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Alzheimer's

Alzheimer's & Dementia: Translational Research & Clinical Interventions 🔳 (2018) 1-15

Featured Article

Advances in functional magnetic resonance imaging data analysis methods using Empirical Mode Decomposition to investigate temporal changes in early Parkinson's disease

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AbstractIntroduction: Previous neuroimaging studies of Parkinson's disease (PD) patients have shown
changes in whole-brain functional connectivity networks. Whether connectivity changes can be de-
tected in the early stages (first 3 years) of PD by resting-state functional magnetic resonance imaging
(fMRI) remains elusive. Research infrastructure including MRI and analytic capabilities is required
to investigate this issue. The NIH/NIGMS Center for Biomedical Research Excellence awards sup-
port infrastructure to advance research goals.

Methods: Static and dynamic functional connectivity analyses were conducted on early stage nevermedicated PD subjects (N = 18) and matched healthy controls (N = 18) from the Parkinson's Progression Markers Initiative.

Results: Altered static and altered dynamic functional connectivity patterns were found in early PD resting-state fMRI data. Most static networks (with the exception of the default mode network) had a reduction in frequency and energy in specific low-frequency bands. Changes in dynamic networks in PD were associated with a decreased switching rate of brain states.

Discussion: This study demonstrates that in early PD, resting-state fMRI networks show spatial and temporal differences of fMRI signal characteristics. However, the default mode network was not associated with any measurable changes. Furthermore, by incorporating an optimum window size in a dynamic functional connectivity analysis, we found altered whole-brain temporal features in early PD, showing that PD subjects spend significantly more time than healthy controls in a specific brain state. These findings may help in improving diagnosis of early never-medicated PD patients. These key observations emerged in a Center for Biomedical Research Excellence–supported research environment.

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Keywords: Resting-state fMRI; Empirical mode decomposition; EMD; Intrinsic mode function; Group ICA; Functional connectivity; PPMI; Parkinson's disease

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1. Introduction

Functionally related regions of the resting brain show a high degree of temporal correlation in blood-flow fluctuations, as measured by the blood-oxygenation level-dependent (BOLD) functional magnetic resonance imaging

https://doi.org/10.1016/j.trci.2018.04.009

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110 (fMRI) signal [1]. Using either seed-based methods or data-111 driven approaches such as independent component analysis 112 (ICA), brain regions that fluctuate in synchrony and consti-113 tute reliable and reproducible functional networks in the 114 human resting brain can be identified [2-6], named resting-115 116 state networks. Resting-state networks were assumed to be 117 static in nature in the past, and approximately a dozen of 118 such static networks have been discovered and investigated 119 in relation to how they are impacted by neurodegenerative 120 disorders. However, more recently, it has been shown that 121 122 resting-state networks are dynamic in character and change 123 on a time scale of several seconds to a minute [7-10]. 124 Analyzing the temporal dynamics of resting-state connectiv-125 ity provides a more accurate picture of the working brain and 126 can help in the early detection of neurological disorders and 127 128 in monitoring effects of potential treatments.

129 Both static and dynamic analysis methods have been 130 applied to study resting-state functional networks in major 131 neurodegenerative diseases, for example, Alzheimer's dis-132 ease (AD). One of the major brain networks affected in AD 133 134 is the so-called default mode network (DMN), which is 135 heavily involved in memory formation and retrieval [11]. 136 In normal subjects, the DMN shows functional connections 137 between the posterior cingulate cortex, angular gyrus, hip-138 pocampus, and the medial prefrontal cortex. In AD pa-139 140 tients, amyloid-beta (AB) protein has been found to 141 accumulate in DMN and other regions, which may disrupt 142 connections and lead to the symptoms of memory and 143 cognitive impairment [12–14]. Early $A\beta$ accumulation is 144 associated with reduced static functional connectivity 145 within the DMN and between the DMN and the 146 147 frontoparietal network (FPN), a network that is involved 148 in attention-demanding tasks [15,16]. The dynamic 149 aspect of the DMN shows significant changes in AD as 150 well [17]. It has been reported that AD subjects spend 151 152 less time in brain states with strong posterior DMN contri-153 butions and more time in states with dorsal medial prefron-154 tal cortex contributions. 155

Parkinson's disease (PD) is, after AD, the second most 156 common neurodegenerative disorder in the elderly and is 157 158 characterized by degeneration of dopaminergic neurons in 159 the substantia nigra pars compacta with resulting striatal 160 dopaminergic deficiency [18]. Previous neuroimaging 161 studies of PD patients have shown that whole-brain func-162 tional networks such as the DMN and networks involving 163 164 the motor pathway are affected, leading to different func-165 tional connectivity patterns when compared to those 166 found in normal controls (NC) [19]. Studies of the tempo-167 ral characteristics of fMRI resting-state brain networks 168 have also shown abnormal spontaneous low-frequency 169 170 content in PD [20]. The dynamic aspects of brain net-171 works have been widely studied using electrophysiolog-172 ical recordings. Intraoperative electrophysiological data 173 have shown that the occurrence of motor symptoms in 174 PD is associated with changes in synchronizations within 175 176 and between brain regions and changes in phaseamplitude coupling between brain regions [21,22]. However, it is not clear if *static* changes in resting-state networks are present in the very early stages (first 3 years) in drug-naïve never-medicated patients with PD. Furthermore, whether changes in temporal dynamics occur in resting-state functional networks in de novo PD subjects is unknown. 177

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In the present study, as part of the NIH/NIGMS Centers of Biomedical Research Excellence grant to the Center for Neurodegeneration and Translational Neuroscience, we investigated low-frequency BOLD fluctuations of major resting-state networks in early PD using data from the Parkinson's Progression Marker Initiative (www.ppmi-info. org). Previously, frequency-specific analysis of restingstate networks has been carried out using bandpass filtering in which the frequency intervals were specified using information from electrophysiological data [23] or simply by dividing the possible frequency range into equal intervals that were specified by the user [24,25]. An alternative approach toward finding frequency intervals in restingstate data is by Empirical Mode Decomposition (EMD) [26,27]. EMD is a data-adaptive analysis method for studying the naturally occurring frequency bands in time series [28]. EMD can be used, in particular, for nonstationary signals and allows the decomposition of time series into nearly orthogonal modes spanning narrow frequency bands. The oscillatory modes are called intrinsic mode functions (IMFs) and are obtained by a sifting algorithm. The novelty of our EMD approach lies in the adaptive decomposition of fMRI data using EMD and identification of resting-state networks based on energy and period (inverse of frequency) characteristics of IMFs. These novel energy-period relationships of resting-state networks in PD may allow use of imaging biomarkers in characterizing or detecting PD in the early stages of the disease. Early stage identification of PD may improve diagnostic accuracy, enrollment in clinical trials of disease-modifying agents, and allow for more effective treatments.

In a second investigation, we explored the dynamic aspects of functional connectivity using the same data set. In previous research studies, dynamic functional connectivity analysis was carried out mainly by using a sliding-window method, in which pairwise linear correlations among network components are captured in subsequent temporal windows with a fixed window size and further clustered into multiple dynamic functional brain states [29,30]. To find an appropriate window size is challenging because the windows size should be small enough to capture existing temporal transients and large enough to produce stable results [10]. The EMD method, however, provides us an alternative way to compute a time-dependent optimum window size in the sliding-window analysis. IMFs obtained from EMD track local periodic changes of nonstationary time series and an optimum window size can be determined at each time point. We incorporated the optimum window size in the sliding-window method to explore dynamic Download English Version:

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