



Contents lists available at ScienceDirect

## Advanced Drug Delivery Reviews

journal homepage: [www.elsevier.com/locate/addr](http://www.elsevier.com/locate/addr)Collagen interactions: Drug design and delivery<sup>☆</sup>Bo An<sup>a</sup>, Yu-Shan Lin<sup>b</sup>, Barbara Brodsky<sup>a,\*</sup><sup>a</sup> Department of Biomedical Engineering, Tufts University, Medford, MA 02155, USA<sup>b</sup> Department of Chemistry, Tufts University, Medford, MA 02155, USA

## ARTICLE INFO

## Article history:

Received 8 September 2015

Received in revised form 19 November 2015

Accepted 20 November 2015

Available online xxxx

## Keywords:

Collagen

Triple helix

Peptide

Recombinant collagen

Interaction

Targeting

Drug delivery

Crystallography

Extracellular matrix

## ABSTRACT

Collagen is a major component in a wide range of drug delivery systems and biomaterial applications. Its basic physical and structural properties, together with its low immunogenicity and natural turnover, are keys to its biocompatibility and effectiveness. In addition to its material properties, the collagen triple-helix interacts with a large number of molecules that trigger biological events. Collagen interactions with cell surface receptors regulate many cellular processes, while interactions with other ECM components are critical for matrix structure and remodeling. Collagen also interacts with enzymes involved in its biosynthesis and degradation, including matrix metalloproteinases. Over the past decade, much information has been gained about the nature and specificity of collagen interactions with its partners. These studies have defined collagen sequences responsible for binding and the high-resolution structures of triple-helical peptides bound to its natural binding partners. Strategies to target collagen interactions are already being developed, including the use of monoclonal antibodies to interfere with collagen fibril formation and the use of triple-helical peptides to direct liposomes to melanoma cells. The molecular information about collagen interactions will further serve as a foundation for computational studies to design small molecules that can interfere with specific interactions or target tumor cells. Intelligent control of collagen biological interactions within a material context will expand the effectiveness of collagen-based drug delivery.

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<sup>☆</sup> This review is part of the Advanced Drug Delivery Reviews theme issue on "ECM and ECM-like materials".

\* Corresponding author.

E-mail address: [Barbara.Brodsky@tufts.edu](mailto:Barbara.Brodsky@tufts.edu) (B. Brodsky).

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## 75 1. Background

76 Collagen, the most abundant protein in the human body, has a long  
77 history as a natural material for diverse biomedical applications, includ-  
78 ing drug delivery [1,2]. Animal tissues rich in type I collagen are impor-  
79 tant sources of leather, cosmetic and gelatin products, in addition to  
80 biomedical devices and implants. From a physical perspective, collagen  
81 forms a rod-like triple-helix which self-associates to form a staggered  
82 array in D-periodic fibrils. The fibrils are cross-linked to provide me-  
83 chanical strength and integrity to the extracellular matrix, and the dis-  
84 tribution of fibril diameters, as well as the degree of cross-linking,  
85 strongly influence the tensile strength and elasticity of tissues. Extracted  
86 collagen molecules or fibers can form hydrogels, films or sponges that  
87 can be used as hemostatic pads, wound dressings, grafts and scaffolds  
88 for surgery and tissue engineering [3–6]. A better understanding of  
89 the interactions between collagen and its environment would enhance  
90 its widespread utility in health-related products.

91 In addition to its material properties, there has been increasing ap-  
92 preciation of the biological importance of collagen in cell signaling and  
93 regulation of extracellular matrix (ECM) function. The collagen triple-  
94 helix interacts with a large number of molecules that trigger biological  
95 events. Collagen interactions with cell surface receptors regulate many  
96 cellular process including adhesion, proliferation and migration [7],  
97 while interactions with other ECM components are critical for matrix  
98 structure and remodeling. In addition, the tight winding of its triple-  
99 helix structure makes collagen largely non-immunogenic, resulting in  
100 excellent biocompatibility of collagen-derived materials. Details about  
101 the immune response to native and denatured collagen are discussed  
102 in several reviews [1,8]. Another important property of collagen-based  
103 materials is their natural degradation in the body. Collagens typically  
104 have a long lifetime, but a regulated breakdown is necessary during tis-  
105 sue turnover, remodeling and wound healing. The triple-helix structure  
106 is resistant to common proteases, but members of the matrix metallo-  
107 proteinase (MMP) family can cleave native and denatured collagen at  
108 specific sites, leading to eventual breakdown of collagenous biomateri-  
109 als in the body. Over the past decade, much information has been  
110 gained about the interactions of collagen with cell surface receptors,  
111 other ECM components and enzymes such as MMPs. Knowledge of  
112 these interactions allows for the possibility of new approaches in drug  
113 **Q3** discovery, targeting and delivery.

