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- Enhanced gene delivery in porcine vasculature tissue following 1
- incorporation of adeno-associated virus nanoparticles into porous silicon microparticles
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ABSTRACT

There is an unmet clinical need to increase lung transplant successes, patient satisfaction and to improve mortal-23 ity rates. We offer the development of a nanovector-based solution that will reduce the incidence of lung ische- 24 mic reperfusion injury (IRI) leading to graft organ failure through the successful ex vivo treatment of the lung 25 prior to transplantation. The innovation is in the integrated application of our novel porous silicon (pSi) micro- 26 particles carrying adeno-associated virus (AAV) nanoparticles, and the use of our ex vivo lung perfusion/ventila-27 tion system for the modulation of pro-inflammatory cytokines initiated by ischemic pulmonary conditions prior 28 to organ transplant that often lead to complications. Gene delivery of anti-inflammatory agents to combat the in- 29 flammatory cascade may be a promising approach to prevent IRI following lung transplantation. The rationale for 30 the device is that the microparticle will deliver a large payload of virus to cells and serve to protect the AAV from 31 immune recognition. The microparticle-nanoparticle hybrid device was tested both in vitro on cell monolayers 32 and ex vivo using either porcine venous tissue or a pig lung transplantation model, which recapitulates pulmo-33 nary IRI that occurs clinically post-transplantation. Remarkably, loading AAV vectors into pSi microparticles in- 34 creases gene delivery to otherwise non-permissive endothelial cells. 35

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1. Introduction

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Acute lung injury (ALI) and its most severe manifestation, acute re-42 43 spiratory distress syndrome (ARDS), are clinical syndromes defined by acute hypoxemic respiratory failure and bilateral pulmonary infiltrates 44 consistent with edema. In-patient mortality is 38.5% for ALI, and 41.1% 45for ARDS [1]. Common causes of ALI/ARDS are sepsis, trauma, multiple 4647 blood transfusion, aspiration, and injury from toxic inhalation [1–3]. At this time, low tidal volume ventilation remains the only intervention 48 that affords mortality benefit. Therefore, clinical approaches based on 49 50interruption of pathways identified in the acute phase are of interest for the development of strategies that can significantly lower the cur-51 rent mortality rates. Typically, a patient's intrapulmonary inflammatory 5253response begins prior to the onset of clinically defined ALI and is most

54intense in the first 3 days after the onset of ALI/ARDS.

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Unlike most animal models for ALI that rely on the administration of 55 an insulting agent (toxins, O2, bacteria, etc.), we have developed a pig 56 lung transplantation model that is the reproduction of the lung 57 ischemia/reperfusion injury (IRI) that occurs clinically post-surgical 58 transplantation. A hybrid nanotechnology platform has been created 59 for the sustained expression of anti-inflammatory agents to combat 60 the inflammatory cascade. A "Trojan horse" [2,3] mesoporous silicon 61 (pSi) microparticle is envisioned to escort its nanovector payload to 62 inflammation-associated endothelium, where it is internalized and sub- 63 sequently releases the therapeutic nanoparticles [4,5]. Proven silicon 64 fabrication processes allow exquisite control over particle geometry 65 (dimensions from 100 nm and above) and porosity (pore size range 66 between 5-100 nm) to create particles with specific size, shape, 67 and surface treatments optimized for specific cargo and surface 68 functionalization [6,7].

Due to their efficient role as gene delivery vectors, a number of virus-70 es are currently being explored for therapeutic gene expression [8]. Be-71 cause of its lack of pathogenicity, adeno-associated virus (AAV) is one of 72 the most commonly investigated viral vectors. AAV can be used to deliv-73 er genes or RNAi [9]. Simple in structure, this virus is composed of a 74 25 nm protein capsid harboring a 4.7 kB single-stranded DNA genome. 75

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AAV is naturally present in a variety of hosts, including humans, but not
pathogenic. To date, at least 12 serotypes have been isolated [10],
with the most commonly used serotype for gene therapy being AAV2.
Approximately 80% of the population has been exposed to this
serotype [11].

We hypothesize that our "Trojan Horse" design concept will provide 81 several important benefits to the immunotherapy approach. First, and 82 83 the focus of this study, the pSi platform will enable the delivery of 84 large payloads of VNPs into the endothelium, effectively increasing the 85 local dosage of therapeutic genes in the target cells resulting in im-86 proved efficacy. Second, the pSi microparticle will shield VNPs from host anti-virus responses, such as neutralization by preexisting antibod-87 ies. Furthermore, the microparticle provides a facile means of combin-88 89 ing multiple types of VNPs, each carrying a different transgene, and ensuring that combinations of genes get delivered to the same target 90 91 cell. Additionally, other bioactive moieties can be incorporated into the microdevice, further enhancing the immunomodulatory capabilities 92 93 of the vector. Lastly, the pSi microparticle can be designed to allow for controlled release of VNPs, consequently resulting in the sustained ex-94 pression of anti-inflammatory factors. 95

