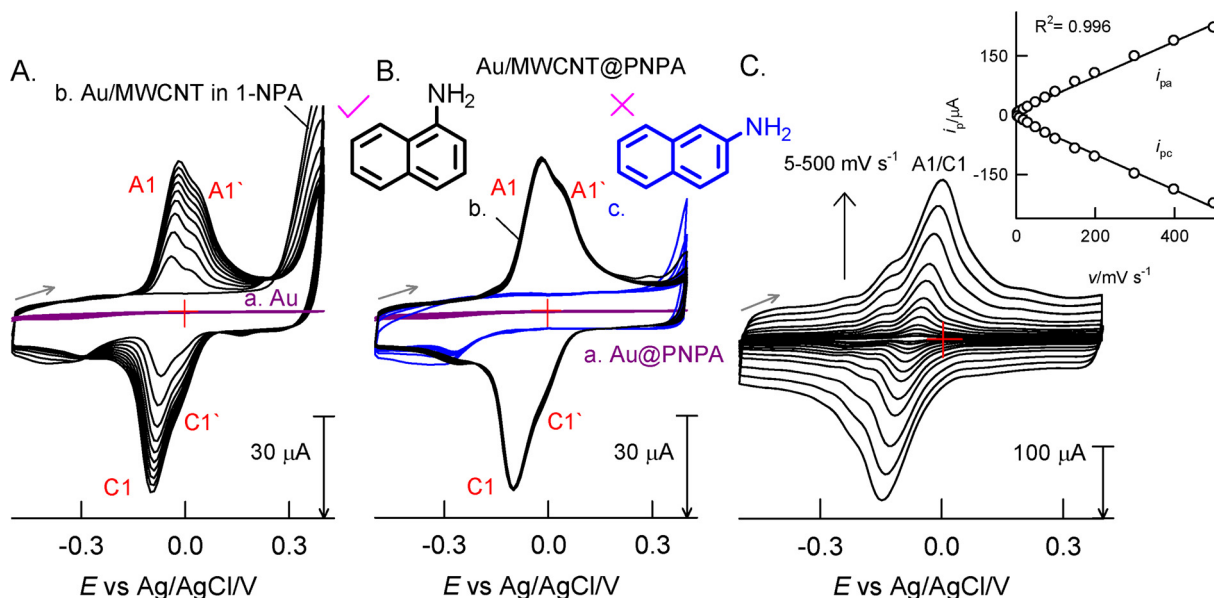
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**Scheme 1.** (A–C) Schematic representation for selective preparation of poly (1-naphthylamine) (PNPA) from 1-naphthylamine (1-NPA) isomer on pristine multi-walled carbon nanotube (MWCNT) modified electrode in neutral pH condition and its control experiments (D&E). (F) Plausible redox transition of PNPA on MWCNT.



**Fig. 1.** Continuous CV responses of (A) Au (curve a) and Au/MWCNT (curve b) in 1 mM 1-NPA, (B) Au@PNPA (curve a) and Au/MWCNT@PNPA formed from 1-NPA (curve b) and 2-NPA (curve c) in pH 7 PBS and (C) effect of scan rate ( $5\text{--}500\text{ mV s}^{-1}$ ) on CV of Au/MWCNT@PNPA in pH 7 PBS. Inset plot is peak current vs scan rate.

shift with respect to an internal standard, 3-fluoropyridine, was reported [13]. Indeed, with respect to on-line measurement, necessary off-line treatment and rare to realize the real-time monitoring in living systems, these methods restrict for routine sample analysis. On the other hand, electrochemical techniques offer a simple, rapid and efficient route for pH sensing. At present, a glass-membrane based ion-selective electrode, in which, a dilute solution of HCl filled membrane micro-ball coupled with Ag/AgCl reference electrode, has been widely used for pH measurements [7–14]. But, they are fragile and need a large

volume of sample ( $> 2\text{ mL}$ ). Alternately, pH sensitive redox probe coupled with voltammetric technique, wherein, the electro-active probe either mounted on working electrode surface (heterogeneous) or dissolved in test solution (homogenous) offers a better alternative for routine and practical analysis.

Electrochemical probes like quinone [15], metal oxide (iridium oxide [16], ruthenium oxide, tin dioxide [17] and zinc oxide [18]), azo dye [19] and conducting polyaniline (PANI) [20] modified on glassy carbon [21], gold [22] screen-printed electrode [23] and pencil lead

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