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Research Paper

Influence of temperature and relative humidity conditions on the pan $\frac{7}{5}$ coating of hydroxypropyl cellulose molded capsules

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ABSTRACT

In a previous study, hydroxypropyl cellulose (HPC)-based capsular shells prepared by injection molding 31 and intended for pulsatile release were successfully coated with 10 mg/cm² Eudragit[®] L film. The suitabil-
ity of HPC capsules for the development of a colon delivery platform based on a time dependent approach 33 ity of HPC capsules for the development of a colon delivery platform based on a time dependent approach was demonstrated. In the present work, data logging devices (PyroButton[®]) were used to monitor the 34 microenvironmental conditions, i.e. temperature (T) and relative humidity (RH), during coating processes 35 performed under different spray rates (1.2, 2.5 and 5.5 g/min). As HPC-based capsules present special fea- 36 tures, a preliminary study was conducted on commercially available gelatin capsules for comparison pur- 37 poses. By means of PyroButton data-loggers it was possible to acquire information about the impact of 38 the effective T and RH conditions experienced by HPC substrates during the process on the technological 39 properties and release performance of the coated systems. The use of increasing spray rates seemed to 40 promote a tendency of the HPC shells to slightly swell at the beginning of the spraying process; moreover, 41 capsules coated under spray rates of 1.2 and 2.5 g/min showed the desired release performance, i.e. abil- 42 ity to withstand the acidic media followed by the pulsatile release expected for uncoated capsules. 43 Preliminary stability studies seemed to show that coating conditions might also influence the release per- 44 45
45 formance of the system upon storage.
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51 1. Introduction

 Film coating of solid dosage forms is frequently used in the pharmaceutical industry to fulfill several needs, either esthetic, stability-related or functional, e.g. modified-release dosage forms [\[1\]](#page--1-0). Pan coaters and fluid-bed systems are the most widely used apparatus to apply polymer coatings. Irrespective of the equipment employed, film coating involves the atomization of polymer solu-tions or dispersions followed by impingement of the atomized dro-

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<http://dx.doi.org/10.1016/j.ejpb.2015.11.021> 0939-6411/© 2015 Published by Elsevier B.V. plets onto the substrate surface and subsequent solvent 59 evaporation to form the film. $\qquad \qquad 60$

When aqueous polymeric suspensions are employed, coales-
61 cence of the discrete polymer spheres needs to take place. In gen- 62 eral, when dealing with aqueous dispersions the formation of a 63 continuous film and its adherence to the substrates strongly 64 depend on the rate of solvent evaporation, which is driven by the 65 thermodynamic conditions in the coating pan, mainly temperature 66 (T) and relative humidity (RH). Adjustments in processing param- 67 eters to achieve the same coating conditions are necessary also 68 in case of transfer to coating pans of different shapes and during 69 $scale-up [2].$ $scale-up [2].$ 70

Because T and RH play such a key role in film formation, the 71 monitoring of the actual microenvironment experienced by sub- 72 strates during their coating assumes essential importance. The 73 exhaust air temperature has been typically considered the moni- 74 toring parameter most representative of the conditions of cores 75 in the pan [\[3\]](#page--1-0). However, such macroscopic measurement captured 76 by sensors often placed far from the pan itself does not fully char-

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Abbreviations: HPC, hydroxypropyl cellulose; T, temperature; RH, relative humidity; SR, spray rate; P_f, PyroButton data-logger fixed in the exhaust air plenum; P_{b} , PyroButton data-logger placed in the tablets bed; T_{exh} , exhaust temperature read by the probe of the coating equipment; $t_{10\%}$, time to 10% drug release; $t_{90-10\%}$, time elapsed between 10% and 90% drug release.

