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### ORIGINAL ARTICLE

## A new orthodontic force system for moment control utilizing the flexibility of common wires: Evaluation of the effect of contractile force and hook length

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contractile force and hook length to elucidate their effects. Three types of commercial wires were tested.

*Results*: The second-order moment was greater on the longer hook side of the model. Vertical force balanced the difference in moments between the two teeth. Greater contractile force generated a greater second-order moment, which reached a limit of 150 g. Excessive contractile force induced more undesired reactions in the other direction. Longer hooks induced greater moment generation, reaching their limit at 10 mm in length.

*Conclusion*: The system acted similar to an off-center V-bend and can be applied in clinical practice as an unconventional loop design. We suggest that this force system has the potential for second-order moment control in clinical applications.

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#### Introduction

Appropriate moment application is crucial for successful orthodontic treatment. Second-order control is especially important in most clinical situations, including extraction space closure, uprighting a tipped molar, and torqueing incisors during anterior retraction. A V-bend is a well-known force system used to apply moments that has been well studied<sup>1,2</sup>; these studies demonstrated that the position and degree of the bend and the wire material influenced the entire system.

Nickel-titanium alloy (Ni-Ti) archwires are mainstays in contemporary orthodontics because of their shape memory and superelasticity.<sup>3,4</sup> Although this material was first produced as an initial leveling wire, Ni-Ti wires are now being tried as working wires due to the light stable force that can be acquired.<sup>5–8</sup> Therefore, moment control using highly flexible Ni-Ti wire has gained attention. Moments produced by a V-bend in superelastic Ni-Ti wires have been reported to have different patterns than other linear elastic materials, such as stainless steel and titanium-molybdenum alloy (Ti-Mo).<sup>9</sup> However, the incorporation of a V-bend into a superelastic Ni-Ti closed-loop mechanism has demonstrated adequate moment-to-force ratio generation for bodily movement.<sup>10</sup>

For more accurate moment control, we attempted to develop new mechanics by taking advantage of the natural characteristics (namely, low stiffness and high spring-back qualities) of Ni-Ti wires. We pinched two crimpable hooks at certain distances on a straight wire and then applied a contractile force between the hooks for activation, which induced curved wire deformation (Figures 1A and 1B). This system acted similarly to a V-bend system that generates moments in the brackets in opposing directions without any burdensome bending procedure that requires an extra heat treatment machine for the Ni-Ti wire. However, in contrast to a V-bend system, which is simply affected by the bending degree and position, our system is related to multiple factors that act in a more complicated fashion.

Although our force system mainly focused on secondorder moment control, unpredictable side effects in other directions frequently confuse clinical orthodontists.<sup>11</sup> To reveal the applied force from this newly designed orthodontic apparatus, a three-dimensional full-scale model is required for force measurements. Recently, various threedimensional force measurement methods have been developed.<sup>12–16</sup> Among these studies, an orthodontic simulator (OSIM) incorporating multiple six-axis force sensors<sup>16</sup> was used in several experiments<sup>17–20</sup> to successfully measure orthodontic force and moment in three dimensions. A modified OSIM device designed to increase operability has also been reported and proved to be effective for evaluating orthodontic force systems.<sup>21</sup> Therefore, the aims of this study were to investigate how the components of the proposed force system affect the generation of moments and forces using a modified OSIM device and to put the knowledge into clinical practice.

#### Methods

#### Experimental model

A schematic of the experiment is shown in Figure 2A. This model was designed to simulate the conditions of lower second premolar extraction. Two artificial teeth were fixed with a distance of 15 mm between the two bracket centers based on the mean tooth diameter of the Mongolian population,<sup>22</sup> where the diameter of the first premolar, second premolar, and first molar were 7 mm, 6.5 mm, and 10 mm, respectively. A straight wire with two different hooks and lengths crimped in the wire next to the bracket was then engaged into the slots. A contractile force was finally applied between the hooks to activate the system with a superelastic Ni-Ti closed spring, which theoretically delivers constant force.<sup>23</sup> Variables that affect this system include  $L_A$ ,  $L_B$ , C, D1, D2, temperature,<sup>24</sup> and the material characteristics of the wire (Figure 2B). The orientation is shown in Figure 2C.

#### Measurement device

We developed a device that incorporates two six-axis sensors (CFS018CA201a: Leptrino, Nagano, Japan) following the principles of the modified OSIM device. Two cylindrical artificial teeth fabricated from an acrylic compound (VeroClear RGD810; Stratasys, Eden Prairie, MN, USA) were linked to these sensors with custom-made aluminum action

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