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Original Article

## Footfall patterns of a runner with an Achilles tendon rupture

Daniel Jandacka<sup>a,\*</sup>, David Zahradnik<sup>a</sup>, Roman Farana<sup>a</sup>, Jaroslav Uchytíl<sup>a</sup>, Joseph Hamill<sup>b</sup><sup>a</sup> Department of Human Movement Studies, Human Motion Diagnostic Center, University of Ostrava, Ostrava 70200, Czech Republic<sup>b</sup> Department of Kinesiology, University of Massachusetts, Amherst, MA 01003, USA

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## Abstract

**Purpose:** This study aims to compare the load and the length of previously ruptured and healthy Achilles tendon (AT) of a recreational runner who used different footfall patterns on each limb during running.

**Methods:** A 41-year-old recreational athlete with a ruptured AT participated in this report. Two force plates and a high-speed motion capture system were used to collect ground reaction force and kinematic data in shod and barefoot running conditions. AT length was measured using ultrasonography and an infrared camera system. AT force was estimated as the active plantar flexion moment divided by AT moment arm during stance phase.

**Results:** The participant used a rearfoot pattern on the affected limb and a forefoot/midfoot pattern on the unaffected limb during shod running and a forefoot/midfoot pattern during barefoot running. There was no difference between the length of the affected and the unaffected AT. During shod running, the maximal AT force and loading rate was lower in the affected AT versus the unaffected AT. During barefoot running, the affected maximal AT force and loading rate was greater than the unaffected AT.

**Conclusion:** Footfall patterns can be an adaptation to reduce the loading on a previously injured AT. It appears that runners may consider using a rearfoot footfall pattern during running to reduce the stress on the AT.

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**Keywords:** Achilles tendon; Calcaneus; Footfall patterns; Injury; Running; Tendon length

## 1. Introduction

Humans are one of the few animals that utilize multiple footfall patterns. Runners may use a forefoot (FF), a midfoot (MF), or a rearfoot (RF) footfall pattern during running.<sup>1,2</sup> Hasegawa et al.<sup>2</sup> reported that approximately 75% of the shod distance runners use an RF pattern and the remaining 25% of the runners use either FF or MF patterns. Only a few studies have reported that some shod runners use different footfall patterns bilaterally.<sup>3,4</sup>

Larson et al.<sup>3</sup> reported some cases where runners exhibited a bilateral difference in footfall patterns with an RF pattern mostly on non-dominant foot and an FF pattern on dominant foot. They stated that it is unclear whether these combined landing patterns were a single uncommon footfall pattern sequence or simply a gait asymmetry. Williams et al.<sup>4</sup> described

an elite female runner with combined footfall pattern and speculated that this asymmetry was related to a previous groin injury. The current study is unique in trying to explain the cause of the unusual utilization of the combination of RF and FF footfall patterns. Some authors assume that MF and FF are natural types of footfall pattern that reduce running related injuries<sup>5,6</sup> and so the change to an FF pattern may be the result of escaping injury to one or the other limbs.

Recently, a runner who used different footfall patterns with each limb during shod running appeared in our laboratory during a research study of recreational runners with a history of Achilles tendon (AT) rupture. There is previous evidence of altered ankle kinematics during stance phase of 2 runners with an elongated AT.<sup>7,8</sup> Furthermore, AT elongation is a common problem for people with history of rupture.<sup>9</sup> AT rupture is a devastating injury that causes a functional deficit of the plantar flexors.<sup>10</sup> In spite of this, humans after AT rupture are still active as recreational athletes. However, running may not be without consequences if the previous musculo-skeletal system injury is associated with a higher incidence of injury among runners.<sup>11</sup>

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\* Corresponding author.

E-mail address: [daniel.jandacka@osu.cz](mailto:daniel.jandacka@osu.cz) (D. Jandacka)

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The second most common running related injury is Achilles tendinopathy whose incidence is estimated at 9.1%–10.9% of all runners.<sup>12</sup> To prevent or even “cure” running injuries, it has been suggested that runners should use either an FF or an MF footfall pattern.<sup>5,6</sup> However, Gruber et al.<sup>13</sup> reported that an FF footfall pattern is associated with higher AT forces compared to the RF pattern. Higher AT forces during running may indicate a greater risk of AT injuries.<sup>14</sup>

Therefore, the purpose of this study was to compare AT loading and AT length of the affected (previous AT rupture) and the unaffected (no injury) AT of a recreational runner who used a combined footfall pattern (i.e., FF on unaffected limb and RF on the affected limb). We hypothesized that the affected AT would appear elongated compared to the unaffected AT which could subsequently affect the ankle kinematics while running.<sup>7,8</sup> In addition, we expected a less loading on the affected AT compared to the unaffected AT. This study offers a unique opportunity to understand the preventive strategies and adaptations of the neuro-muscular system against overloading the weakened structures of the human body.