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 acterize the actual conditions experienced by cores [\[4\].](#page--1-0) This limita- tion can be partially overcome by the use of infrared guns to mea- sure the T of the surface of the substrate bed during the process. However, the need for opening the pan door during the coating run, although for a short time, results in perturbations of the envi- ronmental conditions inside the coating pan. Moreover, no infor- mation about the RH can be obtained with either the probes coating equipment is equipped with or infrared guns. Hence, tradi- tional measurements cannot fully assess the coating process or the 87 relationship between the T and RH in the pan and the coating per- formance. Such limitation becomes a major issue when coating 89 substrates for which T and, in particular, RH have a strong impact 90 on the outcome of the process, e.g. gelatin capsules [\[5\]](#page--1-0). Only very 91 recently, PyroButton®, a tablet-size temperature/humidity data- logger, has been proposed to record the microenvironmental con- ditions in the pan coater during film application on solid tablet cores [\[6–10\].](#page--1-0) PyroButton data-loggers can be fixed in one location or allowed to move freely with the cores in the coating pan.

 In the present work, PyroButton data-loggers were used to monitor conditions in the pan during the enteric coating of novel 98 Chronocap^{M} capsules, in order to correlate T and RH with the phys- ical characteristics and release performance of coated systems. Chronocap^{M} is a capsule-shaped shell made of hydroxypropyl cel- lulose (HPC) prepared by injection molding and intended for delayed/pulsatile release of a variety of fill formulations, e.g. pow- ders, granules, pellets, and solid dispersions [\[11,12\]](#page--1-0). Prototypes filled with different preparations were shown to provide, both in-105 vitro and in-vivo, the liberation of the contained drug after a lag time, which was dependent on the shell composition and thickness [\[12,13\].](#page--1-0) One of the possible applications of delayed/pulsatile release dosage forms is colon targeting. Such a time-dependent approach to achieve colonic delivery relies on the relatively con-110 stant small intestinal transit time (SITT; $3 h \pm 1$ standard error) of 111 dosage forms [\[14–16\].](#page--1-0) The duration of residence in the stomach, however, is unpredictable and this variability can be overcome by the application of a gastroresistant film that dissolves in the small intestine upon the significant increase in the luminar pH. Accordingly, the Chronocap^{M} shell was considered as a substrate for the development of a time-based colonic delivery system [\[17\]](#page--1-0). Preliminary work showed feasibility for the Chronocap^M sys- tem to be coated with an aqueous suspension based on the Eudra-119 git[®] L enteric polymer and the achievement of the desired release performance. However, samples withdrawn from the coating pan at different time points during the process showed a slight increase in the shell wall thickness, probably due to the swelling of the HPC upon contact with the sprayed aqueous polymeric formulation. In 124 the present work, the ability of PyroButton devices to monitor the T and RH conditions experienced by the capsular cores during coat- ing processes was exploited to evaluate the impact of process con-127 ditions on the physico-technological characteristics and release performance of the coated systems. Commercially available gelatin capsules were considered for comparison purposes.

130 2. Materials and methods

131 2.1. Materials

132 The following materials were used: hydroxypropyl cellulose 133 (HPC), Klucel[®] LF (Eigenmann & Veronelli, Italy); polyethylene gly-134 col (PEG) 1500 (Clariant Masterbatches, Italy); acetaminophen 135 granules (APAP), Compap[™] Coarse L (Mallinckrodt, MO, USA); 136 Eudragit[®] L 30 D 55 (Evonik, Germany); triethyl citrate (TEC) 137 (Vertellus Specialties Inc., IN, USA); trifluoroacetic acid ¹³⁸ (Sigma–Aldrich, MO, USA); LC–MS grade methanol, OmniSolv

(EMD Millipore, MA, USA); HPLC grade water; and size 2 hard- 139 gelatin capsules (Capsugel, SC, USA). 140

