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Alzheimer's وجع Dementia

Featured Article Longitudinal uncoupling of cerebral perfusion, glucose metabolism, and tau deposition in Alzheimer's disease Antoine Leuzy^a, Elena Rodriguez-Vieitez^a, Laure Saint-Aubert^a, Konstantinos Chiotis^a, Ove Almkvist^{a,b,c}, Irina Savitcheva^d, My Jonasson^{e,f}, Mark Lubberink^{e,f}, Anders Wall^{e,g}, Gunnar Antoni^{g,h}, Agneta Nordberg^{a,b,*} ^aDivision of Translational Alzheimer Neurobiology, Department of Neurobiology, Care Sciences, and Society, Karolinska Institutet, Stockholm, Sweden ^bDepartment of Geriatric Medicine, Karolinska University Hospital Huddinge, Stockholm, Sweden ^cDepartment of Psychology, Stockholm University, Stockholm, Sweden ^dDepartment of Radiology, Karolinska University Hospital Huddinge, Stockholm, Sweden ^eDepartment of Surgical Sciences, Radiology, Uppsala University, Uppsala, Sweden 19<mark>01</mark> ¹Medical Physics, Uppsala University Hospital, Uppsala, Sweden ^gPET Centre, Uppsala University Hospital, Uppsala, Sweden ^hDepartment of Medicinal Chemistry, Uppsala University, Uppsala, Sweden Introduction: Cross-sectional findings using the tau tracer [¹⁸F]THK5317 (THK5317) have shown Abstract that [¹⁸F]fluorodeoxyglucose (FDG) positron emission tomography data can be approximated using perfusion measures (early-frame standardized uptake value ratio; ratio of tracer delivery in target to reference regions). In this way, a single positron emission tomography study can provide both functional and molecular information. Methods: We included 16 patients with Alzheimer's disease who completed follow-up THK5317 and FDG studies 17 months after baseline investigations. Linear mixed-effects models and annual percentage change maps were used to examine longitudinal change. **Results:** Limited spatial overlap was observed between areas showing declines in THK5317 perfusion measures and FDG. Minimal overlap was seen between areas showing functional change and those showing increased retention of THK5317. Discussion: Our findings suggest a spatiotemporal offset between functional changes and tau pathology and a partial uncoupling between perfusion and metabolism, possibly as a function of Alzheimer's disease severity. © 2017 Published by Elsevier Inc. on behalf of the Alzheimer's Association. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/). Keywords: Positron emission tomography (PET); Tau imaging; THK5317; Neurofibrillary tangles; FDG; Hypometabolism; Perfusion imaging; R1; Perfusion SUVR; Alzheimer's disease; Prodromal Alzheimer's disease; Alzheimer's disease dementia; Mild cognitive impairment; Longitudinal study

1. Introduction

In addition to amyloid- β (A β) and tau pathology, Alzheimer's disease (AD) is characterized by decreased brain perfusion [1,2] and glucose metabolism [3,4]. Cross-sectional comparative studies have indeed shown regional perfusion and metabolism to be tightly coupled in neurodegenerative disorders, including AD [5,6], and in controls, under both active and resting physiological conditions [7]. As such, [¹⁸F]fluorodeoxyglucose (FDG) positron emission tomography (PET) metabolic data can be approximated using early-frame standardized uptake value ratio (p-SUVR) and the ratio of tracer delivery in target (K_1) and reference regions (R_1) , measures **02** shown to correlate strongly with brain perfusion [8,9].

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^{*}Corresponding author. Tel.: +46 8 585 85467; Fax: +46 8 585 85470. E-mail address: agneta.k.nordberg@ki.se

110 Comprehensive compartmental approaches, involving 111 the solution of differential equations and requiring arterial 112 blood sampling, form the basis of PET-based estimation of 113 physiological parameters of interest [10]. Reduced configu-114 ration models have been developed, however, whereby the 115 116 input function derived from arterial plasma is replaced by 117 that from a reference region [10]. These approaches obviate 118 the need for arterial cannulation and metabolite assay, 119 simplifying scanning protocols and data analysis proced-120 ures. While the objective of these models is to obtain an 121 122 estimate of tracer binding, such as the distribution volume 123 ratio (DVR)-total distribution volume in target over refer-124 ence region-derived from reference Logan, a graphical 125 approach involving linearization [11], perfusion information 126 in the form of R_1 can also be obtained using models that rely 127 128 on iterative curve fitting such as the simplified reference tis-129 sue model [12] and related approaches involving parameter 130 coupling [13]. By contrast, calculation of p-SUVR does not 131 require kinetic modeling and instead reflects the assumption 132 that early-time frame uptake reflects K_1 [14], with p-SUVR 133 134 thus reflective of R₁.

