



Determination of amino acids by capillary electrophoresis with differential resonant contactless conductivity detector

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ABSTRACT

The impedance of a capacitively coupled contactless conductivity detector (C^4D) in capillary electrophoresis (CE) was measured by an impedance analysis method. The influence of solution conductivity and capillary dimension on impedance parameters was investigated. Under the experimental conditions used, 86–99.9% of the total impedance of a C^4D is composed by its imaginary part from the capillary wall capacitor. With increasing inner diameter of capillary and solution conductivity in detection zone, the wall capacitance increases, which results in the increase in the response signal of C^4D . But the wall capacitance is only 0.5–12% of the predicted value according to a cylinder capacitor model. As the change in solution resistance is detected in a resonant C^4D (RC^4D), the sensitivity of contactless conductivity detection in CE is improved. The application of an end-to-end differential RC^4D (DRC^4D) system in CE was demonstrated in the determination of 10 amino acids. The running buffer consisted of 2 M acetic acid and 0.1% hydroxyethylcellulose (pH 2.1). The limit of detection for amino acids is in the range of 0.1–0.4 μM . Under our experimental conditions, the sensitivity of DRC^4D enhances by a factor of 15–29 as compared with C^4D .

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1. Introduction

Since the works of Zemann et al. [1] and da Silva and do Lago [2] in 1998, a capacitively coupled contactless conductive detector (C^4D) has received considerable attention as an alternative detection method in capillary electrophoresis (CE) and microchip electrophoresis [3–9]. Besides, the applications of C^4D in high-performance liquid chromatography [10,11], ion chromatography [12,13] and flow injection [14], non-invasive characterization of monolithic stationary-phase coatings [15,16], and measurement of electroosmotic flow (EOF) [17] and conductivity of aqueous droplets in segmented flow [18] were reported. Other measurement models such as four electrode arrangement [19,20], integration electrodes in a miniaturized detection system [21–23] were demonstrated. The influence of the factors such as operating frequency [24–26], detection cell geometry [27], wall thickness of capillary [28], and stray capacitance [29,30] on the response of C^4D was discussed.

To enhance the sensitivity of C^4D , a higher actuator voltage of 500 V [31], thinner insulating layer of 30 nm [32], end-to-end differential model [33] was reported. In our previous papers [34–36], a resonant C^4D (RC^4D) was proposed to improve the

sensitivity of C^4D in microchip electrophoresis and ion chromatography. In this work, the impedance parameters of C^4D under CE conditions were measured. The influence of solution conductivity and capillary dimension on the impedance of C^4D was investigated. The determination of amino acids by CE with end-to-end differential RC^4D (DRC^4D) model was performed. The limit of detection for 10 amino acids is in the range of 0.1–0.4 μM . Compared with C^4D , the sensitivity of DRC^4D enhances by a factor of 15–29 under our experimental conditions.

2. Experimental section

2.1. Chemicals and materials

Polyimide-coated fused silica capillaries (YN-025365, YN-050365, YN-075365, YN-100365) were the product of Yongnian Ruifeng Chromatographic Component Co. Ltd (Hebei, China). All chemicals were of analytical grade purity and used as received. Deionised Milli-Q water (Millipore, Bedford, MA, USA) was used throughout. Ten amino acids (Alanine, arginine, glutamic acid, glycine, leucine, lysine, phenylalanine, proline, threonine and valine) were purchased from Fluka. Hydroxyethylcellulose (HEC) was purchased from Sigma. Stock solutions of individual amino acids (1 mM) were prepared by water and acetonitrile 1:1 (v/v) and stored in the refrigerator at 4 °C. The mixture of 10 amino acids,

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which was made from the stock solutions by diluting with water and acetonitrile 1:1 (v/v), was used as the model sample in CE separation. All solutions were degassed by ultrasonication for 10 min and filtered through 0.22 μm nylon syringe filters (Shanghai Liangzheng Technology Co., China) prior to use.

2.2. Apparatus and setup

Chromatographic experiments were performed with a purpose-built CE system with DRC⁴D (Fig. 1). The separation voltage was provided by a high voltage power supply unit (DW-P303, Tianjing Wendong High Voltage Power Supply Co. Ltd., China). A polyimide-coated fused silica capillary (with inner diameter of 50 μm , with outer diameter of 365 μm , total length of 65 cm) was used for amino acid separation. Two C⁴Ds were fixed to the capillary at the distance of 10 cm from the near ends. The input and signal electrodes were prepared by silvered wire (with diameter of 0.1 mm) twisted tight on capillary. The electrode length was 2 mm and the gap between the input and signal electrodes was 0.6 mm. The C⁴D was mounted in a ground Faraday shielding box to minimize the leakage capacitance. The capillary between two shielding boxes was enveloped by a water bath at the controlled temperature of 25 °C. A purpose-built function generator was designed to provide an actuator voltage of 20 V (peak-to-peak) with frequency breadth less than 1 Hz and voltage stability better than 1 mV. The actuator voltage was applied to the series combination of 10 piezoelectric quartz crystal (PQC) resonators (200 kHz, Beijing Chenjin Quartz Crystal Manufactory, China) and C⁴D on the capillary. The circuitry on the pick-up side comprises a current-to-voltage converter, followed by rectification, low-pass filtering. Prior to chromatographic detection, the capillary was filled the running buffer and the operating frequency of the actuator was scanned. The frequency corresponding to the

maximum output signal was chosen as the operating frequency for RC⁴D. In the end-to-end differential measurement model, the preamplified signals from the upstream and downstream detectors are subtracted from each other. The resulting differential signal is postamplified and recorded by a chromatographic working station.

