

Global and Regional Right Ventricular Function Assessed by Novel Three-Dimensional Speckle-Tracking Echocardiography

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Background: Accurate assessment of global and regional right ventricular (RV) systolic function is challenging. The aims of this study were to confirm the reliability and feasibility of a three-dimensional (3D) speckle-tracking echocardiography (STE) system, using comparison with cardiac magnetic resonance imaging (CMR), and to assess the contribution of regional RV function to global function.

Methods: In a retrospective, cross-sectional study setting, RV volumetric data were studied in 106 patients who were referred for both CMR and 3D echocardiography within 1 month. Three-dimensional STE-derived area strain, longitudinal strain, and circumferential strain were assessed as global, inlet, outflow, apical, and septal segments.

Results: Seventy-five patients (70%) had adequate 3D echocardiographic data. RV measurements derived from 3D STE and CMR were closely related (RV end-diastolic volume, $R^2 = 0.84$; RV end-systolic volume, $R^2 = 0.83$; RV ejection fraction [RVEF], $R^2 = 0.70$; $P < .001$ for all). RVEF and RV end-diastolic volume from 3D STE were slightly but significantly smaller than CMR values (mean differences, -2% and -10 mL for RVEF and RV end-diastolic volume, respectively). Among conventional echocardiographic parameters for RV function (tricuspid annular plane systolic excursion, fractional area change, S' of the tricuspid annulus, RV free wall two-dimensional longitudinal strain), only fractional area change was significantly related to RVEF ($r = 0.34$, $P = .003$). Among segmental 3D strain variables, inlet area strain ($r = -0.56$, $P < .001$) and outflow circumferential strain ($r = -0.42$, $P < .001$) were independent factors associated with CMR-derived RVEF.

Conclusions: RV volume and RVEF determined by 3D STE were comparable with CMR measurements. Regional RV wall motion showed that heterogeneous segmental deformations affect global RV function differently; specifically, inlet area strain and outflow circumferential strain were significant factors associated with RVEF in patients with underlying heart diseases. (J Am Soc Echocardiogr 2017; ■: ■-■.)

Keywords: Three-dimensional echocardiography, Right ventricle, Cardiac function, Cardiac volume, Speckle-tracking, Myocardial strain

Right ventricular (RV) systolic dysfunction, especially RV ejection fraction (RVEF), is crucial in the management of patients with heart diseases, including heart failure,^{1,2} pulmonary arterial hypertension,³ and structural heart disease.⁴ Cardiac magnetic resonance imaging (CMR)

remains the gold-standard imaging tool for assessing RV volume and RVEF.

Three-dimensional (3D) echocardiographic imaging of the right ventricle has a theoretical advantage over the two-dimensional (2D) approach because 3D imaging is not affected by the through-plane phenomenon and can provide real information on volume and wall deformation with no assumptions regarding the complex RV shape. Several studies have reported comparisons between 3D echocardiography and CMR on RVEF and RV volume measurements.⁵⁻¹⁰ Recently, we developed novel RV 3D speckle-tracking echocardiography (STE) software validated using open-chest animal heart models with ultrasonic crystal implantations.¹¹ This novel RV 3D speckle-tracking software provides three separate RV directional strain measurements, including global longitudinal, circumferential, and area strain and regional inflow, apex, and outflow functions. The advantage of this new software is that it enables measurements of regional strain in the inflow, outflow, and apical portions of the right ventricle,^{12,13} which is different from that of the left ventricle.

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Conflicts of Interest: None.

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Abbreviations

2D = Two-dimensional
3D = Three-dimensional
BNP = Brain natriuretic peptide
CMR = Cardiac magnetic resonance imaging
RV = Right ventricular
RVEDV = Right ventricular end-diastolic volume
RVEF = Right ventricular ejection fraction
RVESV = Right ventricular end-systolic volume
RVOT = Right ventricular outflow tract
STE = Speckle-tracking echocardiography
TAPSE = Tricuspid annular plane systolic excursion
TOF = Tetralogy of Fallot

In this study, we sought to investigate several hypotheses: that this new 3D STE software specifically developed for the right ventricle would provide accurate quantitative assessment of RV end-diastolic volume (RVEDV), RV end-systolic volume (RVESV), and RVEF in a wide range of clinical entities, compared with CMR-derived measurements; that compared with conventional 2D echocardiographic indices, regional 3D RV strain would more strongly relate to CMR-derived RVEF; and that regional longitudinal, circumferential, and area strain would contribute differently to CMR-derived RVEF, reflecting intrinsic or acquired functional heterogeneity of the RV wall.