96 Integrating the use of normothermic ex vivo circulation in conjunc-97 tion with our novel "Trojan Horse" approach presents an exciting poten-98 tial technique to effectively reduce the risks associated with systemic delivery by bypassing the negative effects of filter organ clearance and 99 by minimizing the interaction with circulating immune-competent 100 cells. The ex vivo model provides the most promising setup: an isolated 101 viable organ model with normal metabolic functions. The major draw-102103 back of all the present perfusion systems is that their use is based on the concept of preserving the organ at approximately 4 °C by using a 104 cold flushing solution. The lowering of the cellular metabolic rate is nec-105essary to maintain organ viability. This is an obvious impediment for the 106 107 delivery of any agents to the allograft, as all the crucial phases depend 108 on metabolic processes. Improved technologies, such as the development of improved pumps and improved ventilators and the develop-109ment of a lung-specific perfusion solution (Steen solution), which has 110 an optimized composition and oncotic pressure, led to the rebirth of 111 the notion of ex vivo perfusion. The lung has some very peculiar charac-112 113 teristics, as it consists mainly of elastic tissue with a low metabolic requirement. Normally the alveolo-capillary membrane receives its 114 nutrition mostly by direct diffusion and it is possible to sustain the 115 lung tissue by delivering oxygen through the trachea, via mechanical 116 117 ventilation. Therefore, there is no need to perfuse with a cold solution to lower the metabolic rate. The possibility of treating an entire isolated 118 organ, while circulating a normothermic solution and oxygenating 119 through an endotracheal tube creates the ideal milieu for effectively de-120 livering therapeutic agents ex vivo to address potential complications 121 122associated with lung transplant such as IRI.

In this study, we describe optimization of AAV2 loading into pSi microparticles and cell type specific expression of genes delivered by free or encapsulated AAV2. Delivery and expression of the pSi-AAV-GFP vectors *ex vivo* in vascular endothelium is presented as well as expression of the reporter gene in porcine pulmonary tissue following *ex vivo* vascular perfusion of the pSi-AAV2-GFP.

129 2. Materials and methods

130 2.1. Virus production

AAV2-GFP was produced using HEK293T cells and the triple trans-131 fection method [12]. Plasmids pXX6, pXX2, and pAAV-GFP were 132transfected into cells using polyethyleneimine (PEI). Virus was harvest-133 ed 72 h later and purified using density gradient ultracentrifugation. 134 Further purification was performed using a heparin affinity column 135(GE Healthcare) followed by dialysis into DPBS (+Mg/Ca). Virus con-136 centration was quantified using QPCR and primers against the CMV pro-137 138 moter contained within the DNA cassette and standards bearing the CMV promoter. Viral capsids were dissolved with 2 M NaOH at 56 $^\circ C_{139}$ for 30 min and then neutralized with 2 M HCl. $_{140}$

2.2. Silicon microparticle functionalization

Oxidized porous silicon discoidal microparticles with dimensions of 1000 nm \times 400 nm (pore size \sim 50–60 nm) were centrifuged to remove isopropanol and vacuum desiccated. Particles 144 were functionalized with –NH₂ (3-aminopropyl-triethoxysilane), 145 –CH₃ (methyltrimethoxysilane), –COOH (2-(carbomethoxy) ethyltrimethoxysilane), or –PEI (trimethoxysilylpropyl modified (polytrimethoxysilane)), obtained from Gelest. Dry particles were resuspended 148 in silanes diluted to 2% in 95% v/v isopropanol in water. Functionalization 149 occurred for 2 h at 35 °C with 1300 RPM shaking. Particles were then 150 rinsed three times with fresh isopropanol and vacuum desiccated in 151 preparation of loading. The surface charge of each particle type was determined by suspending the particles in phosphate buffer and using a Malvern Zetasizer to determine zeta potential.

2.3. Loading AAV2-GFP within functionalized particles

Microparticles were dried (2e8 particles) and then resuspended in 156 AAV2-GFP in DPBS (50 µl, ~1e12 vector genomes/ml). Loading was 157 allowed to occur for either 15 or 30 min at room temperature. After 158 this time particles were pelleted, rinsed twice with sterile water 159 (100 µl each rinse), and then resuspended in 50 µl water. Loading was 160 determined using QPCR. The same procedure was used as above, as 161 2 M NaOH dissolves silicon microparticles in addition to virus capsids. 162 The presence of dissolved particles was found to not interfere with the 163 PCR reaction (data not shown). 164

2.4. Nanoscale evaluation of pSi surface modification and VNP loading 165

Atomic force microscopy (AFM) was used to image surface topography of oxidized or silane-modified (2% APTES; 2 h incubation) pSi microparticles. Height and peak force measurements of particles were made using a Bruker Dimension ICON AFM. PeakForce tapping was performed using ScanAsyst to adjust imaging parameters and a model ScanAsyst Air probe made of silicon nitride with a silicon tip, and a spring constant of 0.4 N/m, 1 Hz scan rate. Analysis of AAV adhesion to a silicon wafer was performed using a Bruker Multimode AFM.

2.5. Cell culture

Gene delivery efficiency was determined in three cell lines: HeLa, 175 HEK293T, and HMVEC (human microvascular endothelial cells). All 176 cells were cultured at 37 °C with 5% CO₂. HeLa and HEK293T cells 177 were maintained in DMEM with 10% FBS and 1% penicillin/streptomycin. HMVECs were cultured in EGM (Lonza). 179

2.6. Determination of gene delivery using flow cytometry 180

Cells were plated in 24 well plates such that they would be 75% confluent after 24 h. Transduction studies were performed by removing 182 media and replacing with 220 µl fresh media. Either free AAV2-GFP or 183 particle-loaded AAV2-GFP (each surface chemistry) was added to the 184 media at a virus MOI of 1,000. After 3 h the media was removed and replaced with 1 ml fresh media. Cells were then cultured for 3 days before 186 harvesting for flow cytometry analysis of GFP expression. Analysis was 187 performed using a BD Fortessa using the FITC channel to detect GFP 188 expression. 189

2.7. Confocal imaging of gene expression

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HEK293T cells were seeded in 8 well chamber slides (BD) such that $_{191}$ they would be 75% confluent after 24 h. Media was removed and $_{192}$

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