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# Real time Raman imaging to understand dissolution performance of amorphous solid dispersions

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- 17 Intrinsic dissolution rate
- 18 Multi-variate curve resolution (MCR)

#### ABSTRACT

We have employed for the first time Raman spectroscopic imaging along with multi-variate curve resolution 19 (MCR) analysis to investigate in real time and *in-situ* the dissolution mechanisms that underpin amorphous 20 solid dispersions, with data being collected directly from the dosage form itself. We have also employed a 21 novel rotating disk dissolution rate (RDDR) methodology to track, through the use of high-performance liquid 22 chromatography (HPLC), the dissolution trends of both drug and polymer simultaneously in multi-component 23 systems. Two formulations of poorly water-soluble felodipine in a polymeric matrix of copovidone VA64 24 which have different drug loadings of 5% and 50% w/w were used as models with the aim of studying the effects 25 of increasing the amount of active ingredient on the dissolution performance. It was found that felodipine 26 and copovidone in the 5% dispersion dissolve with the same dissolution rate and that no Raman spectral changes 27 accompanied the dissolution, indicating that the two components dissolve as single entity, whose behaviour 28 is dominated by water-soluble copovidone. For the 50% drug-loaded dispersion, partial RDDR values of 29 both felodipine and copovidone were found to be extremely low. MCR Raman maps along with classical 30 Raman/X-ray powder diffraction (XRPD) characterisation revealed that after an initial loss of copovidone from 31 the extrudate the drug re-crystallises, pointing to a release dynamics dependent on the low water solubility 32 and high hydrophobicity of felodipine. Raman imaging revealed different rates of transition from amorphous 33 to crystalline felodipine at different locations within the dosage form.

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#### 1. Introduction

A high number of new chemical entities emerging from the drug development process show pharmacological activity, but at the same time are characterised by poor dissolution and solubility profiles [1]. As a result, there is a strong push to develop innovative formulations for the delivery of such compounds so that the desired oral bioavailability and pharmacological effects are achieved. An increasingly popular class of formulation is represented by amorphous solid dispersions, which are prepared by co-processing the drug and a water-soluble or water-swellable polymeric carrier, commonly *via* spray drying or hot melt extrusion [2,3]. The resultant dispersion, as widely demonstrated for several poorly soluble compounds, has an improved dissolution profile and consequently bioavailability compared to the pure drug [4]. This is attributed to the fact that the drug within the dispersion exists in the amorphous form, which gives a higher dissolution rate than

the corresponding crystalline form, and also due to the presence of the 55 water-soluble polymer [5,6].

One of the key challenges for deploying amorphous solid dispersions 57 in real-world formulations is the understanding of the dissolution per- 58 formance. Although this is very relevant, due to the fact that the dissolution performance limits the in vivo efficacy, relatively few studies 60 have been conducted to investigate the dissolution mechanisms that 61 underpin these systems. As reported by Craig, [7] the dissolution mech- 62 anism of amorphous solid dispersions is characterised by a number of 63 critical processes, which primarily depend on the chemical nature of 64 the components and on the drug-to-polymer ratio. In relation to these 65 parameters, Craig classified the drug release from amorphous solid dis- 66 persions as polymer-controlled or drug-controlled. It has been demon- 67 strated that the re-crystallisation of the drug either in the solid state 68 or after precipitation in solution, [8,9] the formation of nano- and 69 micro-particles during the dissolution [10] and also the behaviour of 70 the polymer itself, [11] strongly contribute to the final dissolution 71 performance. Amorphous solid dispersion dissolution mechanisms are 72 extremely difficult to de-convolute due to several processes occurring 73 simultaneously.

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Classical methods of investigating drug release such as the use of USP dissolution apparatuses [12] do not offer any chemical or spatially-resolved information on potential changes of the solid form (e.g. from amorphous to crystalline, polymorphic transformations or formation of hydrate states) during the dissolution, since the data are collected from the solution, rather than directly from the solid dosage form itself. Given the limitations of the conventional dissolution apparatuses, innovative methods have been developed in an attempt to provide a more complete picture of the drug release. Such methods have included mid-IR, [13,14] near-IR [15,16] and magnetic resonance imaging (MRI) [8,17]. Mid-IR and near-IR provide chemical information, but also have a significant drawback; they are very sensitive to water which clearly limits the use of these techniques in aqueous environments. MRI is attractive as it can offer three-dimensional information, however it provides little chemical specificity.

Raman spectroscopy, theoretically, offers advantages/complementarities compared to these techniques. It provides chemically detailed and two-dimensional spatial information ('hyper-spectral data', one spectrum per pixel) and is able to readily differentiate between amorphous and crystalline solid forms [18,19]. These properties are significant since the chemical and physical forms of the drug can change during the course of the dissolution test [8,9,14]. Moreover, with respect to mid-IR and near-IR, Raman spectroscopy is relatively insensitive to water [20]. Raman spectroscopy is therefore an appropriate technique to investigate how the solid state properties of the drug affect its release and for this reason was employed in this work to understand the performance of amorphous solid dispersions during dissolution in aqueous media.