2.2. Methods 141

2.2.1. Preparation of HPC capsule shells 142

A bench-top micromolding machine (BabyPlast 6/10P; Crono- 143 plast S.L., Spain; Rambaldi S.r.l., Italy) was loaded with a mixture 144 of Klucel[®] LF and PEG 1500 (90% and 10% w/w, respectively), pre- 145 pared in Turbula[®] (Type T2C; WAB, Switzerland). Before use, HPC 146 was dried in a ventilated oven for 24 h at 40 \degree C. Molded items of 147 $600 \mu m$ nominal thickness were prepared by a mold with two 148 interchangeable inserts for the manufacturing of matching caps 149 and bodies, as previously reported (Zema et al. $[12]$). The techno-
150 logical characteristics and release performance of these capsule 151 shells were evaluated after 7 days of storage at ambient conditions 152 $(24 \pm 2 \degree \text{C}/55 \pm 5\% \text{ RH})$. 153

2.2.2. Coating of capsule cores 154

2.2.2.1. Filling of capsule shells. Gelatin capsules (Capsugel, SC, USA) 155 and HPC-based capsules were manually filled with 150 mg of APAP 156 granules. Unlike gelatin capsules, HPC capsules did not require 157 sealing of the closing area prior to coating $[17]$ because of their 158 special locking mechanism $[12]$; hence, only gelatin capsules were 159 manually band sealed, using a 20% w/v gelatin aqueous solution 160 [\[18\]](#page--1-0). 161

2.2.2.2. Preparation of the coating suspension. Commercially avail-
162 able Eudragit® L 30 D 55 dispersion was diluted to decrease the 163 solid contents to 20% and plasticized with 20% w/w TEC (based 164 on the dry polymer weight). After 30 min stirring, the suspension 165 was filtered through a 0.3 mm sieve and maintained under stirring 166 during the coating process. The amount of suspension required for 167 each run in order to apply 10 mg/cm² of polymer on cores was cal-
168 culated based on the total surface area of each type of capsule. 169

2.2.2.3. Coating process and curing. Batches of 500 capsules were 170 coated in a LDCS-3 Hi-coater (Vector Corporation, IA, USA) 171 equipped with a 1.3 L perforated pan. Coating conditions for gela- 172 tin and HPC capsules were as follows: bed air temperature, 30° C; 173 air pressure, 12 psi (82,737 Pa); and pan speed, 15 rpm. The spray 174 rate (SR) was set at 1.2, 2.5 or 5.5 g/min. Samples sprayed for 1 min 175 and at increasing coating levels were withdrawn during each run 176 and replaced with marked placebos of the same capsule type to 177 maintain batch size. Coated capsules were cured in a ventilated 178 oven at 40 \degree C for 2 h. Testing was performed after 7 days of storage 179 at ambient conditions $(24 \pm 2 \degree C/55 \pm 5\degree R)$. 180

2.2.2.4. Temperature and relative humidity monitoring. PyroButton 181 data-loggers (PyroButton-TM, Opulus Ltd., Philadelphia, PA) were 182 used to record T and RH (21-CFR-11 compliant, 17×6 mm diame-
ter) (Fig. 1a and b). PyroButton devices were calibrated before use 184 ter) ([Fig. 1a](#page--1-0) and b). PyroButton devices were calibrated before use as described by Pandey et al. $[8]$ and programmed to record data 185 every 10 s. T and RH working ranges were $2-84$ °C and $3-99\%$, 186 and resolution was $0.5 \text{ }^{\circ}\text{C}$ and 0.64% , respectively. 187

One PyroButton[®] (P_f) was fixed in the exhaust air plenum by 188 means of double-sided tape, close to the probe where the exhaust 189 temperature (T_{exh}) is read. Two other data loggers (P_{b1} , P_{b2}) were 190 placed in the pan with the capsules during the pre-heating stage 191 and allowed to tumble freely with the capsule cores $(Fig. 1c)$ $(Fig. 1c)$ $(Fig. 1c)$. 192

After a 5 min preheating (from -5 to 0 min), capsules were 193
ated with 10 mg/cm² of polymer. Samples were withdrawn after 194 coated with 10 mg/cm² of polymer. Samples were withdrawn after 1 min from the start of the spraying and when theoretical 4, 8, and 195 10 mg of enteric polymer/cm² were applied. T and RH conditions 196 during each coating run were monitored starting from the preheat-
197 ing step to the end of the runs. Since all the operator's actions were 198

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