135 Findings from studies implementing the use of perfusion 136 measures (p-SUVR and R_1) with A β PET tracers have 137 shown to closely correlate with FDG, and to carry potential 138 clinical utility, having been used to distinguish AD from 139 140 controls [15], frontotemporal lobar degeneration [16], and 141 cerebral amyloid angiopathy [17]. Findings from our earlier 142 cross-sectional study using, the tau-specific PET tracer [¹⁸F] 143 THK5317 (THK5317) [18,19] in AD suggest that tau 144 imaging may also prove able to provide both molecular 145 146 and functional information [9], similar to that proposed for 147 A β PET [16]. Given the possible future clinical use of tau 148 PET for diagnostic purposes and evaluation of drug thera-149 pies, as well as the advantages inherent to dual-use imaging 150 [20,21], further exploration of these findings is warranted. 151

152 In this study, we sought to quantify the longitudinal rela-153 tionship between THK5317 perfusion measures, glucose 154 metabolism (FDG SUVR), and tau pathology (THK5317 155 DVR), in a cohort of patients with AD. The test-retest repro-156 ducibility of THK5317 perfusion measures was likewise 157 158 investigated. 159

2. Methods

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2.1. Participants 164

165 Sixteen AD patients (10 prodromal AD and six AD de-166 mentia) who had previously participated in baseline inves-167 tigations [22,23] were here followed up after a median 168 interval of 17 months (interquartile range: 15-18 months) 169 170 [24]. All patients had originally undergone clinical assess-171 ment for memory problems at the Department of Geriatric 172 Medicine, Karolinska University Hospital, Huddinge, Swe-173 den, and had been followed up after diagnosis, as detailed 174 elsewhere [22]. Patients diagnosed with AD dementia met 175 176 the revised NINCDS-ADRDA criteria for probable AD and showed in vivo evidence of AD pathology (abnormal $[^{11}C]$ Pittsburgh Compound B [PIB]) [25]. Patients who fulfilled the diagnosis of mild cognitive impairment [26] and showed a positive PIB scan were diagnosed as prodromal AD [27].

All subjects provided informed consent to take part in the present study, which was conducted according to the Declaration of Helsinki and subsequent revisions. Ethical approval was obtained from the regional human ethics committee of Stockholm and the Faculty of Medicine and Radiation Hazard Ethics Committee of Uppsala University Hospital, Uppsala, Sweden.

2.2. Acquisition and analysis of imaging data

Dynamic THK5317 studies were conducted over 60 minutes, following intravenous bolus injection of 217 \pm 42 MBq. A static 15-minute FDG scan was performed 30 minutes after injection of 3 MBq/kg. Dynamic baseline and follow-up THK5317 and FDG PET images were coregistered to their respective T1-MRIs using PMOD (v.3.5; PMOD Technologies Ltd., Zurich, Switzerland). Structural images were segmented using SPM8, with the inverse transformation parameters generated used to spatially warp a probabilistic atlas [28] into native T1 image space. Voxelwise THK5317 p-SUVR and simplified reference tissue model R₁ maps were obtained with PMOD, using the cerebellar cortex as reference tissue [9,12]. For p-SUVR, the interval 0-3 minutes was selected based on the previously reported observation that this interval showed the highest correlations with FDG [9]. Parametric SUVR (30-45 minutes) and Logan DVR images (30-60 minutes) were created for FDG and THK5317, respectively, using the cerebellar cortex as reference region [11,22].

Annual percentage change was calculated voxelwise for 03 all PET parameters as follows: {[(Follow-up - Baseline)/ Baseline]/Time interval between scans (years)} \times 100%. To binarize resulting parametric maps to examine their spatial overlap, average isocortical test-retest reproducibility of THK5317 perfusion measures (rounded) was adopted to exclude voxels within the test-retest repeatability range of perfusion measures. Voxelwise THK5317 p-SUVR, R₁, and FDG SUVR maps were used to perform pairwise correlations using the biological parametric mapping software package (MATLAB v.3.3). An 8-mm filter and an a priori gray matter mask were then applied to spatially normalized PET images with resulting correlation maps thresholded at P < .001 (uncorrected, cluster extent ≥ 20 voxels).

2.3. Test-retest reproducibility of THK5317 perfusion measures

To establish the test-retest reproducibility of THK5317 p-SUVR and R₁, five subjects (four prodromal AD and one possible corticobasal syndrome) [29] underwent a retest THK5317 PET scan (range: 13-37 days).

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