An amorphous solid dispersion of felodipine, the active ingredient, in a polymeric matrix of copovidone VA64, was used as model formulation. Felodipine is an antihypertensive drug, characterised by high permeability and low water solubility (lower than 0.5 mg/lt) [21]. Copovidone VA64 is a highly water-soluble polymer (solubility higher than 100 mg/lt), [22] recognised as a chemical analogue of polyvinylpyrrolidone (PVP). In previous studies, PVP and copovidone VA64 have been successfully used to prepare one-phase amorphous felodipine binary mixtures over a range of composition (0-70% drug loading), showing the ability to inhibit re-crystallisation and to increase the dissolution rate of poorly soluble felodipine [23-27]. The physical mixture of crystalline felodipine and copovidone VA64 has been shown instead to have a small increase in dissolution rate when compared to pure crystalline felodipine, further demonstrating how the physical state of the active ingredient (e.g. amorphous vs. crystalline) affects the whole dissolution performance regardless the presence or absence of the polymer in the formulation [8]. This work follows on from the recent paper by Langham et al., where the use of a combined spectrophotometric and magnetic resonance imaging technique to investigate the dissolution mechanisms of felodipine-copovidone spray-dried amorphous solid dispersions was described [8]. It was found that the dissolution behaviour of the high drug-loaded amorphous solid dispersions is governed by the low aqueous solubility of felodipine and by the re-crystallisation (confirmed by off-line XRPD) of the drug.

In the present work, we investigated formulations which have different drug loadings (5% and 50% w/w), with the aim of studying the effects of increasing the amount of active ingredient on the dissolution performance. Two different approaches were employed to probe the dissolution performance of amorphous solid dispersions. The first used Raman spectroscopy and the second uses a rotating disk dissolution rate (RDDR) test. Our RDDR method, with respect to conventional intrinsic dissolution rate (IDR) test described in the USP and in the European Pharmacopoeia, [12,28] employs HPLC to separate the drug from the polymer and ultimately allows us to measure the performance in aqueous media of multi-component systems.

The aim of this work is to investigate whether Raman spectroscopy provides additional chemical and spatial information regarding the dissolution mechanisms that underpin amorphous solid dispersions, 141 used in conjunction with RDDR dissolution test.

#### 2. Materials and methods

#### 2.1. Preparation of amorphous felodipine and extrudate solid dispersions

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The amorphous form of felodipine was obtained by heating the drug 145 as received (AstraZeneca, Macclesfield, United Kingdom) in the oven to 146 160 °C and, after melting, cooling back to room temperature. Visual in- 14703 spection and Raman spectroscopy confirmed the formation of the amorphous form and the absence of crystalline material within the detection 149 limits (ca. 0.5% or better). 5% and 50% drug-loaded amorphous solid dispersions of felodipine in copovidone (BASF, Ludwigshafen, Germany) 151 were prepared using a co-rotating twin-screw extruder (Thermo Scien- 152 tific HAAKE MiniLab II). Felodipine and copovidone were pre-mixed for 153 20 min in a Turbula T2F mixer (Willy A. Bachofen AG Mashinefabrik). 154 The extruder was manually fed with the physical mixture. The screw 155 speed was set to 150 rpm and the temperature to 160 °C. The extrudates 156 with spaghetti shape were then collected, cooled to room temperature 157 and manually milled to fine powder. X-ray powder diffraction con- 158 firmed the formation of the amorphous solid dispersion and the absence 159 of crystalline material (Figure S1).

#### 2.2. X-ray powder diffraction (XRPD)

XRPD patterns were obtained using a PANalytical CubiX PRO diffrac- 162 tometer. Samples were exposed to Cu-K $\alpha$  radiation at a voltage of 45 kV  $_{163}$ and a current of 40 mA. After being smeared onto the holder, samples 164 were scanned from  $2^{\circ}$  to  $40^{\circ}$   $2\theta$ , with a step size of  $0.02^{\circ}$   $2\theta$ .

#### 2.3. Rotating disk dissolution rate (RDDR)

RDDR testing was carried on using the rotating disk system, also 167 known as 'Woods apparatus'. The die cavity has a diameter of 8 mm 168 with subsequent exposed sample surface area of 0.5 cm<sup>2</sup>. About 169 250 mg of extrudate powder was compressed under a compression 170 force of 2000 kg using a manual IR press (Specac). The experiment 171 was performed in a Sotax AT7 semi-automated dissolution bath 172 equipped with an automated sample collector. Compressed discs were 173 immersed in 500 ml of deionised water at 37 °C ( $\pm 0.5$ ), at 100 rpm ro- 174 tational speed. The automated sample collector removed aliquots of 175 sample from the dissolution medium at regular time intervals over 176 120 min. The samples were then analysed by reverse phase high performance liquid chromatography (RP-HPLC). Both the experiments for 5 178 and 50% extrudates were performed in triplicate. HPLC analysis was car- 179 ried out using a Agilent 1100 with UV detection at 210 nm, equipped 180 with an Agilent PLRP-S 300 Å 3 µm 50 mm column (polystyrene/ 181 divinylbenzene stationary phase). The flow rate was set to 1.0 ml/min 182 and the temperature of the column was kept at 40 °C. A linear gradient 183 elution was used starting at 40% acetonitrile/60% deionised water and 184 ending at 90% acetonitrile/10% deionised water after 3.5 min, with chromatograms collected up to 5 min. A series of standard solutions of 186 felodipine and copovidone were prepared to generate a calibration 187 curve covering the concentration range of dissolved sample. The partial 188 RDDR of both drug and polymer was calculated using linear regression 189 analysis [12,28]. The partial RDDR of the substance tested was determined from the slope of the regression line. 191

#### 2.4. Raman spectroscopy

We investigated the dissolution performance of compressed 193 extrudate powder. Spherical compacts with a diameter of 5 mm and a 194 weight of 50 mg were prepared with a manual IR press (Specac) using 195 a compression force of ca. 20 kN. The dissolution test was performed 196 in a flow cell, which is illustrated in Figure S2. Deionised water was 197

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