114 The combination of its natural hierarchical physical structures and  
115 biological interactions makes collagen an attractive candidate for a  
116 wide range of biomedical applications, which have proved effective in  
117 many cases. There are a number of excellent review papers that have  
118 focused on advances in the use of collagen materials as drug delivery  
119 vehicles [9–12]. The biological signals present within every animal  
120 collagen molecule for cell receptor binding, degradation, and matrix  
121 organization means that collagen within every biomaterial and drug de-  
122 livery vehicle will naturally interact with its environment. This can lead  
123 to unintended consequences or to unregulated processes. The impor-  
124 tant progress in understanding the nature and specificity of collagen in-  
125 teractions which has taken place in recent years sets the stage for more

126 intentional, regulated biological activities within collagen-based mate-  
127 rials. This review will focus on collagen interactions with cell receptors,  
128 other ECM proteins and enzymes, and consider the implications of these  
129 interactions for directed drug delivery and designer biomaterials.

## 130 2. The collagen molecule: an interaction perspective

131 Proteins which contain a triple-helix domain and which play a struc-  
132 tural role in the ECM are classified as collagens. The human family of col-  
133 lagens currently includes 28 distinct genetic types, and may be broadly  
134 divided into fibrillar types and non-fibrillar collagens (see [13] for a re-  
135 cent review). The fibrillar types I, II and III form typical collagen fibrils  
136 with an axial periodicity of 67 nm and are the most abundant collagens.  
137 Different genetic types exhibit a tissue-specific distribution: type I in  
138 bone, skin, tendon, cornea; type II in cartilage and the vitreous; and  
139 type III, together with type I, in skin, blood vessels and more flexible tis-  
140 sues. Type I collagen is a heterotrimer consisting of two  $\alpha 1(I)$  chains and  
141 one  $\alpha 2(I)$  chain, and this most abundant collagen forms the basis of  
142 most biomaterial applications. Type II and III collagens show homology  
143 to the  $\alpha 1$  chain of type I collagen, but are homotrimers. The non-fibrillar  
144 collagens include type IV collagen, which forms network-like structures  
145 in basement membranes, as well as FACIT collagens and membrane-as-  
146 sociated collagens.

147 Fibrillar collagens extracted in bulk from tissues such as cow hide,  
148 pig intestines or fish skin represent the dominant collagen protein  
149 used for biomedical applications. To complement extracted animal col-  
150 lagens, the production of recombinant human collagen has been exten-  
151 sively explored [11] and significant advances have been made.  
152 Expression of recombinant human collagen in mammalian cell lines  
153 has led to the generation of constructs with variations in individual res-  
154 idues or in the organization of the D-periodic elements [14–16], but the  
155 small yields limit the use of such material in practical applications.  
156 Efforts are ongoing to produce human collagen in recombinant systems  
157 such as yeast, insect cells and plants [17,18]. The task of large-scale  
158 expression of stable and functional recombinant animal collagens  
159 is far from simple, in large part due to the requirement for post-  
160 translational proline hydroxylation for animal collagen stability. Recent  
161 findings of collagen-like proteins in bacteria suggest that these triple  
162 helix-forming proteins may represent alternative biosynthetic collagen  
163 materials that could enhance current collagen sources [19,20].

164 In this section, the nature of the triple-helix is considered as well as  
165 the features of the structure that direct interactions with other proteins.

### 166 2.1. Collagen structure

167 In the 1950s, fiber X-ray diffraction studies, together with amino  
168 acid composition/sequence data and model building, led to the proposal  
169 of a triple-helix as the molecular structure for collagen [21,22]. In this  
170 structure, three polyproline II-like polypeptide chains are supercoiled  
171 about a common axis. The close packing of the three chains near the  
172 central axis requires Gly as every third residue, generating the charac-  
173 teristic collagen (Gly-Xaa-Yaa)<sub>n</sub> repeating sequence. The Gly residues

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