Each new capillary was activated by sequentially flowing (pressure-driven by a medicine syringe) 0.5 M solution of sodium hydroxide, deionised water, and running buffer for 20 min, respectively. The capillary was then equilibrated in the running buffer under a voltage of 25 kV for 20 min prior to sample injection. Sample was injected hydrostatically by elevating the sample vials to a height of 10 cm for 10 s. As two C⁴Ds were equipped at both ends of the capillary, sampled injection was performed by turning the whole equipment box around its rotary axis. Separation was taken place at +25 kV. Between each consecutive run, the capillary was flushed with deionised water followed by running buffer for 10 min each for reproducible results.

The impedance of C⁴D was measured in an impedance analyzer (Model 4294A, Agilent) at the constant laboratory temperature of 25 \pm 1 °C. To increase the signal-to-noise ratio in impedance measurement, a parallel arrangement of 10 C⁴Ds with the same electrode geometry was employed (Fig. 2). The impedance of a single C⁴D is 10 times of that of the C⁴D array, which was set in a grounded shielding box to minimize the stray capacitance. The contactless electrodes were fabricated from syringe cannulas with length of 10 mm. The gap between the electrodes was 2 mm. The test solution was injected into capillary array by a pressure-driven medicine syringe. The impedance was scanned three times (with 401 points in a scan) for each solution, the averaged values were reported. Capillary array with different inner diameter (25, 50, 75, 100 μm) was exchanged after a group measurements.

3. Results and discussion

3.1. Measurement of the impedance of C⁴D in capillary electrophoresis

Analysis of the impedance of C⁴D shows how the detector can be optimized. Fig. 3A presents an simplified equivalent circuit

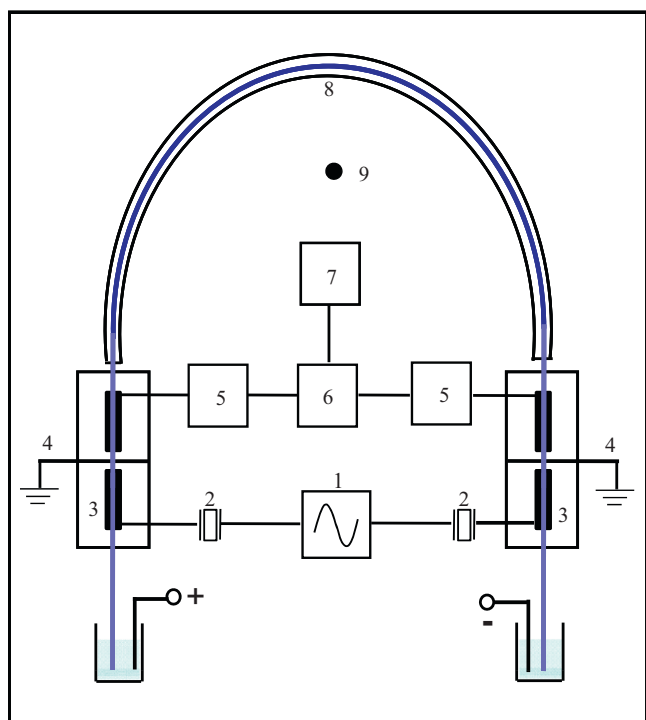


Fig. 1. Schematic drawing of end-to-end differential resonant C⁴D for capillary electrophoresis (not to scale). (1) function generator; (2) piezoelectric quartz crystal resonator array; (3) contactless electrode; (4) ground shielding box; (5) current detection circuitry; (6) differential detection circuitry; (7) chromatographic working station; (8) separation capillary; (9) rotary axis for hydrostatic sample injection.

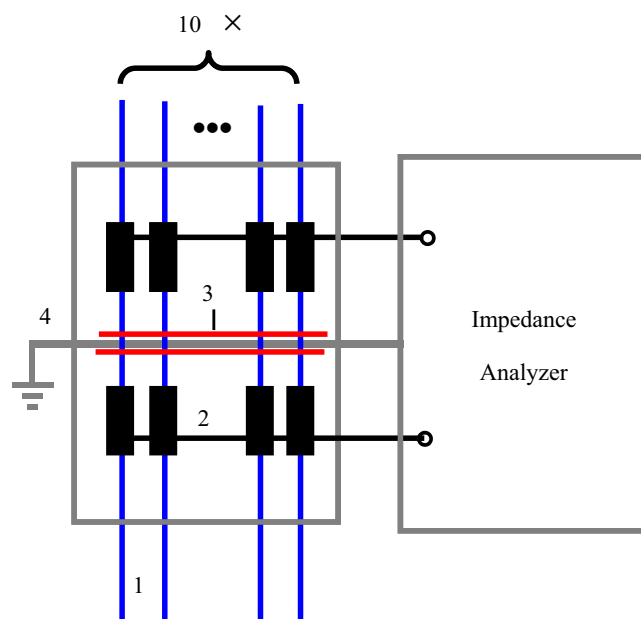


Fig. 2. Schematic drawing of C⁴D array for impedance measurement (not to scale). (1) capillary array; (2) contactless electrode array; (3) Teflon insulation film; (4) ground shielding box.

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