## 2. Case report

### 2.1. Participant

A 41-year-old recreational athlete and professional fireman sustained AT rupture on the left limb when he suddenly changed direction during running. The AT was sutured by mini-invasive technique on the day of the injury. Treatment of the subsequent inflammation required ablation of the proximal part of the calcaneus. From an ultrasonograph examination, a noticeable defect of the calcaneus and insertion of the affected AT was apparent (Fig. 1). Further treatment resulted in casting the knee and ankle for 6 weeks and followed by 4 months of rehabilitation. Four years later, this individual participated in a research study of running biomechanics of participants with a history of AT rupture. This individual reported that he used an FF footfall pattern when running before the AT injury. The procedure was approved by the University of Ostrava Ethics Committee and the informed consent was obtained from the study participant.

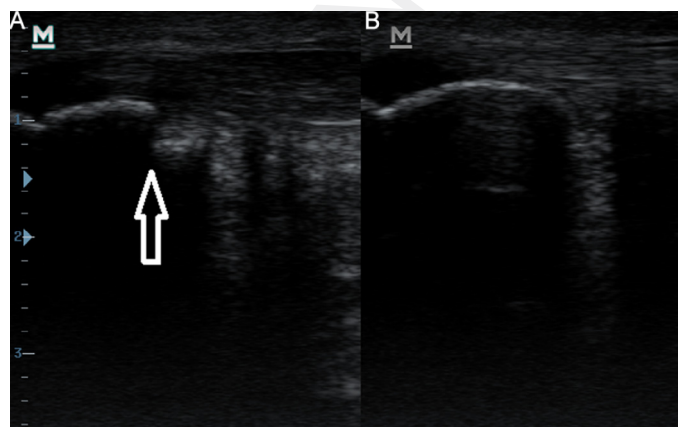


Fig. 1. Ultrasonography of the (A) affected and (B) unaffected insertion of the Achilles tendon on calcaneus.

At the time of the research study in which the subject initially completed, the participant’s body mass was 86.5 kg, height 1.73 m and body fat 23% of the total body weight. He reported a fifth level of physical activity (i.e., medium intensity exercise at least 3 times per week).<sup>15</sup> The maximum moment of force during the isometric contraction of dorsal and plantar flexors was measured using a force plate (Fitronic, FitroForce, Bratislava, Slovakia) with the individual’s lower extremity positioned at 90° of flexion at the ankle, knee, and hip.<sup>16</sup>

The results of the analysis indicated a greater dorsiflexor moment on the repaired AT limb versus the unaffected AT (difference 11 N·m, ES > 0.8) and a weaker plantar flexor moment on the affected limb (difference 41 N·m, ES > 0.8) compared to the repaired AT limb. The runner reported no pain or restrictions in activity shown by the foot and ankle outcome score (FAOS).<sup>17</sup> However the Achilles tendon total rupture score (ATRS) was rated at 44, causing the runner to feel limited during running.<sup>18</sup>

### 2.2. Instrumentation, protocol, and statistics

Two force plates (Kistler, 9286 AA a 9281CA; Kistler Instrumente AG, Winterthur, Switzerland) were used to collect ground reaction force data. The force platforms were placed in a 17-m-long runway and were situated flush with the floor. Data were sampled at a frequency of 1,200 Hz. Retro-reflective markers were placed on the subject prior to data collection according to the protocol suggested by Hamill and colleagues.<sup>19</sup> Calibration markers were placed bilaterally on the lateral and medial malleoli, the medial and lateral femoral condyles, the greater trochanter, and on the shoe/foot over the first and fifth metatarsal heads. Tracking markers were securely positioned to define the pelvis (iliac crest and posterior superior iliac spine, anterior superior iliac spine), the thighs and shanks (4 light-weight rigid plates holding a quaternion of markers), and the shoe/foot (a triad of markers on the heel over the calcaneus). Kinematics of the foot, leg, thigh, and pelvis were recorded at a frequency of 240 Hz using a motion capture system (Qualisys Oqus 100; AB, Göteborg, Sweden).

The participant completed a 5-min warm-up prior to data collection. Subsequently, he completed 5 acceptable trials over the force platforms at a speed of 3.2 m/s ( $\pm 5\%$ ) in each of 2 conditions: (1) running shod (Mizuno Crusader, Osaka, Japan) and (2) running barefoot. The barefoot condition was included to determine that the individual was capable of running with an FF pattern. The difference in the dependent variables was evaluated using effect size (ES), which was calculated and interpreted as trivial with ES < 0.2, small with ES between 0.21 and 0.50, medium with ES between 0.51 and 0.80, and large with ES > 0.81.<sup>20</sup>

### 2.3. Footfall pattern

This individual clearly used an RF pattern on affected and an FF pattern on unaffected foot when shod (Figs. 2A and 3 and Table 2). During barefoot running, he used only an FF footfall pattern (Fig. 4). However, during barefoot running, the ankle plantar flexion angle on the unaffected lower extremity was

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