METHODS**Study Population**

We included 106 consecutive adult patients referred for clinically indicated CMR and echocardiography at Tsukuba University Hospital between May 2012 and April 2016 in a retrospective study setting. Transthoracic 3D echocardiography, focused on the right ventricle, was performed within 1 month of CMR. Serum brain natriuretic peptide (BNP) level within 1 month of CMR was measured. The study was approved by a local institutional review committee, and all subjects provided informed consent.

Conventional Echocardiography and 2D Strain

Echocardiographic examinations were performed with an ARTIDA ultrasound system (Toshiba Medical Systems, Tochigi, Japan). A 5-MHz transducer was used for conventional 2D echocardiography. Our echocardiography laboratory is maintained according to guidelines established by the Japanese Society of Echocardiography.¹⁴ Left ventricular volume and ejection fraction were measured using the modified Simpson rule.¹⁵ RV diameter and function were also measured using a standard method¹⁵ that assesses basal RV linear dimension, midcavity RV linear dimension, fractional area change, tricuspid annular plane systolic excursion (TAPSE), and peak systolic velocity of the tricuspid annulus (*S'*) using a tissue Doppler method. Furthermore, 2D speckle-tracking for RV free wall longitudinal contraction was performed using an RV-focused four-chamber view (2D Wall Motion Tracking; Toshiba Medical Systems).

Three-Dimensional RV Echocardiographic Acquisition

Full-volume electrocardiographically gated 3D RV images with six subvolumes were acquired using an appropriate duration of breath holding with a matrix-array 3D transducer. Echocardiographers were trained to obtain 3D images of the entire right ventricle, including the RV inlet, apex, and outflow, using a dedicated bed with an adjustable cut-out section located at the left chest area for

optimal probe access when obtaining high lateral apical views. The size of the ultrasonic scanning angle was set as small as possible to obtain a high temporal resolution of >20 volumes/sec. Data were stored and transferred to a computer (Inspiron 1300; Dell, Round Rock, TX) for offline analysis. RV 3D speckle-tracking echocardiographic images were analyzed using prototype software for dedicated RV assessment (Toshiba Medical Systems).

Three-Dimensional Wall Motion Tracking Algorithm for the Right Ventricle

Details of the 3D wall motion tracking algorithm for the right ventricle were reported previously.⁷ Five cross-sectional images were obtained: a four-chamber RV inlet-to-apex view, coronal apex-to-outflow view, and three axial views for the tricuspid annular plane, mid-RV level, and apical level, respectively (Figure 1, top). The end-diastolic frame was chosen at the beginning of the QRS complex of the electrocardiographic monitoring signal. Endocardial borders were traced manually in the coronal plane and the three axial planes of the end-diastolic frame. RV trabeculations and papillary muscles were included in the intraventricular blood volume. For anatomically faithful segmentation, the attachment sites of the moderator band in the ventricular septum and anterior papillary muscle in the free wall, which are the landmarks that divide the inlet, outflow, and apex segments, can be adjusted manually. The software automatically tracks the voxel pattern of the speckles frame by frame in 3D space (Figure 1, bottom). Ultimately, the software produces a complete data set comprising RVEDV, RVESV, RVEF, longitudinal strain, circumferential strain, and area strain (Figure 2). Longitudinal strain was defined as the percentage change in regional length in the direction of the longitudinal axis of the endocardium, circumferential strain was defined as the percentage change in regional circumference of the endocardium, and area strain was defined as the percentage change of the regional area of the endocardium,¹⁶ which can be regarded as the product of both longitudinal strain and circumferential strain. Manual correction of the endocardial border was prohibited after tracking was completed. Each segmental data set could be deleted from the results of strain analysis if tracking quality was determined to be inappropriate by eyeball judgment. Temporal changes in strain data were obtained as time-strain curves (Figure 2). We defined each strain measurement as the peak systolic strain value globally and in seven segments: inlet lateral, inlet inferior, inlet septum, outflow septum, outflow free wall, apical free wall, and apical septum. The SD of the time to peak area strain of the seven segments was measured as the RV dyssynchrony parameter.

In the validation study of 3D STE-derived RV volume and systolic function, RVEDV, RVESV, and RVEF were compared with those derived from CMR. To evaluate the significance of echocardiographic measurements, correlations between the CMR-derived RVEF and conventional echocardiographic parameters or 3D STE-derived strain measurements were assessed.

CMR for RV Volume and Function

CMR examinations were performed with a 1.5-T superconducting unit (Philips, Best, the Netherlands) with a phased-array cardiac coil. Electrocardiographically gated cine mode images using a steady state were obtained in a short-axis view with 10-mm slice thickness without an intersection gap. The acquisition time was 10 to 16 sec while patients held their breath. CMR images were analyzed using offline software (ViewForum; Philips). From short-axis images, we selected the slice

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