



ORIGINAL ARTICLE / *Head and neck imaging*

# Diffusion-weighted magnetic resonance imaging of extraocular muscles in patients with Grave's ophthalmopathy using turbo field echo with diffusion-sensitized driven-equilibrium preparation

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## KEYWORDS

Diffusion-weighted imaging;  
Apparent diffusion coefficient;  
Orbit;  
Thyroid associated ophthalmopathy;  
Graves' disease

## Abstract

**Purpose:** The purpose of this study was to correlate diffusivity of extraocular muscles, measured by three-dimensional turbo field echo (3DTFE) magnetic resonance (MR) imaging using diffusion-sensitized driven-equilibrium preparation, with their size and activity in patients with Grave's ophthalmopathy.

**Materials and methods:** Twenty-three patients with Grave's ophthalmopathy were included. There were 17 women and 6 men with a mean age of  $55.8 \pm 12.6$  (SD) years (range: 26–83 years). 3DTFE with diffusion-sensitized driven-equilibrium MR images were obtained with b-values of 0 and  $500 \text{ s/mm}^2$ . The apparent diffusion coefficient (ADC) of extraocular muscles was measured on coronal reformatted MR images. Signal intensities of extraocular muscles on conventional MR images were compared to those of normal-appearing white matter, and cross-sectional areas of the muscles were also measured. The clinical activity score was also evaluated. Statistical analyses were performed with Pearson correlation and Mann-Whitney *U* tests.

**Results:** On 3DTFE with diffusion-sensitized driven-equilibrium preparation, the mean ADC of the extraocular muscles was  $2.23 \pm 0.37$  (SD)  $\times 10^{-3} \text{ mm}^2/\text{s}$  (range:  $1.70 \times 10^{-3}$ – $3.11 \times 10^{-3} \text{ mm}^2/\text{s}$ ). There was a statistically significant moderate correlation

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between ADC and the size of the muscles ( $r=0.61$ ). There were no statistically significant correlations between ADC and signal intensity on conventional MR and the clinical activity score.

**Conclusion:** 3DTE with diffusion-sensitized driven-equilibrium preparation technique allows quantifying diffusivity of extraocular muscles in patients with Grave's ophthalmopathy. The diffusivity of the extraocular muscles on 3DTE with diffusion-sensitized driven-equilibrium preparation MR images moderately correlates with their size.

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## Introduction

Grave's ophthalmopathy is an autoimmune disorder of the orbit that is clinically symptomatic in 25–50% of patients with Graves' disease [1–4]. Patients with Grave's ophthalmopathy often experience highly incapacitating symptoms such as severe ocular pain and diplopia [5]. Previous studies have shown that computed tomography of the orbit could provide information on fat and muscle enlargement, which can be useful for diagnosing Grave's ophthalmopathy [5–11]. Other studies using magnetic resonance (MR) imaging revealed that the extraocular muscles of patients with active disease had a higher signal intensity ratio on T2-weighted and postcontrast T1-weighted MR images than those with inactive disease [6–12].

Diffusion-weighted (DW) MR imaging is widely used to diagnose tumors, inflammation, and vascular disease in both intracranial and extracranial lesions [5,13–22]. Previous studies also revealed the efficacy of DW MR imaging to evaluate orbital lesions including orbital tumors [16,18,20,21,23], IgG4-related disease [16], endophthalmitis [13], and optic nerve lesions [14]. However, it is sometimes difficult to evaluate intraorbital structures with echo planar imaging, which is the most common imaging technique for DW MR imaging. A previous study with echo planar DW MR imaging revealed its efficacy in assessing the activity of Grave's ophthalmopathy but found unsatisfactory image quality [5].

Compared to echo planar DW imaging, three-dimensional turbo field echo (3DTE) with diffusion-sensitized driven-equilibrium preparation can produce images with higher spatial resolution and fewer susceptibility artifacts [15–20]. 3DTE with diffusion-sensitized driven-equilibrium preparation minimizes image distortion while reducing B0 and B1 inhomogeneity and eddy current effects [24]. It was used to assess cholesteatoma [15], pituitary gland [17,19], and orbital tumors [16,18,20]. However, to date no studies have evaluated 3DTE with diffusion-sensitized driven-equilibrium preparation in Grave's ophthalmopathy.

The purpose of this study was to compare diffusivity of extraocular muscles, measured by 3DTE MR imaging with diffusion-sensitized driven-equilibrium preparation, with their size and activity in patients with Grave's ophthalmopathy.

## Methods

This retrospective study was approved by our institutional review boards, and written informed consent was waived.

## Patients

Twenty-three consecutive patients with Grave's ophthalmopathy who underwent 3DTE with diffusion-sensitized driven-equilibrium preparation MR imaging examination between January 2011 and February 2014 at our institution were studied. There were 17 women and 6 men with a mean age of  $55.8 \pm 12.6$  (SD) years (range: 26–83 years). All patients were diagnosed with Graves' disease. The previous treatments before MR imaging for hyperthyroidism in these 23 patients were as follows: none ( $n=12$ ; 12/23; 52.2%), potassium iodine ( $n=6$ ; 6/23; 26.1%), 1-methyl-2-mercaptoimidazole ( $n=6$ ; 6/23; 26.1%), radiation ( $n=2$ ; 2/23; 8.7%) and surgery ( $n=1$ ; 1/23; 4.3%). Two patients (2/23=8.7%) had previously received steroid for Grave's ophthalmopathy. The clinical activity score, which includes spontaneous retrobulbar pain, pain on attempted up- or down gaze, redness of the eyelids, redness of the conjunctiva, swelling of the eyelids, inflammation of the caruncle and/or plica, and conjunctival edema, were assessed by the referring clinicians [3]. A clinical activity score more than 3 indicated active Grave's ophthalmopathy [3].

## Imaging technique

All patients underwent MR imaging with a 3.0-T system (Achieva TX<sup>®</sup>, Philips, Best, The Netherlands) with an 8-channel head coil. The details of the 3DTE with diffusion-sensitized driven-equilibrium preparation are described elsewhere [15–20]. Briefly, it has two distinct components: the diffusion-sensitized driven-equilibrium preparation, and the segmented 3DTE data acquisition [24]. Adiabatic refocusing pulses and additional gradients inserted in front of the sequence were used to reduce the sensitivity to B0 and B1 inhomogeneity as well as eddy current effects [24]. Data acquisition using 3DTE was performed immediately after the diffusion-sensitized driven-equilibrium preparation.

To eliminate T1 effects in the acquired signal by 3DTE, we used a phase-cycling scheme. For the 3DTE with

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